

Human Brain ¹H MRS of GM and WM: a Comparison of BASE-SLIM and CSI Regression

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TARGET AUDIENCE: Scientists and technologists who are interested in non-Fourier based spectral localization methods for advanced *in vivo* ¹H MRS to measure neurochemicals in a region-specific and/or tissue type-specific manner.

INTRODUCTION: Neurochemical measurement shows significant concentration variations between tissue-types, e.g., gray (GM) and white matter (WM), as well as tissue-type specific alterations in neurological disorders. Current ¹H MRS acquisition strategies present significant challenges in ascertaining metabolite quantification of GM and WM. Regression analysis of CSI data with GM & WM tissue fractions¹ has been widely used to extrapolate metabolite concentrations from GM and WM. However, the accuracy of CSI regression analysis is hampered by a poor spread of tissue fraction values and inability to correct for B₀ and B₁ inhomogeneities in the analysis. Recently, we introduced BASE-SLIM², an advanced form of Spectral Localization by Imaging (SLIM)³, which overcomes limitations of SLIM by incorporating B₀ and B₁ field corrections. In this study, we present ¹H MRS of pure GM and WM using BASE-SLIM that incorporates anatomical contours of both GM and WM boundaries, and we compare the results with the regression analysis of CSI.

METHODS: Nine healthy subjects (31 ± 4 yrs, mean±SD) were studied, at 3 T (Skyra, Siemens) with a 16 channel head receive coil. The ¹H CSI was acquired using a semi-LASER sequence⁴ (TE/TR=35/1600ms, matrix=16x16, FOV=20cm) with the slab positioned across the prefrontal to parietal lobes. B₀ and coil sensitivity (B₁) maps were acquired using gradient echo sequences (TE=4.92/7.38ms for B₀, TE=2.07ms for B₁). BASE-SLIM reconstruction was performed using the CSI k-space data, B₀ and B₁ maps, and high resolution GM and WM segmentation masks. Coil combination of each ¹H MR spectrum from 16 channels was performed to maximize SNR with a maximal ratio combining scheme using the signal and noise spectral power estimates. Metabolite concentrations were quantified using LCModel³ and non-suppressed water scan as a concentration reference. CSI voxels with greater than 75% tissue fraction were selected for the regression analysis. The GM and WM regions covered in BASE-SLIM were identical to the CSI ROI in the regression analysis. BASE-SLIM reconstruction was implemented as previously described², involving an expanded geometry matrix for multiple coil sensitivity profiles and a time-dependent solution for B₀ corrections.

RESULTS AND DISCUSSION: Distinct spectral patterns of GM and WM ¹H MRS of the human brain show high choline to creatine ratio in WM than GM, which is visible from the spectra in Fig. 1. GM and WM compartments used for BASE-SLIM reconstruction are shown in inset MR images above ¹H MR spectra. Metabolite concentrations of GM and WM from CSI acquisition were quantified from scatter plots of each metabolite using a linear regression fit. An example of total choline fit is shown in Fig. 2. Metabolite quantification from BASE-SLIM reconstruction was in agreement with the extrapolated CSI regression for GM and WM. For example, NAA, creatine,

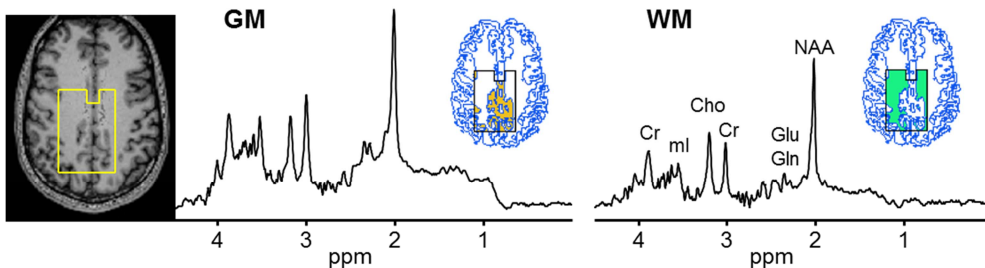


Fig. 1. ¹H MRS of gray and white matter using 3D BASE-SLIM. Selected ROI for BASE-SLIM and CSI analysis is shown in MRI (most left) and inset MRIs show GM (left) and WM (right) compartments where the corresponding ¹H MR spectra were measured.

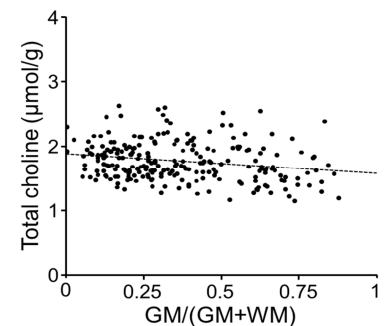


Fig. 2. Relationship between total choline and GM fraction (n=9).

choline, myo-inositol concentrations between two methods were within 10% differences while quantification of glutamate (Glu), glutamine (Gln) and the sum (Glu+Gln) was more reliable using BASE-SLIM: Glu+Gln in GM (12.0±1.3 µmol/g) and in WM (6.7±2.3 µmol/g). Our results suggest that BASE-SLIM can provide accurate assessment of tissue type-specific as well as region-specific metabolite quantifications that match or exceed the accuracy of the CSI regression method. In conclusion, BASE-SLIM based ¹H MRS may eliminate the need for Cartesian k-space acquisition and provides MR spectra from GM and WM with improved quality with minimum B₀ and B₁ inhomogeneity related errors.

REFERENCES: 1. Hetherington et al., *PNAS* 3115,1985. 2. Adany et al. *PISMRM* 3967, 2013. 3. Provencher, *MRM* 672, 1993. 4. Scheenen et al. *MRM* 1, 2008. This work is partly supported by the National Institutes of Health (S10RR29577, UL1TR000001) and the Hoglund Family Foundation.