Magnetic Resonance-Fluorescent Dual Imaging of Fluorescein Coated Gd$_2$O$_3$ Nanoparticles


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Introduction

MRI is a very useful technique in diagnosing diseases because of its high spatial resolution and good sensitivity. Detection of diseases can be further improved by using MRI contrast agents through contrast enhancement. Fluorescein coated gadolinium oxide nanoparticles are promising candidates as either T1 MRI-CL or MRI-FI dual agents because gadolinium oxide nanoparticles show a longitudinal relaxivity ($r_1$) which is much larger than those of Gd (III) -chelates while dyes generally provide a very strong fluorescent intensity. The enhanced $r_1$ of gadolinium oxide nanoparticles with respect to those of Gd (III) - chelates is due to a high density of probing Gd (III) ions in nanoparticles.

Gadolinium oxide nanoparticles must be biocompatible and completely excreted from the body through the renal system to avoid any danger such as nephrogenic systemic fibrosis. Therefore, nanoparticles should be well-coated with water-soluble and biocompatible ligands. In this work, fluorescein is conjugated to hydrophilic and biocompatible polyethyleneimine (PEI) (Mn = y1200 amu) to improve both water-solubility and biocompatibility of fluorescein through the EDC/NHS coupling method. Finally, fluorescein-PEI was conjugated to gadolinium oxide nanoparticles. We demonstrated MRI-CL dual functionality of fluorescein-PEI coated gadolinium oxide nanoparticles both in vivo and in vitro.

Materials and methods

2 mmol of GdCl$_3$. $n$H$_2$O was added to 20 mL of triethylene glycol in a three-necked flask and magnetically stirred at 80°C. Then, 6 mmol of NaOH was added and stirred for 2 h. Then, 3.5 mL of H$_2$O solution was added. After 2 h the product solution was cooled to room temperature and then washed three times with triply distilled water. Fluorescein-PEI was synthesized by using the EDC/NHS coupling method. 2 mmol of EDC and 2 mmol of NHS were added to 20 mL of PBS (pH = 6) at room temperature and under atmospheric condition. Here, a pH = 6 of PBS was obtained by slowly adding 1 mM HCl dropwise to the original PBS with pH = 7.2. After magnetic stirring for 15 min, 0.1 mmol of fluorescein was added to the solution and then the solution was magnetically stirred for 2 h. Then, 1.2 mL of PEI solution was added to the above solution with magnetic stirring for an additional 2 h to obtain fluorescein-PEI. Gadolinium oxide nanoparticles were added to the above fluorescein-PEI solution. The reaction mixture was magnetically stirred for 16 h; the product solution was transferred into a 1 L beaker containing 500 mL of triply distilled water, and then washed with triply distilled water three times.

Result and discussion

HRTEM images of fluorescein-PEI coated gadolinium oxide nanoparticles range from 2 to 6 nm. The core davg and hydrophilic core davg of fluorescein-PEI coated gadolinium oxide nanoparticles were estimated to be 3.92 and 7.5 nm, respectively. HRTEM images of fluorescein-PEI coated gadolinium oxide nanoparticles range from 2 to 6 nm. The core davg and hydrophilic core davg of fluorescein-PEI coated gadolinium oxide nanoparticles were estimated to be 3.92 and 7.5 nm, respectively. The core davg and hydrophilic core davg of fluorescein-PEI coated gadolinium oxide nanoparticles were estimated to be 3.92 and 7.5 nm, respectively.

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The magnetic properties of fluorescein-PEI coated gadolinium oxide nanoparticles were characterized by recording both M–H curves (-5 ≤ H ≤ 5 tesla) at T = 5 and 300 K and ZFC–M–T Curves (-5 ≤ T ≤ 330 K) at H = 100 Oe. The net magnetization of gadolinium oxide nanoparticles was estimated by using the net mass of gadolinium oxide nanoparticles estimated from a TGA analysis. These nanoparticles showed $r_1$ of gadolinium oxide nanoparticles with respect to those of Gd (III) - chelates is due to a high density of probing Gd (III) ions in nanoparticles.

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