

# High resolution 3D abdominal T<sub>1</sub> mapping in one breath-hold using the Look-Locker method and non-Cartesian GRAPPA acceleration

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**Target Audience** This work targets those interested in rapid measurement of relaxation times in abdominal tissues and in applications of non-Cartesian parallel imaging.

**Purpose** Quantitative knowledge of T<sub>1</sub> relaxation time provides valuable information in a variety of pathological conditions and is also necessary for quantitative perfusion measurements<sup>1</sup>. In practice, measurement of T<sub>1</sub> values can be challenging over large volumes affected by motion, such as the abdomen. Previous studies have used a variable flip angle approach to acquire full volume abdominal T<sub>1</sub> maps in multiple breath-holds<sup>2</sup>. This method is sensitive to B<sub>1</sub> field inhomogeneity and subject to relative motion between breath-holds. The Look-Locker technique is another method for rapid T<sub>1</sub> mapping, but this method combined with a Cartesian readout cannot provide high resolution 3D T<sub>1</sub> maps in short scan times due to the large volume to be covered. In this study, we applied the Look-Locker method with a stack-of-spirals k-space acquisition accelerated using through-time non-Cartesian GRAPPA reconstruction to obtain ultrafast 3D T<sub>1</sub> maps in a single clinically feasible breath-hold. The technique was tested for accuracy in phantoms and is demonstrated in normal volunteers.

**Methods** MRI experiments were performed on a Siemens 1.5T Espree scanner with 12 receive channels (a six-channel body array coil and 6 channels from the spine array). The inversion-recovery Look-Locker method was combined with a stack-of-spirals trajectory and through-time non-Cartesian GRAPPA to accelerate data acquisition. The scan was divided into four segments (four inversion recovery periods, each of 2.7 sec) with a pause of 3.5 sec between segments. A total of 24 partitions (32 total partitions, partial Fourier 6/8) were divided into four segments and acquired in an interleaved manner. To meet the Nyquist criterion, a total of 48 spiral interleaves in-plane are required. To accelerate the scanning, a reduction factor of four was used in-plane and then reconstructed using 3D through-time non-Cartesian GRAPPA<sup>3</sup>. A GRAPPA kernel of size 2 × 3 was used in the spiral arm × readout direction. To calculate the GRAPPA weights, a reference scan of eight fully sampled 3D volumes (~77 sec) was acquired during free breathing. Overall, eight T<sub>1</sub>-weighted 3D volumes were obtained with inversion times from 240 to 2600 ms. Other parameters were: FOV= 40×40 cm; matrix size 208×208 for an effective in-plane resolution of 1.9 mm; TR 4.5 ms; TE 0.6 ms; flip angle 7°; partition thickness 4 mm. Images were reconstructed offline using Matlab and gridding was performed using non-uniform Fourier Transform (NUFFT)<sup>4</sup>.

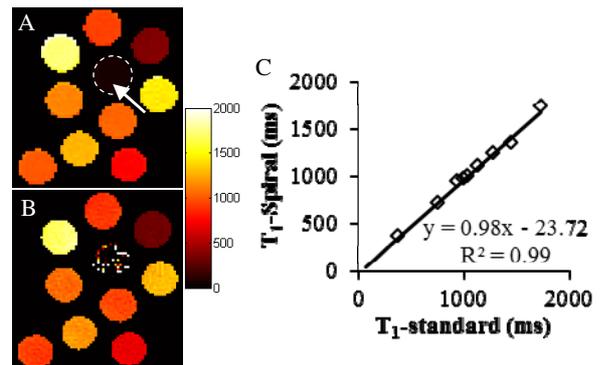


Fig. 1. T<sub>1</sub> maps of multi-compartment phantoms acquired using (A) inversion-recovery single-echo spin echo (TR: 6s) and (B) inversion-recovery stack-of-spirals method. The arrow points to a vial with T<sub>1</sub> of only 70 msec. (C) Comparison of T<sub>1</sub> values from the two sequences.

The accuracy of the T<sub>1</sub> measurement was first validated using a phantom containing several vials with varying concentrations of GdCl<sub>3</sub> and agarose. T<sub>1</sub> values measured with inversion-recovery single-echo spin-echo sequence (TR: 6 s; seven inversion times between 23 ms to 3000 ms) were used as the gold standard reference. After phantom validation, five asymptomatic volunteers were scanned. The overall acquisition time for one T<sub>1</sub> map of the whole abdomen with the above spatial resolution was 21 seconds.

**Results and Discussion** Results from the phantom study suggest that T<sub>1</sub> values acquired with the spiral sequence agree well with the results from an IR spin echo sequence (Fig. 1), with the exception of one vial. The T<sub>1</sub> of this vial was ~70 ms, which is extremely short, and unlikely to be encountered in most practical non-enhanced clinical settings.

Figure 2 shows representative T<sub>1</sub>-weighted images along various points on the inversion recovery curve, and a corresponding T<sub>1</sub> map of one slice acquired from a normal subject. Average T<sub>1</sub> values of different tissues from the five subjects are summarized in Table 1, all in excellent agreement with the literature<sup>5</sup>.

**Conclusion** In this study, a high resolution 3D abdominal T<sub>1</sub> mapping technique was developed using the Look-Locker method, a stack-of-spirals trajectory and through-time non-Cartesian GRAPPA. This technique allows fast and accurate T<sub>1</sub> mapping of the whole abdomen in one breath-hold without the need for B<sub>1</sub> mapping or image registration.

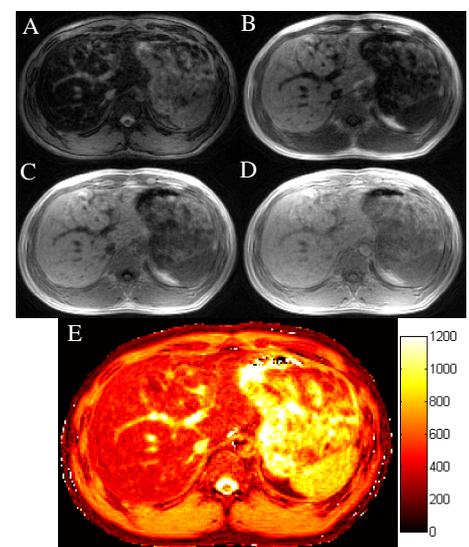


Fig. 2. (A-D) T<sub>1</sub>-weighted images of one slice at different inversion times of 243, 587, 931 and 2652 ms. (E) Corresponding T<sub>1</sub> map.

Tab. 1. T<sub>1</sub> relaxation times (ms) for different tissues. Values are means ± standard deviation.

Tissue	T <sub>1</sub> relaxation time (ms)
Liver	545 ± 78
Kidney - Medulla	1384 ± 95
Kidney - Cortex	802 ± 26
Spleen	1001 ± 98
Skeletal muscle	805 ± 50
Fat	256 ± 22

## References

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