

Importance of Biexponential T2* and Partial Volume Effect Corrections on Quantification of Sodium Concentrations and Fixed Charge Density of Articular Cartilage with ²³Na-MRI at 7T

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Target Audience: Researchers aiming to apply sodium MRI in articular cartilage research

Purpose: Quantification of sodium (²³Na) concentration and fixed charge density (FCD) with ²³Na-MRI are dependent on the postprocessing steps and corrections applied to measured ²³Na signal intensity (SI). Here we demonstrate how the correction for relaxation times and the correction of signal attenuation due to partial volume effect (PVE) affect the calculated ²³Na-concentrations and thus FCD of articular cartilage of a knee joint.

Methods: The ²³Na imaging of the knee joint was performed in an asymptomatic volunteer with an optimized 3D-vTE- spoiled GRE (SPGR) -sequence^[1] at 7T (²³Na-MRI: TR = 11 ms, TE₁ = 1.42 ms, flip angle (θ) = 33°, resolution of 1.5 x 1.5 x 2.8 mm³). All ²³Na-images were corrected for B₁ inhomogeneity by calculating the correction maps using a cylindrical phantom filled with ²³Na solution. The SI of manually segmented tibial and femoral tissue (S_{xy}) were corrected with factors obtained from SPGR signal equations using a) T1 and monoexponential T2*^[2] (T1 = 20 ms, T2* = 9.1 ms)^[3] or b) T1 and biexponentially analyzed T2* (T1 = 20 ms, T2*_{short} = 0.9 ms, A_{short} = 0.34, T2*_{long} = 13.3 ms, A_{long} = 0.66)^[3,4]. The biexponentially corrected signal (S₀) was further divided with PVE-correction factors (PVE_{cf}, Eq. 1) obtained by determining the mean tibial and femoral cartilage thickness (x_{tibia} = 2.8 ± 0.9 mm, x_{femur} = 2.5 ± 0.8 mm) from 3D-DESS images (TR/TE = 7.81/2.62 ms, isotropic resolution of 0.34 x 0.34 x 0.34 mm³) and fitting them to a function describing the attenuation of signal (Fig. 1a).^[5] Average water fraction (f = 0.75) of the cartilage tissue was also taken into account in all methods.^[4] The corrected SIs of cartilage tissue were fitted to a ²³Na calibration curve (linear fit to mean SI of four calibration phantoms corrected for T1 and monoexponential T2* (²³Na = 100-250 mM) and mean background noise (²³Na = 0 mM)) to obtain the corresponding ²³Na concentrations (Fig. 1b).^[6] FCD was calculated with respect to ²³Na – concentration of synovial fluid ([²³Na_{sf}] = 150mM): FCD = [²³Na_{sf}]² / [²³Na (x,y)] - [²³Na (x,y)].^[6]

$$S_0(x, y) = S_{xy}(x, y) * \frac{1 - \cos \theta * (e^{-TR/T1})}{(1 - e^{-TR/T1}) * \sin \theta (A_{short} * e^{-TE_1/T2^{*}_{short}} + A_{long} * e^{-TE_1/T2^{*}_{long}})} * \frac{B_1(x, y)}{f * PVE_{cf}} \quad (Eq. 1)$$

Results: The ²³Na concentrations of tibial and femoral cartilages using monoexponential T2* correction were (mean ± SD, all slices) 107 ± 31 and 98 ± 34 mM (Fig. 2a). The biexponential T2* correction of signal increased ²³Na to 141 ± 40 and 129 ± 43 mM (up to +33%, Fig. 2b), respectively. Biexponential T2* correction combined with PVE correction resulted in 251 ± 68 and 236 ± 78 mM (up to +179%, Fig. 2c) ²³Na concentrations and FCDs of -168 ± 83 mM and -157 ± 92 mM (Fig. 2d), respectively. The low ²³Na concentrations of monoexponentially and biexponentially T2* corrected data resulted mainly in positive FCD values.

Discussion and Conclusion: Importance of taking into account the biexponential T2* values and the signal attenuation due to PVE of ²³Na MRI were investigated in determining the ²³Na-concentration and FCD of tibial and femoral cartilage. The ²³Na concentrations calculated in this study were in agreement with previously reported ²³Na concentrations (240mM – 270mM)^[2,6] only after applying both the biexponential T2* and PVE corrections to ²³Na SI. Also in order to determine the fixed charge density (FCD)^[6] of articular cartilage, both biexponential T2* and PVE corrections were needed to reach adequate ²³Na concentrations. These results suggest that the biexponential decay of T2* and especially the signal attenuation due to PVE are important for correct evaluation of ²³Na concentration in knee cartilage even at high field strength (7T) and with images of fair resolution (in-plane 1.5 x 1.5mm, slice thickness 2.8mm).

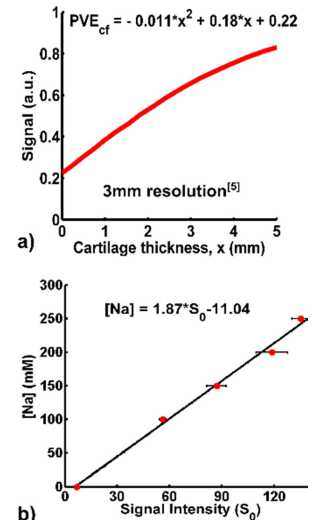


Fig 1: (a) Signal attenuation with respect to tissue thickness (adopted from Moon et.al 2013)^[5]. (b) Sodium calibration curve (phantom and noise values presented with red).

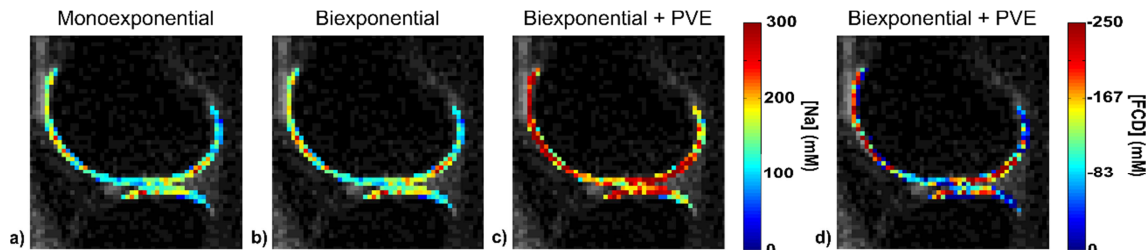


Fig 2: Sodium maps of tibiofemoral cartilages from a mid-sagittal slice of the knee calculated using (a) monoexponential T2* SI correction and (b) biexponential T2* SI correction. (c) Sodium and (d) FCD –maps with biexponential T2* and PVE corrections.

References:[1] Deligianni, X. et al. *Magn Reson Med* 70 (5), 1434-39. 2013. [2] Wheaton, A.J. et al. *Radiology* 231, 900–5. 2004. [3] Madelin, G. et al. *NMR Biomed.* 530–537. 2012. [4] Madelin, G. et al. *Radiology* 268, 481–91. 2013. [5] Moon, C.H. et al. *J. Magn. Reson. Imaging* 38, 1063–1072. 2013. [6] Shapiro, E.M. et al. *Magn. Reson. Med.* 47, 284–291. 2002.