

# Refined Balanced Steady-State Free Precession in Breath-hold Coronary MRA at 3.0T

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**INTRODUCTION:** Transient balanced steady-state free precession (bSSFP) is the sequence of choice in non-contrast enhanced coronary MRA at 1.5T because of its intrinsically high blood signal and blood-myocardium contrast compared to non-balanced sequences<sup>1</sup>. Earlier studies of bSSFP at 3.0T report dark bands, degraded image quality, shorter visible vessel lengths, and elevated inter-observer variability compared to spoiled gradient echo sequences at 3.0T<sup>2</sup>. In a recent study, localized RF and B<sub>0</sub> shimming provided reproducible bSSFP acquisitions for imaging the major coronary arteries in a breath-hold at 3.0T<sup>3</sup>. In this work, we propose to refine the breath-hold sequence in ref. 3 with modifications that were previously proposed for acquisitions with respiratory navigators<sup>4</sup>: 1) shortened RF pulses using variable-rate selective excitation<sup>5</sup> (VERSE) to reduce both TR and acquisition time (Fig. 1B), 2) pre-saturation of dark band areas, and 3) improved transition to steady state.

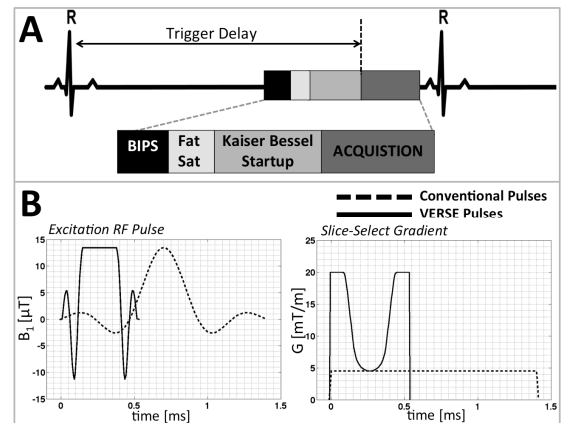
**METHODS:** A 3D volume-targeted bSSFP sequence was optimized on a 3.0T MR scanner (Philips Achieva TX, Best, The Netherlands). An axial B<sub>1+</sub> map was acquired for localized RF shimming and a B<sub>0</sub> map was acquired along the 3D track of the coronary of interest to determine the localized 2<sup>nd</sup> order shim and resonance frequency<sup>6</sup>. Coronary MRA acquisitions were performed using the original<sup>3</sup> and the proposed sequence (Fig. 1A). Five binomial pre-saturation (BIPS) pulses were used to saturate the spins at frequencies where dark bands occur. The transition to steady state prior to acquisition was accelerated with a Kaiser-Bessel shaped flip angle sweep of 10 startup RF pulses<sup>7</sup>. This preparation scheme has previously been reported to suppress artifacts originating from the dark band frequencies<sup>4</sup>. In initial studies, the spectrally selective fat saturation (fat sat) excitation angle was optimized over the range of 80-140° for an improved fat suppression and less sensitivity to TR and field inhomogeneities. VERSE pulses<sup>5</sup> (Fig. 1B) were implemented reducing the TR from 3.9ms to 3.2ms. Other parameters were: TE=1.5ms,  $\alpha=50^\circ$ , FOV=300×300×22mm<sup>3</sup>, voxel size=1.1×1.1×2.4mm<sup>3</sup>, acquisition window 95ms, half-Fourier factor 0.6, SENSE 2.5 in phase-encode direction. The data were acquired during 21±1 s breath-holds. Three healthy volunteers (44-52 years old) and one patient (76 years old) with coronary artery disease were scanned. Analysis was performed using the semi-automated Soap-Bubble tool<sup>8</sup>.

**RESULTS AND DISCUSSION:** All volunteers successfully completed the scans. The experimentally optimized fat sat angle was 95°. Images of the left anterior descending artery (LAD) and the right coronary artery (RCA) are shown in Figs. 2 and 3. The BIPS pre-saturation, Kaiser-Bessel startup sweep, and shorter TR due to VERSE achieved a better suppression of artifacts as highlighted by the white arrows. The visualized vessel length and vessel sharpness compared favorably for the proposed method at 104.1mm and 51% with the conventional sequence at 92.5mm and 49%, respectively.

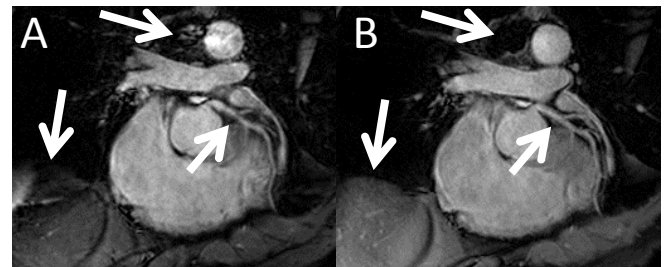
**CONCLUSION:** The refined sequence in combination with RF and B<sub>0</sub> shimming demonstrates image quality improvements in breath-hold bSSFP coronary MRA at 3T and warrants further investigation.

**REFERENCES:** [1] *Invest Radiol*'02; 37:637-647. [2] *RoFo*'04; 176:1560-1565. [3] *JCMR*'13; 15(s1):E11. [4] *Proc ISMRM*'06; 370. [5] *JMR*'88; 78: 440-458. [6] *MRM*'04; 51:799-806. [7] *JMR*'03; 163:23-37 [8]. *MRM*'02; 48:658-666.

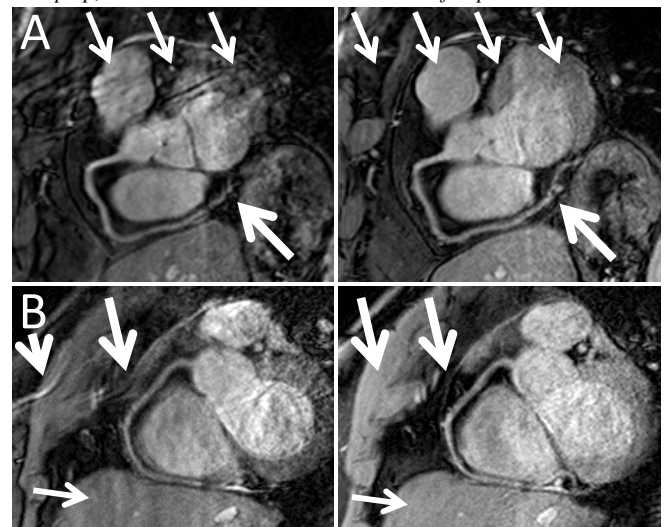
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**Fig. 1:** (A) The proposed transient bSSFP sequence. Magnetization is prepared with a 5-pulse binomial pre-saturation (BIPS), fat saturation, and Kaiser-Bessel shaped flip angle sweep. (B) RF and gradient pulses with standard and VERSE designs for demonstration.



**Fig. 2:** Multi-planar reformatted images of LAD in a healthy volunteer, acquired with (A) the conventional  $\alpha/2$ -TR/2 startup without VERSE and (B) the proposed combination of BIPS, Kaiser-Bessel sweep up, and VERSE. Arrows indicate areas of improvement.



**Fig. 3:** Multi-planar reformatted RCA images acquired in a single breath-hold using (left) the conventional  $\alpha/2$ -TR/2 startup vs. (right) the proposed combination of BIPS, Kaiser-Bessel sweep up, and VERSE in (A) a patient with no significant stenosis in the proximal-mid RCA and (B) a healthy volunteer. Arrows show areas of improvement.