

## Optimised segmentation scheme for high-resolution multi-shot 3D-GRASE pCASL with improved point spread function

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**Purpose.** Pseudo-continuous arterial spin labelling 3DGRASE provides high signal-to-noise ratio (SNR) with uniform background suppression (BS) and inversion time in all slices [1-3]. Typical spatial resolution in ASL is around  $4 \times 4 \times 6 \text{ mm}^3$ . Single shot 3DGRASE can provide higher spatial resolution and whole brain coverage but suffers from severe blurring in the partition/slice direction due to T2 decay if the echo train is excessively long. Multi-shot 3D-GRASE [4-6] has been proposed to reduce echo train duration and related blurring. We propose a new segmentation scheme for an isotropic 3.2mm spatial resolution acquisition combining both in-plane and through-plane segmentation, improving through-plane point spread function (PSF) and SNR of 3DGRASE pCASL.

**Methods.** 5 subjects were scanned on a 3T Tim Trio Siemens scanner (32-channel head-coil) with 4 segmentation schemes, either 1-shot or 4-shot (Figure 1). Common Parameters: 30 partitions (20% oversampling, 6/8 partial Fourier), FoV ( $220 \text{ mm}^2$ ), matrix  $64 \times 64$ , nominal voxel size ( $3.2 \text{ mm}^3$ ), TR = 4100 ms, acquisition time  $4'31''$ , BW = 2790 Hz/Pixel,  $130^\circ$  refocusing flip angle, 32 or 8 averages respectively for single-shot and 4-shot schemes. Other parameters are shown in Figure 2 (nPE=PE steps/shot). pCASL labelling and background suppression (BS) were implemented as in [3]. Echo-shifting [8] was applied for segmentation in the PE direction. For each scheme, M0 images were acquired without BS (41s, 8 and 2 averages for single-shot and 4-shot respectively). We acquired images without phase encoding (PE) and BS in order to measure the PSF. The PSF was also simulated with the extended phase graph (EPG) algorithm [7] using  $T1/T2/T2^* = 1310/100/45 \text{ ms}$ .

**Results.** Average control and difference images for one subject are shown in Figure 2 with the same intensity scaling. Low segmentation factor in the PE direction leads to severe distortions in the orbito-frontal cortex (red arrows) while through-plane blurring is reduced at shorter Echo Train durations, ETD (yellow arrows). Higher SNR is observed at shorter TE and shorter ETD. Moreover SAR reduces with Turbo Factor (aka ETL): by 11% and 17% in the 2x2 and 4<sub>PAR</sub>x1<sub>PE</sub> schemes respectively vs 1-shot and 1<sub>PAR</sub>x4<sub>PE</sub> schemes. Simulated PSFs in the partition (through-plane) direction show good agreement with *in vivo* data (Figure 3). As expected the PSF becomes narrower for shorter ETD (2x2 and 4<sub>PAR</sub>x1<sub>PE</sub>). Results from the other subjects were consistent with these findings.

**Discussion and Conclusions.** Novel acquisition schemes using segmentation in the partition direction have been proposed. Taking into account objective criteria (SNR, SAR, spatial resolution and geometric distortions), the best trade-off is achieved for a 4-shot 3DGRASE with the 2<sub>PE</sub>x2<sub>PAR</sub> segmentation scheme. This scheme provided promising results and negligible through-plane blurring, avoiding excessive in-plane geometric distortions, increasing the SNR and reducing the SAR. A wider range of segmentation schemes and echo trains with variable flip angles is currently under investigation for further optimisation.

**References.** 1. Ye, MRM 2000, 44(1):92; 2. Gunther, MRM 2005, 54:491; 3. Vidorreta, NeuroImage 2012; 66C:662; 4. Feinberg ISMRM 2009,622; 4. Cutajar, MAGMA 2012, 25(2):145; 5. Baiteau, ESMRMB 2013, 333; 6. Tan, MRM 2011. 66(1):168; 7. Hennig, JMR 1988, 78:397; 8. Feinberg, JMR 1992, 97:177.

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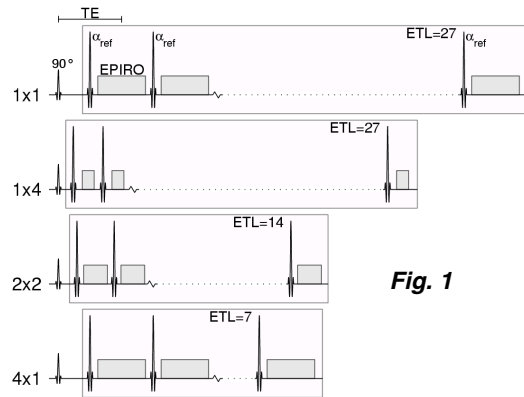


Fig. 1

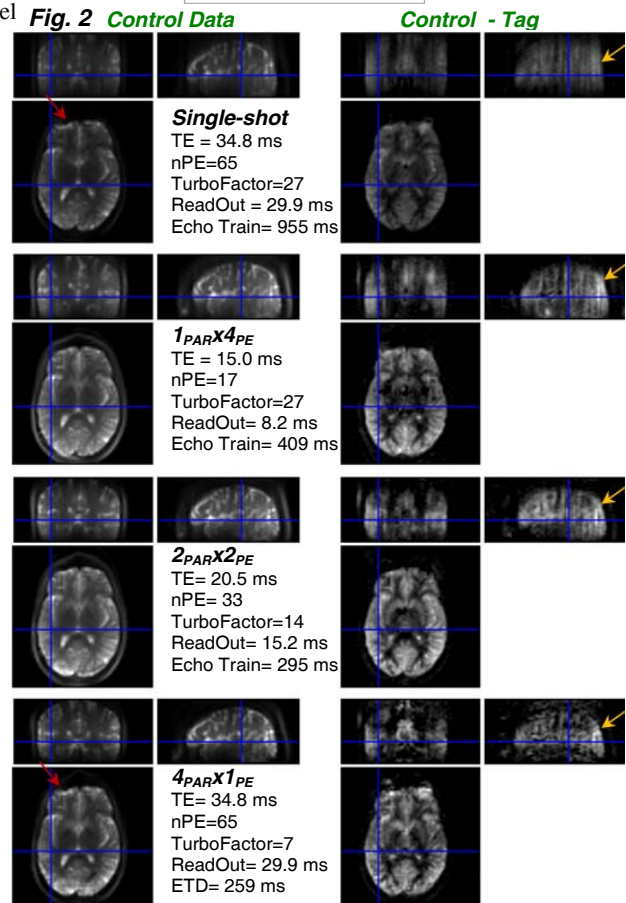


Fig. 2 Control Data

Control - Tag

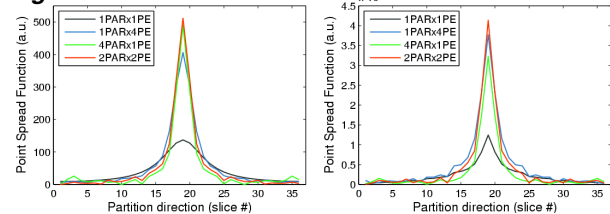


Fig. 3 EPG Simulated PSF

In vivo measured PSF