

Ins and Outs of Biological Tissue Bi-exponential Quadrupolar NMR Signal Relaxation:

There is No Bound Sodium

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Among the most abundant magnetic atomic nuclei in biology, three have the spin quantum number $I = 3/2$. These are: ^{23}Na , ^{35}Cl , and ^{39}K .¹ In tissue, these elements exist almost exclusively as the mobile mono-aquoions, Na_{aq}^+ , Cl_{aq}^- , and K_{aq}^+ . Since they are isoelectronic with closed shell inert gas atoms Ne (for Na^+) and Ar (for Cl^- and K^+), they do not form covalent chemical bonds with other atoms. (A small atom fraction of biological Cl atoms, in the Cl^0 oxidation state, forms single covalent bonds with C atoms.) Their homeostatic *tissue* concentrations are: $[\text{Na}_t^+] = 44$, $[\text{Cl}_t^-] = 56$, and $[\text{K}_t^+] = 47$ mM.¹ Most importantly, however, these are not their compartmental concentrations.

The almost exclusive biological role of these species is manifest by their maintenance in homeostatic trans-(cell)membrane concentration gradients. Typical values are: $[\text{Na}_i^+] = 15$, $[\text{Na}_o^+] = 135$ mM; $[\text{Cl}_i^-] = 15$, $[\text{Cl}_o^-] = 105$ mM; and $[\text{K}_i^+] = 150$, $[\text{K}_o^+] = 5$ mM,² where the “i” and “o” subscripts signify inside and outside cells, respectively. Taking the typical membrane potential (E_m) to be that caused by homeostatic cellular K^+ efflux, 90 mV (inside negative), the electrochemical potential free energy values are $\Delta G_{\text{Na}} = -14.4$ kJ/mole for Na^+ influx, and $\Delta G_{\text{Cl}} = -3.62$ kJ/mol for Cl^- efflux. Continued expenditure of metabolic energy is required to sustain these conditions. Thus, the Na^+ and Cl^- gradients serve to store chemical energy derived from ATP hydrolysis, and that of K^+ maintains the cell membrane potential. These are absolutely vital functions for cell life, and are driven by the continual operation of the crucial plasma membrane Na^+, K^+ -ATPase (NKA) enzyme, the “sodium pump.” Particularly prominent roles are found in excitatory signal transmission.

The *in vivo* ^{23}Na signal is much larger than those of ^{35}Cl and ^{39}K .¹ And, obviously, the Na^+ biological role is crucial. Thus, it has long been hoped ^{23}Na MRI could prove of clinical benefit. However, realization has been difficult. Current human ^{23}Na MRI voxel volumes are approximately 60 μL . This means there are typically 6×10^6 cells in a voxel. At best, quantitative ^{23}Na MRI can assess the averaged, tissue concentration. However, as detailed above, this gives no information on the essential trans-cytolemmal $[\text{Na}^+]$ gradient. This is because $[\text{Na}_t^+] = v_e[\text{Na}_o^+] + v_i[\text{Na}_i^+]$, where v_e and v_i are the extra- and intracellular volume fractions, respectively. Clinical changes in $[\text{Na}_t^+]$ can be caused by: a) changes in v_e ($= 1 - v_i$) at constant $[\text{Na}_o^+]$, $[\text{Na}_i^+]$; b) changes in $[\text{Na}_o^+]$, $[\text{Na}_i^+]$ (or both) at constant v_e , v_i ; or c) some combination of these. This is the *Hilal ambiguity*.³ Discriminating intra- and extracellular ^{23}Na signals, either from living animals using a shift reagent⁴ or from cell suspensions with no shift reagent,⁵ does not resolve this confound. These approaches give only the $v_i[\text{Na}_i^+]$ and $v_e[\text{Na}_o^+]$ products. They cannot lead to ΔG_{Na} mapping, an ultimate goal. ($\Delta G_{\text{Na}} = RT \ln\{[\text{Na}_i^+]/[\text{Na}_o^+]\} + eFE_m$; e is the electron electric charge and F the Faraday constant.) The $[\text{Na}_i^+]$ and v_i values must be determined independently.

Complicating the situation further is the fact that ^{23}Na is a spin 3/2 nucleus. Even when the latter is isolated (not J-coupled to another spin – the usual case for ^{23}Na), it has four spin states (energy levels).^{4,6-9} This means a single ^{23}Na nucleus in any particular Na^+ molecular environment can exhibit one of three single quantum (SQ) resonances. This is dramatically different than the case for a spin 1/2 nucleus (^1H) with only two spin states, and has led to much misinterpretation. The MRI world is accustomed to the fact that a single type of $^1\text{H}_2\text{O}$ molecule in a single type of molecular environment gives only a single signal (one site: one resonance).

