

# Single breath-hold 3D cardiac T<sub>1</sub> mapping

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**Target Audience** This work targets those interested in rapid measurement of relaxation times in cardiac tissues and in applications of non-Cartesian parallel imaging.

**Purpose** Cardiac T<sub>1</sub> mapping holds great potential for the detection of various cardiac diseases<sup>1</sup>. In practice, due to cardiac and respiratory motion, measurement of T<sub>1</sub> values of heart can be extremely challenging, especially for quantitative analysis of the entire heart. Recently, a rapid and accurate single breath-hold 3D T<sub>1</sub> mapping method for the abdomen has been developed, using the Look-Locker technique in combination with through time spiral GRAPPA for acceleration<sup>2</sup>. In this study, this strategy is modified with a segmented EKG triggered acquisition for cardiac application. GPU image reconstruction was also established for rapid image reconstruction, making the technique feasible for clinical applications.

**Methods** MRI experiments were performed on a Siemens 3T Skyra scanner with 32 receive channels. An algorithm similar to the modified Look-Locker inversion recovery (MOLLI) method was adopted for T<sub>1</sub> measurement<sup>3</sup>. The scan was divided into two segments (two inversion recovery periods, each of four heart beats) with a pause of 4 sec between segments. In each inversion recovery period, the data acquisition was EKG-triggered and all the data were obtained during mid- to end-diastole. In the first segment, data acquisition started right after the inversion RF pulse, while in the second segment, a delay (400–500 ms dependent on the heart rate) was applied to achieve full coverage along the T<sub>1</sub> relaxation curve. This modified inversion-recovery Look-Locker method was combined with a stack-of-spirals trajectory and through-time non-Cartesian GRAPPA to accelerate data acquisition. To meet the Nyquist criterion, a total of 48 spiral interleaves in-plane are required. To accelerate the scanning, a reduction factor of six was used in-plane (only 8 arms were collected) and then reconstructed using 3D through-time non-Cartesian GRAPPA<sup>2</sup>. To calculate the GRAPPA weights, a reference scan of twelve fully sampled 3D volumes (~43 sec) was acquired during free breathing, and was used for calibration along with a 4x1 segment size. Other parameters were: FOV= 44x44 cm; matrix size 224x224 for an effective in-plane resolution of 2.0 mm; TR 4.7 ms; TE 0.6 ms; flip angle 7°; slice thickness 8 mm; partial Fourier in the partition direction, 6/8. Overall, eight T<sub>1</sub>-weighted 3D volumes were obtained with inversion times from 320 to 3600 ms and the acquisition time for each 3D volume was about 450 ms. The non-Cartesian GRAPPA image reconstruction and Fourier transform was performed using similar framework as for non-Cartesian radial GRAPPA with a single GPU card (NVIDIA Fermi M2090)<sup>4</sup>. The GRAPPA weights calibration was achieved in approximately 90 sec and the image reconstruction for eight 3D volumes including filling missing interleaves using the GRAPPA weights and non-uniform FFT required approximately 20 sec.

The accuracy of the T<sub>1</sub> measurement was first validated using a manufactured phantom containing several vials with varying concentrations of GdCl<sub>3</sub> and agarose. T<sub>1</sub> values measured with an inversion-recovery single-echo spin-echo sequence (TR: 6 s; seven inversion times between 23 ms to 3000 ms) were used as the gold standard reference. After phantom validation, whole-heart T<sub>1</sub> mapping was performed on five asymptomatic volunteers in the short-axis view. The average acquisition time for T<sub>1</sub> mapping of the whole heart (16 slices) was 12.1±0.3 sec (12 heart beats in a single short breath-hold).

**Results and Discussion** Phantom results show that T<sub>1</sub> values acquired with the spiral sequence are in close agreement with the results from an IR spin echo sequence for a wide range of T<sub>1</sub> relaxation times from 400 to 1700 ms (Fig. 1). Fig. 2 shows representative T<sub>1</sub>-weighted images along various points on the inversion recovery curve, and a corresponding T<sub>1</sub> map for a single slice from a volunteer. Representative whole-heart T<sub>1</sub> maps from another volunteer are shown in Fig. 3. The T<sub>1</sub> value of left ventricular myocardium from the five subjects was 1194±49 ms, which is in excellent agreement with the literature<sup>5</sup>.

**Conclusion** In this study, a 3D whole-heart T<sub>1</sub> mapping technique was developed using the modified Look-Locker method, a stack-of-spirals trajectory and through-time non-Cartesian GRAPPA acceleration. This technique allows fast and accurate T<sub>1</sub> mapping of the whole heart in a single short breath-hold. The fast image reconstruction framework developed using a GPU makes this technique further feasible for a clinical setting.

## References

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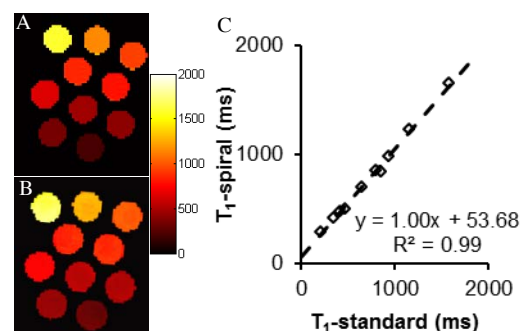


Fig. 1. T<sub>1</sub> maps of multi-compartment phantoms acquired using (A) inversion-recovery single-echo spin echo (TR: 6s) and (B) inversion-recovery stacks-of-spirals method. (C) Comparison of T<sub>1</sub> values from the two sequences.

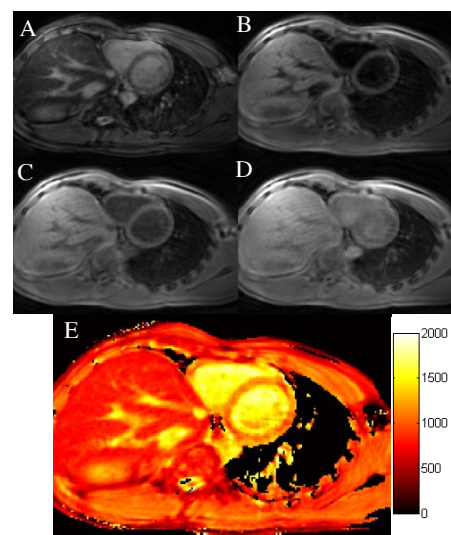


Fig. 2. (A-D) T<sub>1</sub>-weighted images of a normal volunteer at different inversion times of 327, 919, 1428 and 3122 ms. (E) The corresponding T<sub>1</sub> map.

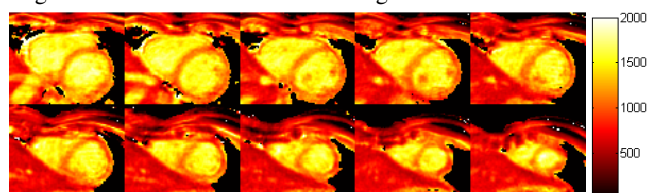


Fig. 3. Representative 3D cardiac T<sub>1</sub> maps from a volunteer.