

Multi-Echo fMRI Atlas of Seed-Based Functional Connectivity with Power Analysis

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Background Multi-echo (ME) fMRI methodology has recently been adopted by several groups for large cohort studies on typical development and neuropsychiatric disorders (e.g. autism, addiction, chronic pain). Here we present a novel atlas of group-level seed-based functional connectivity from a large sample of normal control datasets ($N=139$), using the unbiased seed-connectivity estimator achieved by combining multi-echo (ME) fMRI and ICA (ME-ICA)[1]. This estimator, called multi-echo independent coefficients regression (ME-ICR), interprets ICA as a transformation of data into approximately independent/sparse coefficients, enabling: classification of components as BOLD/non-BOLD based on component-level TE-dependence (κ) in ME-fMRI data; denoising by non-BOLD component rejection; correlation between the BOLD coefficient vectors of voxels; and finally BOLD degree of freedom (DOF) regularization within the Fisher R -Z transform. As an unbiased estimator, ME-ICR produces nearly normally distributed subject-level correlation distributions for any given seed, and group-level analysis with type I error control when comparing datasets with BOLD DOF differences (due to acquisition sensitivity variation from motion). By comparison, conventional seed-based functional connectivity using correlation between “denoised” single-echo fMRI time series suffers from ineffective denoising, unaccounted DOF variability across datasets, high type I error from group analysis, and poor understanding of statistical power with increasing N . Here we demonstrate group ME-ICR seed-connectivity maps for numerous cortical and subcortical regions, alongside power analysis using subsampling at $N=10,25,50,75,100$ to assess N required to make specific connectivity observations. **Methods** *Subjects and Acquisition* 139 subjects were scanned for 10 min. with multi-echo EPI (TR=2.47s; flip angle=78°; 3.75x3.75x4.4mm³; 32 oblique alternating slices, iPAT 3; 1698 Hz/pixel; TE = 12,28,44,60ms) [2], and MRPAGE (1mm³ iso., TI=1100ms) on Siemens 3T Tim Trio. *Preprocessing* ME-ICA v2.5 implemented slice and volume realignment, nonlinear coregistration (AFNI *Qwarp*[3]), T₂* weighted combination[4], BOLD/non-BOLD ME-PCA dimensionality detection and BOLD/non-BOLD ME-ICA decomposition and component separation (97% dataset variance explained on average) [1]. *Subject-level ME-ICR* The ICA mixing matrix was fit to the T₂* weighted combination of ME data, and concatenated (unthresholded) maps of “high- κ ” BOLD components produced the coefficient vector dataset. After computing Pearson correlation (R) between seed and target coefficient vectors, R values were converted to standard (Z_{corr}) scores using the Fisher R -Z transform, which adjusted for BOLD DOF (i.e. number of high- κ components) using the canonical standard error term. *Group ME-ICR* Subject-level ME-ICR coefficient datasets and dataset-level standard error terms were input to AFNI *3dGroupInCorr*, which produced 1-sample T -test group connectivity maps for several seeds. T -values were converted to standard scores (Z_T). **Results** Group ICR maps are shown in Figure 1a, with Z_{corr} overlay and Z_T threshold ($Z_T=6[\sigma]$). Overall: maps are sparse; conform well to anatomy; show cortical and subcortical connectivity with comparable performance (note thalamic nuclei); do not show anticorrelation (thus rendered all positive); and agree with localization seen from task activation. Maps are rendered here to convey power gains from group analysis. At subject level, Z_{corr} is both effect size and the basis of significance (p). At group level, significance is determined by Z_T , and smaller Z_{corr} effect sizes are observed with greater Z_T significance. Warm and yellow colors indicate $Z_{corr}\geq 1$ and $Z_{corr}\geq 2$ (i.e. $p\leq 0.05$), so yellow connectivity is significant at subject level, while cooler colors indicate weaker magnitude connectivity exposed by group analysis. Cooler regions may extend yellow cores, or show long-range connectivity (e.g. fusiform face area to amygdala). Small displacements in seed localization produce connectivity differences, e.g. posterior putamen seed shows connectivity to Brodmann area 4 while anterior putamen seed shows connectivity to area 6. Figure 1b demonstrates power gain with higher N for connectivity analysis of the orbitofrontal cortex (OFC), and reveals that a $Z_T=3[\sigma]$ OFC-hippocampus connectivity is observable at $N=25$ but in a noisy map, while a 6σ observation is achievable at $N\sim 75$, and higher $N>75$ does not proportionally add power to this 1-sample analysis. **Discussion** Group ME-ICR enables high-quality whole-brain functional connectivity analysis for hypotheses regarding individual brain regions, producing well-localized connectivity maps that have stable behavior across varying N . **Conclusion** Current and future studies on functional connectivity using ME data may benefit substantially from the sensitivity of ME-ICR to cortical and subcortical connectivity, directness of analysis, simplicity of use, and statistical stability.

