

DOUBLE-RESONANT $^{13}\text{C}/^1\text{H}$ COIL SYSTEM FOR $\{^1\text{H}\} ^{13}\text{C}$ IN VIVO NMR SPECTROSCOPY ON A 7-T WHOLE-BODY MR TOMOGRAPH

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INTRODUCTION: ^{13}C NMR spectroscopy (^{13}C MRS) enables noninvasive quantification of various metabolites in vivo with or without enrichment of ^{13}C . High field ^{13}C MRS in combination with ^1H -decoupling provides a gain of information and signal in ^{13}C NMR spectra. The aim of this study was to design, implement and test a surface coil system for in vivo ^1H -decoupled ^{13}C NMR spectroscopy on an experimental 7-T whole-body MR tomograph. Hence a $^{13}\text{C}/^1\text{H}$ double-resonant transmit/receive coil system was developed. In order to reduce dielectric losses and capacitive detuning and to impose proper balancing a transmission line resonator¹ (TLR) concept was used. Furthermore specific filters were implemented to decouple both channels properly.

METHODS: The TLR consists of a semi-rigid coaxial cable ($\varnothing_{\text{cable}} = 5.5$ mm) arranged to a loop ($\varnothing_{\text{loop}} = 7.5$ cm, fig. 1a+b). A small gap separates its outer conductor into two equal parts. The ^{13}C matching network is located on the left side and the ^{13}C short circuit at the right end of the loop, for ^1H the other way round. To achieve adequate electromagnetic decoupling for both channels (^{13}C , ^1H) frequency selective filters are implemented. In particular the Chebyshev low pass filter in the ^{13}C channel is very important for the acquisition of ^1H -decoupled ^{13}C NMR spectra (fig. 1c+d).

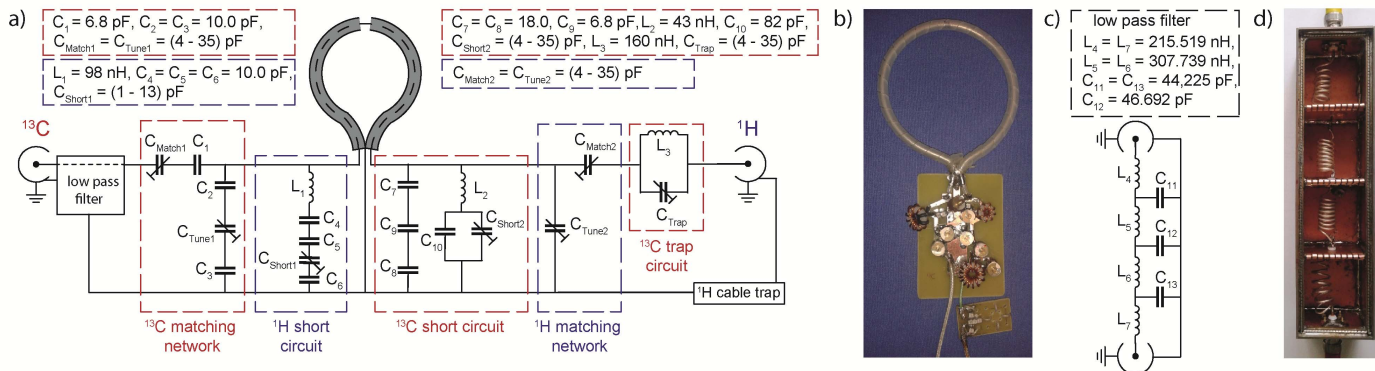


Fig. 1: (a) Circuit diagram and (b) implementation of $^{13}\text{C}/^1\text{H}$ double-resonant surface coil with $f_0(^{13}\text{C}) = 74.73$ MHz and $f_0(^1\text{H}) = 297.15$ MHz, (c) simulated, (d) constructed Chebyshev low pass filter with 4 chambers (bandwidth = 80 MHz, # poles = 7, passband ripple = 1.0 dB, $Z_{\text{in/out}} = 50 \Omega$)

The double-resonant coil loaded with a vegetable oil phantom (280 ml) was tuned and matched. The quality factors of the loaded coil and the forward transmission losses S_{21} from one channel to the other were determined with a network analyzer to evaluate the coil. Finally B_0 -shimmed ^{13}C NMR spectra of the phantom were acquired without and with ^1H -decoupling (WALTZ-4) on a MAGNETOM 7 T (Siemens Healthcare, Erlangen, Germany).

