

Motion Correction of Free Breathing Quantitative Myocardial T₂ Mapping: Impact on Reproducibility and Spatial Variability

Sébastien Roujol¹, Tamer A. Basha¹, Sebastian Weingärtner¹, Mehmet Akcakaya¹, Sophie Berg¹, Warren Manning^{1,2}, and Reza Nezafat¹

¹Department of Medicine, Beth Israel Deaconess Medical Center and Harvard Medical School, Boston, Massachusetts, United States, ²Department of Radiology, Beth Israel Deaconess Medical Center and Harvard Medical School, Boston, Massachusetts, United States

Target Audience

Scientists and clinicians who are interested in myocardial tissue characterization.

Purpose/Introduction

Quantitative myocardial T₂ mapping is a promising technique for the detection of inflammation and edema¹. Conventional sequences generally use a breath-hold electrocardiogram (ECG)-triggered T₂-prepared (T₂-prep) steady-state free precession (SSFP) acquisition¹. Due to limitations of breath-hold duration, these sequences are typically restricted to the acquisition of four T₂-weighted images. Free breathing myocardial T₂ mapping sequences remove this time constraint and enable the acquisition of more samples along the T₂ decay curve, which may result in improved precision and reproducibility of T₂ estimates. However, this approach requires more advanced respiratory motion correction techniques². We recently developed a technique for Adaptive Registration of varying Contrast-weighted images for improved Tissue Characterization (ARCTIC) which we have evaluated for myocardial T₁ mapping³. In the current study, we sought to investigate the performance of ARCTIC for free breathing T₂ mapping and its impact on in-vivo reproducibility and spatial variability of myocardial T₂ estimates.

Materials and Methods

T₂ mapping sequence: A free breathing respiratory gated ECG-triggered T₂-prep SSFP acquisition was used with different T₂-prep echo times (TE_{T2P})⁴. A 6 second rest cycle was inserted between the acquisitions of two successive T₂-weighted images to ensure full re-growth of longitudinal magnetization. Image acquisition immediately after a saturation pulse was used to simulate an infinitely long T₂-prep echo time (TE_{T2P} = ∞). No T₂-prep or imaging pulses were applied if the navigator signal was outside the gating window.

In-plane motion correction: The ARCTIC approach was used to compensate for in-plane motion between T₂-weighted images. In this approach, all images are registered individually to a common reference image, chosen as the first image of the series (TE_{T2P} = 0). Affine motion descriptors are first estimated over a region of interest surrounding the heart. This global transformation is then used as initialization of a local non-rigid motion estimation step which simultaneously estimates motion field and intensity variations on a per-pixel basis with an additional regularization term based on automatic feature tracking. A GPU implementation of ARCTIC was used to accelerate the process.

Experimental evaluation: All data were acquired on a 1.5 T Phillips scanner. Seven healthy adult subjects (30±17 years, 3 male) were imaged 5 times using the described T₂ mapping sequence (1 slice, field of view = 240×240 mm², in-plane resolution = 2.5×2.5 mm², slice thickness = 8 mm, TR/TE = 2.7 ms/1.35 ms, flip angle = 85°, 10 linear ramp-up pulses, SENSE rate = 2, acquisition window = 138 ms, phase encoding lines = 51, linear k-space ordering, 20 T₂-prep echo times (0, 25, 30, 35, ..., 95, 100, ∞, ∞, ∞). T₂ maps were reconstructed using a 3-point fit model⁴.

Data Analysis: In-vivo spatial variability and reproducibility of T₂ mapping were measured in uncorrected and motion corrected T₂ maps using a 6 myocardial-segment based analysis. Spatial variability was defined as the average (over the 5 scans) of the standard deviation of T₂ estimates over a given segment. Reproducibility was defined as the standard deviation (over the 5 scans) of the spatial average T₂ values in one given segment. To investigate the motion influence in T₂ mapping sequences using a conventional number of T₂-prep echo times, this analysis was performed using all 20 T₂-prep echo times (20TEs) and using only a subset of the T₂-weighted images (4 T₂-prep echo times (4TEs) of 0, 25, 50, ∞). Statistical significant differences between continuous variables were assessed by means of Student's t-Tests.