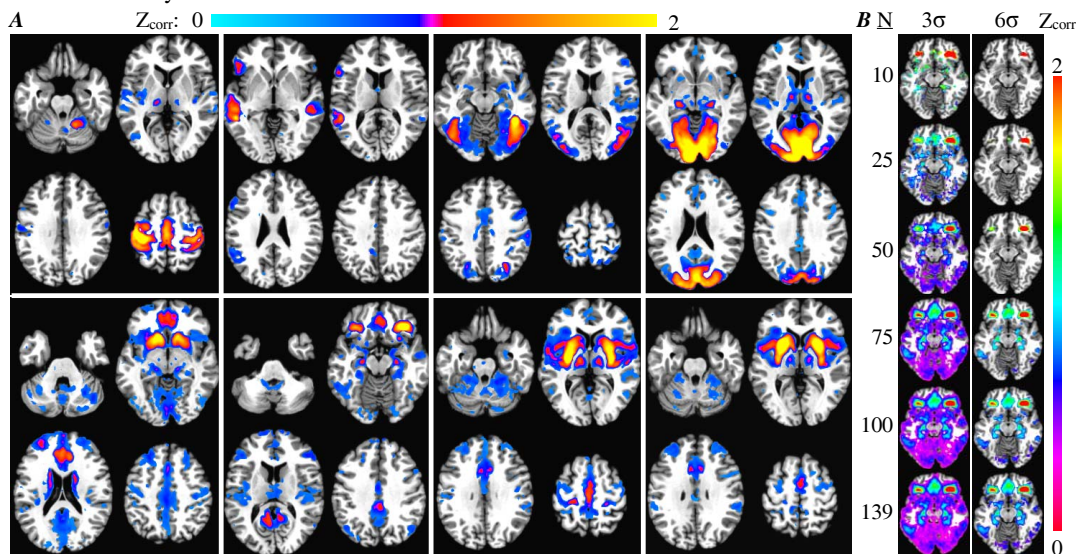


Fig. 1 Underlay is high-resolution MNI template (a) Group ICR maps of seeds (clockwise) in MNI coordinates. Overlay is mean Z_{corr} thresholded by $Z_T\geq 6[\sigma]$: right hand area (-33,-29,57), Wernicke's area (-53,-41,2), fusiform face area (43,-44,-18), primary visual (-5,-96,-4), ant. putamen (-24,10,1), pos. putamen (-29,-8,4), orbitofrontal cortex (36,34,-16), ventral striatum (-13,20,5). (b) Orbitofrontal connectivity at 3σ and 6σ for varying N . Note stable 6σ connectivity for $N\geq 75$.

References [1] Kundu, P. *et al* (2013). Integrated strategy for improving functional connectivity mapping using multiecho fMRI. *PNAS*, 201301725. [2] Poser, B.A. *et al* (2006). BOLD contrast sensitivity enhancement and artifact reduction with multiecho EPI: parallel acquired inhomogeneity desensitized fMRI. *Magnetic Resonance in Medicine*, 55, 1227–1235 [3] Cox, R. (2012). AFNI: what a long strange trip it's been. *Neuroimage*, 62, 743–747 [4] Posse, S. *et al* (1999). Enhancement of BOLD-contrast sensitivity by single-shot multi-echo functional MR imaging. *Magnetic Resonance in Medicine*, 42, 87–97.