RESULTS: The measured quality factors of the coil are $Q(^1\text{H}) = 77$ and $Q(^{13}\text{C}) = 91$. The forward transmission losses S_{21} - low pass filter not included - amount to $S_{21}(1: ^{13}\text{C}, 2: ^1\text{H}, 74.73 \text{ MHz}) = -48$ dB and to $S_{21}(1: ^1\text{H}, 2: ^{13}\text{C}, 297.15 \text{ MHz}) = -24$ dB. The low pass filter performs very well with $S_{21}(74.73 \text{ MHz}) = -0.15$ dB and $S_{21}(297.15 \text{ MHz}) \approx -100$ dB. The complete coil design ensures a sufficient electromagnetic decoupling for both frequencies and allows its application in the decoupling mode ($\{^1\text{H}\} - ^{13}\text{C}$ MRS). Fig. 2 shows the methyl and methylene resonances of triacylglycerides (TAG) in the vegetable oil phantom without and with ^1H -decoupling.

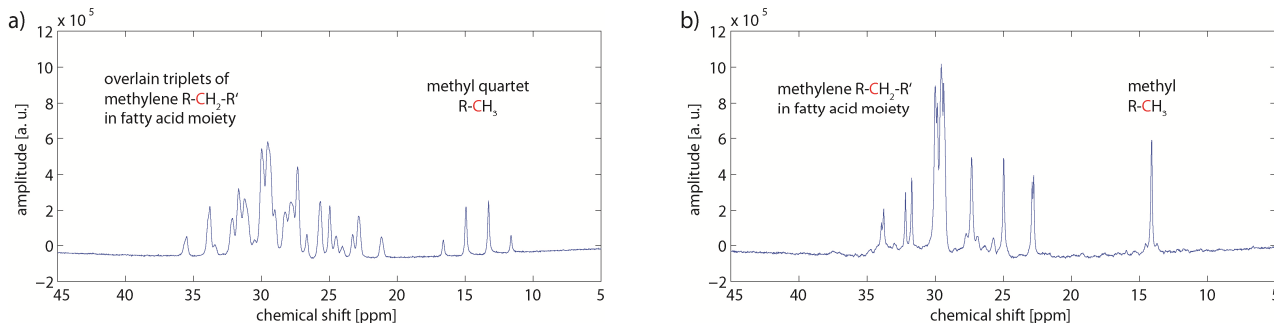


Fig. 2: B_0 -shimmed ^{13}C NMR spectra with methyl and methylene resonances of TAG in the vegetable oil phantom (^{13}C FID sequence parameter: 32 avg., TR = 3.5 s, pulse length = 0.12 ms, $\Delta f = 4$ kHz, 2048 data points, $U_{\text{pulse}} = 30$ V) (a) without decoupling and (b) with ^1H -decoupling (WALTZ-4: decoupling duration = 2 ms, DC total duration = 50 %, DC pause duration = 20 %, $U_{\text{WALTZ}} = 60$ V)

CONCLUSION: In this work a home-built $^{13}\text{C}/^1\text{H}$ double-resonant surface coil for in vivo application was developed and implemented on a 7-T whole-body tomograph. Due to optimized frequency filter circuits an acquisition of ^1H -decoupled ^{13}C NMR spectra was possible with this coil design. High resolution ^{13}C NMR spectra of a model solution with and without ^1H -decoupling were acquired in about 2 minutes. ^1H NMR spectra and images can also be obtained with this coil system.

REFERENCES: 1. Zabel H-J, et al. High-Quality MR Imaging with Flexible Transmission Line Resonators. Radiology. 1987; 165:857-859