## Chronic Myocardial Infarctions can be Reliably Characterized using Contrast-Free T1 Mapping at 3T

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**Target Audience** – Scientists and clinicians studying myocardial infarction

**Purpose** – Late Gadolinium Enhancement (LGE) Cardiovascular Magnetic Resonance (CMR) imaging is a powerful method to characterize myocardial infarctions (MIs). However, the requisite gadolinium infusion is contra-indicated in nearly 40% of the MI patients who also suffer from end-stage kidney disease. In this study, we tested the hypothesis whether contrast-freeT<sub>1</sub> maps at 3T can detect chronic MIs with high diagnostic accuracy relative to LGE images.

Methods - CMR Protocol: Canines (n=29) were subjected to 3 hours of full LAD occlusion followed by reperfusion. CMR was performed at 7 days (acute, AMI) and 4 months (chronic, CMI) post-MI on 19 canines at 3T and 10 canines at 1.5T. ECGtriggered breath-held 2D contrast-free T<sub>1</sub> maps (MOLLI; 8 TIs with 2 inversion blocks of 3+5 images; minimum TI=110ms; ΔTI=80ms; TR/TE=2.2/1.1ms), contrast-free T2 maps (T2-prepared SSFP; T2 preparation times = 0, 24 and 55ms; TR/TE=2.8/1.4ms) and LGE images (IR-prepared FLASH; optimal TI to null remote myocardium; TR/TE=3.5/1.75ms) of contiguous short-axis slices were acquired. Commonly used imaging parameters were slice thickness=6mm and in-plane resolution=1.3x1.3mm<sup>2</sup>. *Image Analyses:* Remote myocardium was identified as the region showing no signal hyperintensity on LGE images. Infarcted myocardium was identified on both LGE images and T<sub>1</sub> maps using Mean + 5 standard deviations (SD) criterion relative to a reference ROI drawn in the remote myocardium. Infarct size (IS) was measured as the percentage of LV volume, as well as on a segmental basis using the AHA 17-segment model. Infarct transmurality (IT) was measured as the mean extent of the infarct along 100 equally-spaced radial chords drawn on each slice. Histology: Canines were sacrificed following month 4 CMR scan and the hearts were excised. TTC and Elastin Masson's Trichrome staining were performed. Statistical Analyses: T<sub>1</sub>, T<sub>2</sub> and LGE signal intensity (LGE-SI) values were measured from remote and infarcted myocardium and compared. T<sub>1</sub> maps and LGE images were also compared for IS and IT measurements using paired t-test and Bland-Altman analysis. ROC analysis was performed to determine the diagnostic accuracy of T<sub>1</sub> maps for detecting MIs relative to LGE images.

**Results** – At 3T,  $T_1$  maps showed no difference in IS and IT relative to LGE images in CMI (IS:  $5.6\pm3.7\%$  vs.  $5.5\pm3.7\%$ , p=0.61 and IT:  $44\pm15\%$  vs.  $46\pm15\%$ , p=0.81), but overestimated IS and IT

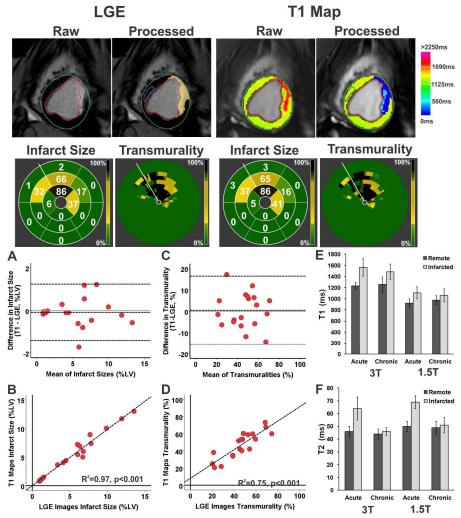


Figure 1: Representative slice-matched LGE images and contrast-free  $T_1$  maps acquired from a canine imaged at 3T (4 months post MI) are shown. Post-processed images delineating the MI territories using Mean+5SD criterion relative to remote myocardium are also shown. Hypointense core of iron deposition within hyperintense MI zone on  $T_1$  maps was manually included in the analysis (highlighted light blue pixels on the processed images). AHA 17-segment bulls-eye plots showed excellent correlations between LGE images and  $T_1$  maps for measuring infarct size (IS) and transmurality (IT). Strong agreement and correlation were observed between LGE images and T1 maps for measuring chronic IS (Bias = -0.08±0.68% (panel A) and  $R^2$ =0.97 (panel B)) and IT (Bias = 0.45±8.14% (panel C) and  $R^2$ =0.75 (panel D)) at 3T. Mean  $T_1$  of infarcted myocardium was elevated relative to remote myocardium in AMI at both 3T and 1.5T (panel E). Mean  $T_2$  of infarcted myocardium was elevated relative of remote myocardium in AMI at 3T and 1.5T (panel F).  $T_2$  values of infarcted myocardium in CMI returned to baseline levels at 3T and 1.5T.

relative to LGE images in AMI (IS:  $13.3\pm8.4\%$  vs.  $11.6\pm6.8\%$ , p=0.007 and IT:  $64\pm19\%$  vs.  $56\pm17\%$ , p=0.007). At 1.5T,  $T_1$  maps underestimated IS and IT relative to LGE images in AMI (IS:  $9.4\pm5.6\%$  vs.  $15.5\pm9.4\%$ , p<0.001 and IT:  $59\pm5\%$  vs.  $76\pm6\%$ , p<0.001) and CMI (IS:  $2.1\pm1.2\%$  vs.  $4.8\pm1.8\%$ , p<0.001 and IT:  $47\pm7\%$  vs.  $66\pm9\%$ , p<0.001). Relative to the remote territories,  $T_1$  of the infarcted myocardium was elevated in AMI (3T: p<0.001; 1.5T: p<0.001) and CMI (3T: p<0.001; 1.5T: p=0.037).  $T_2$  of the infarcted myocardium was elevated in AMI (p<0.001 at both 3T and 1.5T), but not in CMI (3T: p=0.19, 1.5T: p=0.55) indicating that myocardial edema resolved at 4 months post-MI. Histology showed extensive replacement fibrosis within the CMI territories. CMI detection sensitivity and specificity of  $T_1$  CMR were 95% and 97% respectively at 3T, and 58% and 78% respectively at 1.5T. Conclusions — Contrast-free  $T_1$  maps can reliably determine the location, size and transmurality of CMIs at 3T. Field-strength dependent native  $T_1$  elongations of replacement fibrosis within CMIs may explain the observed sensitivity differences between 1.5T and 3T.