

A 32-channel intracranial and extracranial vascular array for three dimension arterial wall MR imaging at 3T

Xiaoqing Hu¹, Lei Zhang¹, Chao Zou¹, Huabin Zhu², Xiaoliang Zhang³, Yiu-cho Chung¹, Xin Liu¹, Hairong Zheng¹, and Ye Li¹

¹Lauterbur Research Center for Biomedical Imaging, Shenzhen Institutes of Advanced Technology of Chinese Academy of Sciences, Shenzhen, Guangdong, China,

²Suzhou Medcoil Healthcare Co.,Ltd, Suzhou, Jiangsu, China, ³Department of Radiology and Biomedical Imaging, University of California San Francisco, San Francisco, CA, United States

Introduction Accurate characterization and quantification of the intracranial and extracranial vascular diseases by magnetic resonance imaging (MRI) is desirable in identifying high-risk patients [1]. Due to the thin thickness of the vessel wall, the multi-channel head array [2] and neck arrays with high signal-to-noise ratio (SNR) and capability of parallel imaging are preferred in clinical examination. Since there is a lack of RF coil arrays [3] capable of large longitudinal coverage for the carotid arteries which are composed of the intracranial and extracranial vessels, intracranial and extracranial vessels are usually imaged separately in clinical examinations. In this work, a 32-channel intracranial and extracranial vascular (IEV) array was designed and fabricated for the whole carotid artery imaging at 3T. Both phantom and *in-vivo* experiments were carried out to evaluate the performance of the 32-channel IEV array.

Coil Design: The 32-channel IEV array was composed of two parts: 24-channel for the head and 8-channel for the neck. In the head part, 24 circular loops were arranged in four columns as shown in Fig. 1. The numbers of the loops were 1, 7, 7 and 9 from anterior side to posterior side respectively. The loops were designed to closely fit the head [2]. In the neck part, there are 3 rectangular loops overlapping with a butterfly-shape loop on each side [3-4]. All the elements were tuned to 123.2 MHz and matched to 50 Ω . Overlapping among the elements and low input impedance amplifier were used for element decoupling. **Phantom Studies:** Phantom studies were carried out to evaluate the performance of the IEV array. A spherical phantom with 175 mm diameter and a cylindrical bottle with 115 mm diameter and 200 mm length were employed to mimic the human head and neck. The spherical phantom was filled by 1.25g/L $\text{NiSO}_4 \cdot 6\text{H}_2\text{O}$ while the cylindrical bottle was filled by 3.75g/L $\text{NiSO}_4 \cdot 6\text{H}_2\text{O}$ and 5g/L NaCl.

The phantom studies were performed on a 3T Siemens Trio MRI system. The SE sequence with following parameter was utilized: TR/TE = 300/15ms, FOV = 150 \times 230mm², resolution matrix = 152 \times 256, bandwidth = 260Hz/pixel. A noise scan was performed to acquire the noise covariance matrix by setting transmit power to zero. The covariance root sum of square (Cov-rSoS) [5] method was used to reconstruct the images. The SNR map was calculated based on reference [5]. **In-Vivo Studies:** The *in-vivo* experiments were performed in accordance with the institution's IRB regulations including informed consent. High resolution anatomical images were acquired to illustrate the performance of the 32-channel IEV array. T1-weighted 3D Sampling Perfection with Application optimized Contrasts using different flip-angle Evolution (SPACE) sequence was utilized [6], covering from extracranial carotid to brain vessel. The imaging parameters were: FOV = 180 \times 180mm², ETL = 9, ESP = 3.58ms, resolution matrix = 256 \times 256, slice thickness = 0.7mm (isotropic voxel size of 0.7mm³), TR/TE = 926/25ms, bandwidth = 476Hz/pixel, Averages = 2.

