

## Non-invasive imaging of deep venous thrombi by $^{19}\text{F}$ MRI using targeted perfluorocarbon nanoemulsions

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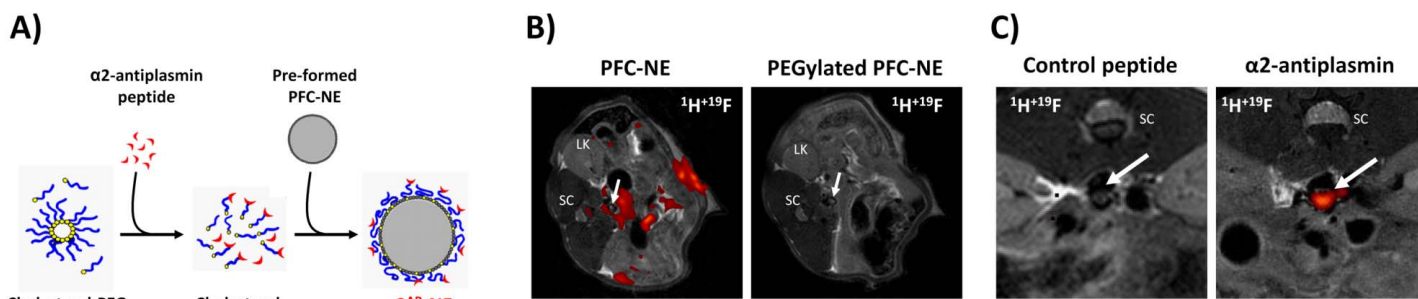
**Purpose:** Detection of deep venous thrombi which are not accessible by ultrasound is still a serious challenge. Therefore a non-invasive technique for unequivocal identification of those thrombi for diagnosis and subsequent monitoring of antithrombotic therapy would be highly desirable. Up to now  $^{19}\text{F}$  MRI has been widely used for cell tracking purposes either after *ex-vivo* or *in-vivo* loading of target cell populations. However, intravenous injection of perfluorocarbon nanoemulsions (PFC-NE) results in rapid clearance of circulating PFC-NE particles, since they are avidly taken up by blood monocytes and organs of the reticuloendothelial system. Therefore, a minimization of this phagocytic uptake is a prerequisite for an efficient targeting of PFC-NE to other cells or structures. Moreover, generation of targeted PFC-NE is hampered by the high-pressure homogenization process (about 1000 bar) required for preparation of PFC-NE which may easily destroy thermodynamically labile ligands. Thus, in the present study, we aimed at evaluating a novel post-insertion technique for generation of targeted PFC-NE, which makes use of a cholesterol-polyethylglycol<sub>2000</sub>-maleimide anchor (Chol-PEG<sub>2000</sub>). Here, the targeting ligand can be coupled to the maleimide group under very mild conditions while the cholesterol-anchor smoothly inserts into the lipid layer of preformed PFC-NE and the PEG moiety concomitantly impairs the PFC uptake by monocytes (Fig. 1a).

**Methods:** For targeting of freshly induced thrombi, we used the 14 amino-acid  $\alpha 2$ -antiplasmin ( $\alpha 2^{\text{AP}}$ ) peptide which is known to be cross-linked to fibrin *via* the glutamine (Q3) by active factor XIII (Miserus *et al.*, *JACC Cardiovasc. Imaging* 2, 8 (2009)). As control Q3 was mutated to alanine (Q3A). Peptides were conjugated to the Chol-PEG<sub>2000</sub> anchor *via* an additional cysteine residue in the peptide to obtain Chol-PEG- $\alpha 2^{\text{AP}}$  or the Chol-PEG- $\alpha 2^{\text{APQ3A}}$  (control) conjugate. Both constructs were inserted into preformed PFC-NE (containing 20% perfluoro-15-crown-5 ether) by incubation at 37 °C for 1 h and were subsequently characterized by photon correlation spectroscopy (PCS). Thrombi were induced *in-vivo* using a filter paper soaked with 10%  $\text{FeCl}_3$  which was applied to the external side of the *vena cava inferior* for 8 min and resulted in a non-occlusive thrombus. Since factor XIII is active during the early phase of the thrombus formations, we injected  $\alpha 2^{\text{AP}}$ -targeted-NE (or NE with  $\alpha 2^{\text{APQ3A}}$  as control) 5 min prior to  $\text{FeCl}_3$  application. Combined  $^1\text{H}/^{19}\text{F}$  MRI was performed 2 h, 8 h or 24 h after PFC injection at a vertical 9.4 T Bruker Avance<sup>III</sup> Wide Bore NMR spectrometer using a microimaging unit (Micro 2.5) with an actively shielded 40-mm gradient set (1 T/m maximum gradient strength and 110  $\mu\text{s}$  rise time at 100 % gradient switching. Mice were placed in a 25-mm  $^1\text{H}/^{19}\text{F}$  birdcage resonator and analyzed using standard  $^1\text{H}/^{19}\text{F}$  multi-slice RARE sequences ( $^{19}\text{F}$  RARE: 2.56x2.56 cm<sup>2</sup> FoV, 64x64 matrix, 1 mm slice thickness, TR 4000 ms, 256 averages, 34 min acquisition time). Subsequently, excised thrombi (fixed and embedded in agarose) were examined *ex-vivo* by high resolution  $^1\text{H}/^{19}\text{F}$  MRI ( $^{19}\text{F}$  3D RARE: 1x1x1 mm<sup>3</sup> FoV, 128x128 matrix, 67 h scan time). For further *ex-vivo* analysis, FITC-labelled  $\alpha 2$ -NE were applied, thrombi were excised and processed for histology or flow cytometry.

