

## Enhanced tissue classification of acute ischemic diffusion kurtosis lesion with intrinsic kurtosis heterogeneity correction

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**Purpose** Kurtosis, a measure of non-Gaussian diffusion, has been introduced as a metric for imaging a host of neurological disorders<sup>1-4</sup>. Recent animal studies of transient ischemic stroke have demonstrated that mean kurtosis (MK) lesion captures the irreversibly damaged ischemic core, and hence, delineates the standard DWI lesion for improved stratification of graded ischemic tissue injury<sup>5</sup>. However, unlike the relatively homogeneous trace diffusion image, the complexity of cerebral structure and composition leads to a heterogeneous MK map, in which the specificity of kurtosis abnormality to ischemia is somewhat compromised<sup>6</sup>. A means to minimize the intrinsic cerebral tissue MK variation would thus enhance the conspicuity of the ischemic kurtosis lesion, to in turn facilitate the practical use of kurtosis MRI in the setting of acute stroke.

**Methods** **Animal model:** Seven normal rats (n=7) and fifteen stroke rats (n=15), following a standard intraluminal middle cerebral artery occlusion (MCAO) procedure were imaged. Two MCAO rats showed minimal ischemic lesions in striatum and were excluded from the analysis. **MRI:** All experiments were conducted at a 4.7T small-bore MRI scanner after acute MCAO. We acquired perfusion (TR/TS/TE=6500/3250/14.8ms, NSA=32), diffusion (TR/TE=3250/54ms, b=250, 500, 750, 1000, 1500, 2000, 2500, and 3000 s/mm<sup>2</sup>, NSA=4), T<sub>1</sub> (IR, TI from 250 to 3000 ms, NSA=4) and T<sub>2</sub> (SE, TR/TE1/TE2=3250/30/100 ms, NSA=16) MRI. **Data Analysis:** We used Matlab. P-values less than 0.05 were considered statistically significant.

**Results and Discussion** We evaluated the relationship between MK and multivariate MRI indexes using Pearson's correlation with a Student's t distribution, excluding ventricle regions using a diffusion threshold-based mask (Fig. 1). As Fig. 1 a shows, there was little correlation between MK and MD ( $R^2<0.01$ ,  $P>0.18$ ), suggesting that MK is different from the standard MD index. The per-pixel analysis showed significant correlation between MK and FA ( $R^2=0.29$ ,  $P<0.001$ , Fig. 1 b), MK and R<sub>1</sub> ( $R^2=0.67$ ,  $P<0.001$ , Fig. 1 c), and MK and R<sub>2</sub> ( $R^2=0.13$ ,  $P<0.001$ , Fig. 1 d). Notably, the correlation between MK and R<sub>1</sub> was significantly higher than that of MD, FA and R<sub>2</sub> ( $P<0.001$ ). Because MD and FA may change substantially during acute stroke, we compared the univariate regression of MK and R<sub>1</sub> versus multiple regression of MK with R<sub>1</sub> and R<sub>2</sub>. We found the coefficient of determination was  $0.60 \pm 0.09$  (MK and R<sub>1</sub>,  $P<0.001$ ) and  $0.61 \pm 0.09$  (MK, R<sub>1</sub> and R<sub>2</sub>,  $P<0.01$ ); there was no significant difference between R<sup>2</sup> obtained by univariate regression of MK and R<sub>1</sub> and that determined by multiple regression of MK, R<sub>1</sub> and R<sub>2</sub> (Two-sample t-test,  $P>0.80$ ).

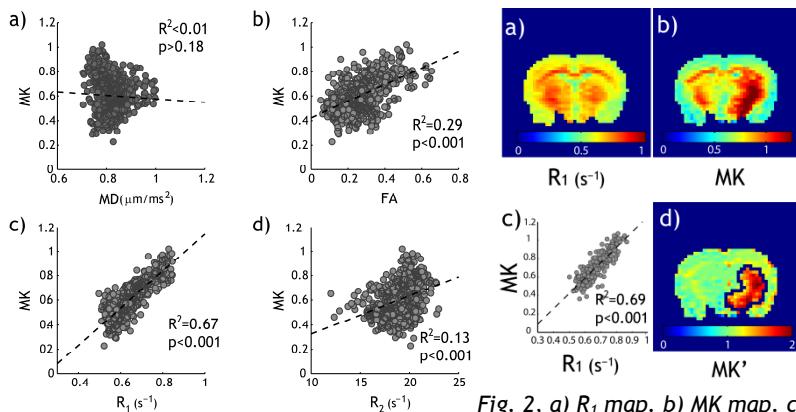


Fig. 1, Univariate regression between MK and multi-parametric MRI indexes. a) MK with MD. b) MK with FA. c) MK with R<sub>1</sub> and normal brain. d) MK with R<sub>2</sub>. Fig. 2, a) R<sub>1</sub> map. b) MK map. c) Univariate regression analysis of R<sub>1</sub> and MK (contralateral to stroke). d) modified MK' map.

Fig. 2 compares the conventional MK map and the proposed relaxation-scaled MK (MK') map in a representative normal rat. R<sub>1</sub> map shows relatively small change (Fig. 2a). The conventional MK map (Fig. 2b) shows hyperintensity in regions of the striatum and corpus callosum, indicating complex local microstructure. Fig. 2c shows the estimated MK map (MK<sub>est</sub>) using the univariate linear regression coefficients determined from MK and R<sub>1</sub>, per pixel ( $MK_{est} = 1.51 * R_1 - 0.37$ ). Fig. 2d shows the proposed relaxation-normalized MK map (i.e. MK' = MK / MK<sub>est</sub>), which was significantly more homogeneous than the raw MK map (Fig. 2b). The coefficient of variation (COV, i.e., S.D./mean) was 22.4% and 14.0% for the conventional MK and proposed MK' maps, respectively. This represented a relative COV decrease of 37.5%, confirming that the proposed MK' map can reasonably account for a substantial portion of the MK heterogeneity in the

intact brain. Using a one-tailed paired t-test ( $P<0.01$ ) we found that the kurtosis lesion volume ( $172 \pm 78$  mm<sup>3</sup>) was significantly less than that of diffusion ( $206 \pm 93$  mm<sup>3</sup>). Moreover, MD was  $0.64 \pm 0.05$  and  $0.64 \pm 0.04$  in the MD and MK' lesions, respectively, and there was no statistically significant difference ( $P=0.61$ ). Importantly, MK' was significantly different between MD and MK' lesions ( $1.58 \pm 0.10$  vs.  $1.70 \pm 0.11$ ,  $P<0.001$ ). In summary, our results demonstrate that relaxation-normalized kurtosis MRI effectively reduced the intrinsic kurtosis heterogeneity, enabling automated tissue segmentation of the kurtosis lesion during acute ischemic stroke.

**References** 1) Moseley M et al. AJNR 1990;11(3):423-9. 2) Fiehler et al. Stroke 2002;33(1):79-86. 3) Jensen JH et al. MRM 2005;53(6):1432-40. 4) Hui et al. Brain Research 2012;1451(0):100-9. 5) Cheung et al. Stroke 2012;43(8):2252-4. 6) Mori S and van Zijl P. MRM 1995;33:41-52.