Results

Figure 1 shows an example of uncorrected and motion corrected data where the use of ARCTIC substantially improved the alignment of all images and resulted in improved T₂ map quality. Reduced spatial variability was observed over all subjects and myocardial segments in T₂ maps reconstructed from 4 T₂-prep echo times (13.7±4.3 vs. 11.1±3.6 ms, p<0.001) and 20 T₂-prep echo times (10.6±5.3 vs. 7.9±1.8 ms, p=0.001) (Figure 2a). Improved reproducibility was observed over all subjects and myocardial segments in T₂ maps reconstructed from 4 T₂-prep echo times (5.9±3.1 vs. 5.0±2.3 ms, p=0.011) and 20 T₂-prep echo times (4.3±3.9 vs. 2.4±1.0 ms, p=0.002) (Figure 2b). T₂ maps reconstructed with 20 T₂-prep echo times had higher reproducibility and lower spatial variability than motion corrected T₂ maps with 4 T₂-prep echo times (p<0.001).

Conclusions

The ARCTIC technique improves the reproducibility and spatial variability of in-vivo free breathing myocardial T₂ mapping.

Acknowledgements

Grant support from NIH R01EB008743-01A2 and Samsung Electronics.

References

- [1] McNamara, Circulation, 1985 [2] Giri, MRM, 2012
[3] Roujol, MRM, 2014 [4] Akcakaya, MRM, 2014

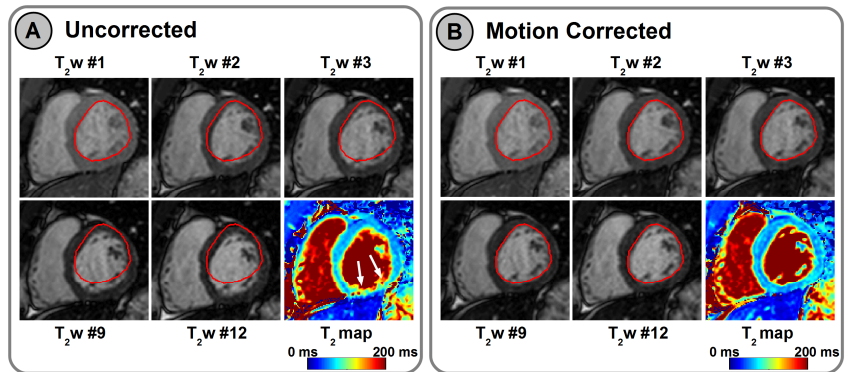


Figure 1. Uncorrected (a) and ARCTIC motion corrected (b) T₂-weighted images and T₂ maps. The ARCTIC technique improves the alignment of T₂-weighted images and the T₂ map quality.

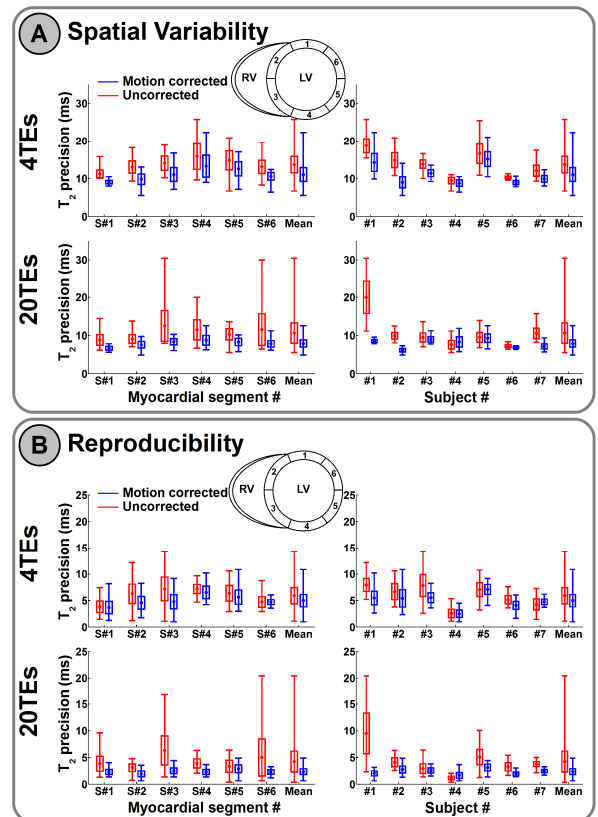


Figure 2. In-vivo spatial variability (a) and reproducibility (b) of T₂ mapping. ARCTIC motion correction improved both spatial variability and reproducibility of T₂ estimates.