Fundamentally, an MR resonance has four properties: 1) intensity; 2) Larmor frequency (ν_L); 3) longitudinal relaxation rate constant, $R_1 = 1/T_1$; and 4) transverse relaxation rate constant, $R_2 = 1/T_2$. Even for a single molecular environment, a spin 3/2 signal has its intensity partitioned into three relative values (0.3:0.4:0.3) determined by quantum mechanical principles.^{4,6-9} Their resonance frequencies can be different ($\nu_0 + \langle \nu_Q \rangle$; ν_0 ; $\nu_0 - \langle \nu_Q \rangle$), where $\langle \nu_Q \rangle$ is the temporal mean quadrupolar spectroscopic splitting factor (“coupling constant;” $\langle \nu_Q \rangle = \langle \omega_Q \rangle / 2\pi$).^{4,6-9} These are usually referred to as one “central” and two “satellite” transitions.

A spin 3/2 nucleus has an *electric* quadrupole. Thus, its orientation, relative to the *magnetic* field (\mathbf{B}_0) direction, depends on the orientation (in \mathbf{B}_0) of the *electric* field *gradient* (EFG; dE/dx ; q) of its immediate molecular environment. The nucleus also has a *magnetic* dipole. So, the orientation of the latter in \mathbf{B}_0 also depends on that of q . The ^{23}Na

nuclear quadrupole moment (Q) is rather large (10 (fm)^2), and when a $^{23}\text{Na}^+$ ion is “trapped” in an anisotropic site with a very large q , as is often the case in the solid state, ν_Q for ^{23}Na can approach 10 MHz.⁴ The value of ν_Q is proportional to e^2qQ/h , where h is Planck’s constant. Thus in the solid state, q can be as great as $10 \times 10^{30} \text{ (V/m)/nm}$.

However, in any aqueous fluidic environment (such as biological tissue), there is much molecular motion. Fluctuation of q magnitude/orientation is characterized by a ν_Q modulation correlation time constant, τ_c . The mean Na_{aq}^+ structure ($\text{Na}(\text{OH}_2)_6^+$) is isotropic ($q = 0$). However, because of hydration shell normal mode vibrations, $\tau_c = \tau_v < 1 \text{ ps}$, $\langle \nu_Q \rangle = 0$. The central and two satellite resonances are isochronous. Upon temporal averaging, the square of ν_Q , $\nu_Q^{\text{rms}} = 1 \text{ MHz}$.^{4,7}

Molecular motion also has significant consequences for the third and fourth signal properties, the relaxation rate constants. There are two SQ R’s for each: $^{10}\text{R}_{1s}$ and $^{10}\text{R}_{1f}$, and $^{10}\text{R}_{2s}$ and $^{10}\text{R}_{2f}$, where the s and f subscripts represent “slow” and “fast,” respectively. We will not dwell on $^{10}\text{R}_{1s}$ and $^{10}\text{R}_{1f}$ here, because their relationships to the spin states are complicated,⁷ and they are rarely discriminated.

The behavior of $^{10}\text{R}_{2s}$ and $^{10}\text{R}_{2f}$, however, is crucial. Fortunately, these can be identified with the central and satellite resonances, respectively. The very fast modulation in the Na_{aq}^+ environment causes $^{10}\text{R}_{2f}$ to equal $^{10}\text{R}_{2s}$. It is too fast for efficient relaxation. Thus, there is a single, narrow resonance with a single $^{10}\text{R}_2$ value – a *homogeneous* resonance, with a single exponential transverse decay. We have termed this a *type d spectrum*.^{4,6-9} It is also often said to be in the “extreme narrowing limit.”

The mean lifetime (τ_M) of the sodium-oxygen coordinate covalent bond in Na_{aq}^+ is approximately one nanosecond. During its diffusional excursions in the tissue *milieu*, the Na_{aq}^+ ion encounters other molecules and, sometimes, one inner coordination sphere water molecule is transiently replaced by (almost exclusively) an oxygen atom of the other molecule. This new sodium-oxygen bond provides a significant q , but does not last even a nanosecond. Encountering further molecules gives transient q ’s with all possible orientations in \mathbf{B}_0 . Generally, there is no macroscopic orientational order in the surroundings.