**Results and Discussion:** Chol-PEG<sub>2000</sub>- $\alpha 2^{\text{AP}}$  nanoemulsions ( $\alpha 2^{\text{AP}}$ -NE) were analyzed by PCS measurements and compared to the pre-formed PFC-NE stock solution. We observed a slight increase in size (diameter: NE = 149±15 nm;  $\alpha 2^{\text{AP}}$ -NE = 165±13 nm), a similar size distribution (polydispersity index: NE = 0.136±0.01;  $\alpha 2^{\text{AP}}$ -NE = 0.164±0.05), and a profoundly reduced  $\zeta$ -potential (NE = -37.2±4 mV;  $\alpha 2^{\text{AP}}$ -NE = -11.7±7 mV) indicating the successful incorporation of Chol-PEG<sub>2000</sub>- $\alpha 2^{\text{AP}}$  into PFC-NE. PEGylation of particles resulted also in significantly altered *in-vivo* distribution when intravenously injected immediately prior to thrombus induction. Unmodified PFC-NE were quickly phagocytosed, which gave rise to a strong  $^{19}\text{F}$  signal in the area of the surgery due to infiltration of PFC-loaded immune cells, but no PFC deposition was noticed within the thrombus. However, upon PEGylation almost no  $^{19}\text{F}$  signals were detected within the area of interest (Fig. 1b). The absence of untargeted PFC-NE in thrombi was further confirmed by flow cytometry which revealed infiltration of a negligible amount of monocytes and some neutrophils into the plug.

In the next step, we explored the suitability of the PEGylated PFC-NE, which were additionally equipped with the ligand  $\alpha 2^{\text{AP}}$ , for specific thrombus detection. To this end,  $\alpha 2^{\text{AP}}$ -NE (or  $\alpha 2^{\text{APQ3A}}$ -NE) were injected prior to thrombus induction and animals were analyzed by non-invasive  $^1\text{H}/^{19}\text{F}$  MRI after 24 h. In animals which received  $\alpha 2^{\text{AP}}$ -NE strong  $^{19}\text{F}$  signals could be detected within the thrombus which were absent when NE with control peptide was injected (Fig. 1c). Importantly,  $\alpha 2^{\text{AP}}$ -NE clearly delineated the thrombus but were not found in the area of the surgery. The location of the  $^{19}\text{F}$  signal within the thrombus was further confirmed by analyzing isolated thrombi *ex-vivo* by high resolution  $^1\text{H}/^{19}\text{F}$  MRI as well as by histology. To test whether  $^{19}\text{F}$  MRI can also be performed quite shortly after  $\alpha 2^{\text{AP}}$ -NE administration, we analyzed the  $^{19}\text{F}$  signal after 2 h, 8 h and 24 h and found that  $^{19}\text{F}$  signal reached 80% of the 24 h signal even after 2 h which mirrors the fast completion of thrombus formation in this model.

**Conclusion:**  $^{19}\text{F}$  MRI using stable  $\alpha 2$ -antiplasmin targeted PFC-NE is a valuable tool for the rapid, highly specific and unequivocal identification of freshly developed deep venous thrombi, which might have a potential clinical application in detection of rethrombosis or lung thromboembolism after surgery. Moreover, we propose that the sterol-based post-insertion technique is a promising platform to equip PFC-NE with different ligands (peptides, antibodies etc.) for *in-vivo*  $^{19}\text{F}$  MRI of specific targets.



**Figure 1:** A) Scheme showing the principle of the sterol-based post-insertion technique for generation of  $\alpha 2$ -antiplasmin targeted PFC-NE ( $\alpha 2^{\text{AP}}$ -NE). B) *In vivo*  $^1\text{H}/^{19}\text{F}$  MRI of mice which received intravenously administered untargeted PFC-NE (left) or PEGylated PFC-NE (right). Arrows show the location of the thrombus. C) Magnification of *in vivo*  $^1\text{H}/^{19}\text{F}$  MRI scans of mice which received  $\alpha 2^{\text{AP}}$ -NE (right) or NE with a control peptide (left). Arrows indicate the location of the thrombus.