Results The noise covariance matrix of the 32-channel IEV array was shown in Fig. 2. It can be seen that the mutual coupling between 24-channel head part and 8-channel carotid part is very small. The phantom image and corresponding SNR map in sagittal plane of the proposed 32-channel IEV array were shown in Fig. 3. The 1/g-factor maps with reduction factor $R=2$ and 3 were also displayed in Fig. 3(C) and 3(D), which demonstrated that the parallel performance of the proposed 32-channel IEV array is very well. In volunteer studies, the vessel walls of major arteries such as extracranial and intracranial arteries with resolution 0.7 \times 0.7 \times 0.7mm³ was shown in Fig. 4, which demonstrated the large coverage and high resolution imaging capability of the 32-channel IEV array.

Discussion/Conclusion This study demonstrates a 32 channel IEV array design by combining an 8 channel carotid array and a 24 channel head array in convenient fashion. Both phantom and *in-vivo* experiment results show that the proposed array is capable to provide a large coverage from carotid to brain vessels with high SNR to achieve high resolution vessel wall images. This would benefit arterial disease diagnosis. Future investigation will focus on coil configure optimization of the head/neck array to further improve image resolution with high SNR.

Reference [1] Z.C.Zhou, et.al., ISMRM 2013, p.0877. [2]Wiggins GC., MRM (2006), 56(1), 216-223. [3] Y.Q.Zhang, et.al., ISMRM2012, p.2652. [4] X. Hu, et al., ISMRM 2014, p. 2543. [5] B. Keil et al., JMR 2013, 229, 75-89. [6] L. Zhang, et.al., ISMRM 2013, p3610.

Acknowledgments This work was supported in part by the NSFC Grant No. 81327801, 51307171, 61401450 and 61201442, and Key Project of Shenzhen Basic Research Program under Grant No. SY294261001, SIAT Innovation Program for Excellent Young Researchers under Grant No. 201314.

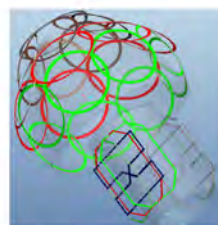


Fig.1 The figure of 32-channel IEV array.

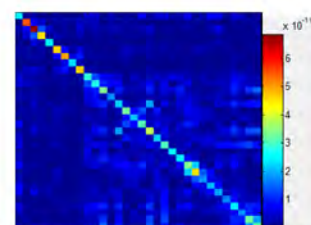


Fig.2 The noise covariance matrix of the IEV array

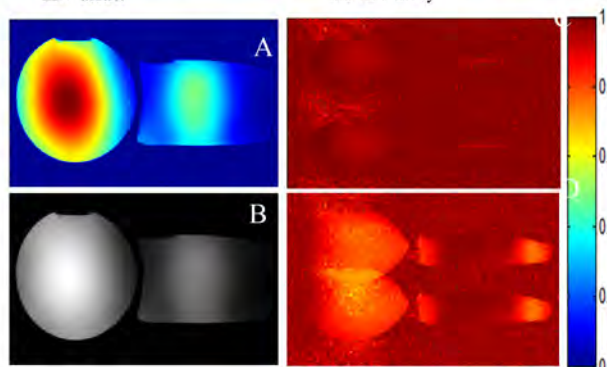


Fig.3 (A) The SNR map of 32-channel IEV array in sagittal plane. (B) The image of Cov-SoS. (C) and (d) 1/g-factor with reduction factor $R=2$ and 3.

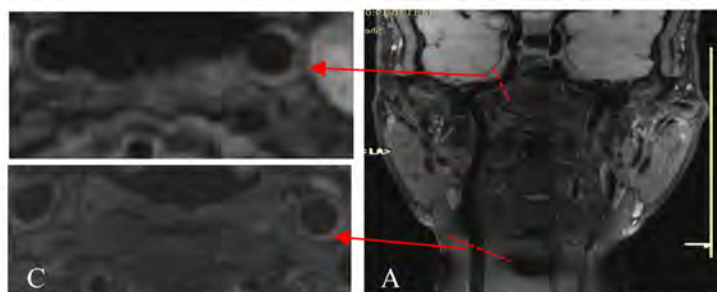


Fig.4 (A) The curve reconstruction results of the extracranial and intracranial arteries for 3D SPACE. (B) short axial of supraclinoid segment and (C) internal carotid artery.