Thus, a much slower modulation, 10^3 MHz (τ_M^{-1}), is superimposed on the fast, fundamental 10^6 MHz (τ_v^{-1}) fluctuation of ν_Q .⁷ Even if the other molecule is as small as 100 kDa, its rotational correlation time, τ_r , is $> 60 \text{ ns}$. So, in the complete expression, $\tau_c^{-1} = \tau_v^{-1} + \tau_M^{-1} + \tau_r^{-1}$, only the first two terms are of any consequence: $(60 \text{ ns})^{-1}$ is only 17 MHz.

Values of ν_L for ^{23}Na MR studies are tens of MHz. If the slow ν_Q modulation (τ_M^{-1}) is near or even less than ω_L ($2\pi\nu_L$), and has sufficient amplitude (significant q values), it acts particularly to catalyze (increase) $^{10}\text{R}_{2f}$, which is more sensitive to slow fluctuations than is $^{10}\text{R}_{2s}$.⁷ The $^{10}\text{R}_{2f}$ and $^{10}\text{R}_{2s}$ values become different: $^{10}\text{R}_{2f} > ^{10}\text{R}_{2s}$. Thus, though the resonances remain isochronous, and the satellite transition remains *homogeneous*, the transverse relaxation becomes bi-exponential. We termed this a *type c spectrum*.^{4,6-9}

In biological tissue, the *type c* condition obtains almost exclusively for the ^{23}Na resonance. [More restricted conditions (with some macroscopic orientational order), *type b* and *type a*,^{4,6-9} are very rare.] Unfortunately, however, *type c* has been often misinterpreted. Let us re-state the situation: the resonance consists of two signals with the same resonance frequency but two different $^{10}\text{R}_2$ (T_2) values. Depending on the experimental dead-time, some of the signal with $^{10}\text{R}_{2f}$ usually decays before acquisition begins ($^{10}\text{T}_{2f}$ values can be a few hundred μs .⁶). This has been called “ ^{23}Na MR invisibility,” and has often been interpreted that some Na is missing, or “bound.” But this is not the case. All tissue Na contributes to *each* signal; satellite and central. Some of the signal is missing, not some of the Na. The central transition acts very much like that of a spin $\frac{1}{2}$ nucleus [the $^{10}\text{R}_{2s}$ expression has no “secular” term].^{4,6-9} The resonances of ^{35}Cl and ^{131}Xe ($I = 3/2$) can exhibit similar spectra,⁷ and no one thinks of Cl[−] or Xe as forming covalent bonds. This misinterpretation contributed to one of the most significant controversies in bio-science history.¹⁰

References

1. Springer, "Measurement of metal cation compartmentalization in tissue by high-resolution metal cation NMR," *Ann. Rev. Biophys. Biophys. Chem.* **16**:375-399 (1987).
2. Milo, Phillips, Orme, "Cell Biology By the Numbers," Garland Science, New York (2016); p. 92.
3. Rooney, Li, Sammi, Bourdette, Neuwelt, Springer, "Mapping human brain capillary water lifetime: high-resolution metabolic neuroimaging," *NMR Biomed.* **28**:607-623 (2015).
4. Springer, "Biological Systems: Spin-3/2 Nuclei," *Encyclo. NMR* **2**:940-951 (1996).
5. Zhang, Poirer-Quinot, Springer, Balschi, "Discrimination of intra- and extracellular $^{23}\text{Na}^+$ signals in yeast cell suspensions using longitudinal magnetic resonance relaxography," *J. Magn. Reson.* **205**:28-37 (2010).
6. Rooney, Springer, "The molecular environment of intracellular sodium: ^{23}Na NMR relaxation," *NMR Biomed.* **4**:227-245 (1991).
7. Rooney, Springer, "A comprehensive approach to the analysis and interpretation of the resonances of spins 3/2 from living systems," *NMR Biomed.* **4**:209-226 (1991).
8. Xu, Barbara, Rooney, Springer, "Two-dimensional multiple-quantum NMR spectroscopy of isolated spin 3/2 systems. II. ^{35}Cl Examples" *J. Magn. Reson.* **83**:279-298 (1989).
9. Rooney, Barbara, Springer, "Two-dimensional double-quantum NMR spectroscopy of isolated spin 3/2 systems: ^{23}Na Examples," *J. Am. Chem. Soc.* **110**:674-681 (1988).
10. Hazlewood, Ed., "Physiochemical state of ions and water in living tissues and model systems," *Ann. NY Acad. Sci.* **204**: (1973).

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