

## Investigation of the dependence of measured lung $T_1$ on TE using UTE

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### Target audience:

This work is relevant for researchers working in  $T_1$  quantification in the lung (and possibly other compartmentalized tissues) as well as functional lung imaging in general.

### Purpose

In this work, it is demonstrated that the  $T_1$  measured in the lungs depends significantly on the applied echo time  $TE$ . This dependence is especially apparent when using ultra short  $TE$ s which are otherwise beneficial to overcome the short  $T_2^*$  found in the lungs.

### Methods

All measurements were performed on a clinical 1.5T scanner, using a multi-gradient-echo 2D UTE sequence described previously<sup>2</sup>, using a segmented, golden angle<sup>3</sup> encoded inversion recovery. 10

healthy non-smoking volunteers and one COPD patient were examined in single coronal slices. This allows for the calculation of  $T_1$  maps<sup>4</sup> at 5 different  $TE$ s between 70 $\mu$ s and 2.30ms, acquired during free breathing. Average  $T_1$  values were calculated by fitting the mean signal inside ROIs drawn over the entire lungs.

### Results

Figure 1 shows  $T_1$  maps of a healthy volunteer and a COPD patient, each sorted by  $TE$ . A gradual increase in  $T_1$  as  $TE$  rises is visible in the lung, while relaxation in long- $T_2^*$  tissue such as muscle appears almost unaffected. This increase of  $T_1$  with  $TE$  is apparent in all 10 volunteers investigated: The median  $T_1$  found at the investigated  $TE$  were  $T_1(TE_{1..5}) = 1051 \pm 57$  ms,  $1240 \pm 77$  ms,  $341 \pm 72$  ms,  $1335 \pm 80$  ms, and  $1408 \pm 73$  ms, showing a significant increase of  $T_1$  with  $TE$  ( $p < 0.001$ ). This is also apparent in the  $T_1$  measurements from a subset of volunteers shown in table 1, as well as those from a COPD patient.

### Discussion

The dependence of measured  $T_1$  on  $TE$  shown can be explained by two separate compartments in the lungs with both different  $T_1$  and  $T_2^*$ . We assume that these compartments represent blood and extravascular lung water, with the extravascular compartment having shorter  $T_1$  and  $T_2^*$ , and the blood protons longer relaxation times but still much shorter  $T_2^*$  than other tissues.

### Conclusion

In consequence, this leads to two main conclusions: When comparing lung  $T_1$  values measured in different subjects or experiments, the  $TE$  used should also be given to ensure comparability. However, it may also be exploited to gain diagnostic information since it is determined by the composition of lung tissue. The patient data so far is only preliminary and further studies are necessary to evaluate this effect in lung disease patients.

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### References

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	$T_1$ [ms]				
$TE$ [ms]	0.07	0.50	1.20	1.65	2.30
healthy	1140	1261	1373	1400	1426
	1105	1260	1391	1388	1485
COPD	1079	1277	1381	1421	1470
	761	911	940	993	986

Table 1: Average  $T_1(TE)$  values measured in the lungs of 3 volunteers and a COPD patient.

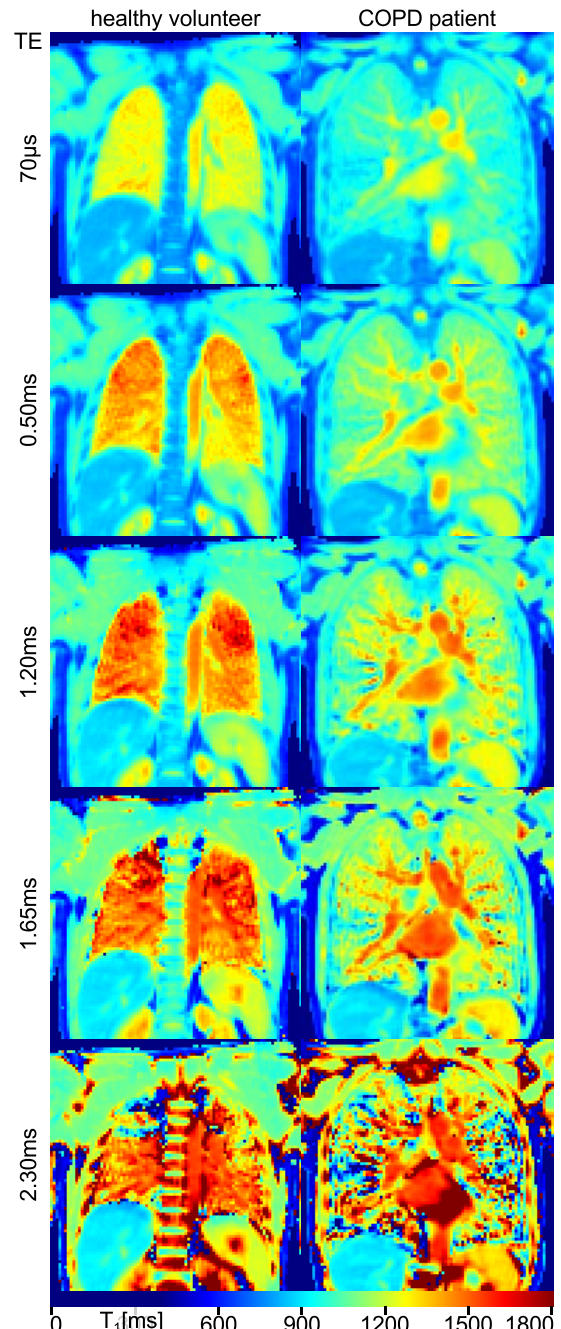


Figure 1:  $T_1$  maps acquired at 5  $TE$ s between 70 $\mu$ s and 2.30ms. Due to the short  $T_2^*$ ,  $T_1$  quantification fails in some voxels at long  $TE$ s.