

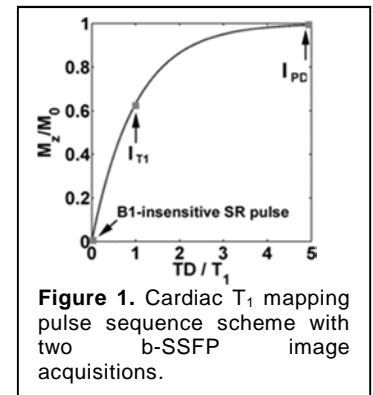
# Quantitative MRI Assessment of LV Structural Remodeling and Fibrosis Formation in Canine Models of Chronic Atrial Fibrillation

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**INTRODUCTION:** Atrial fibrillation (AF) is a multi-faceted, progressive disease that, if left untreated, could lead to increased risk of strokes, hospitalizations, heart failure, and left ventricular (LV) dysfunction. The mal-adaptive remodeling (i.e., cardiac fibrosis) of the LV caused by AF is clinically important, because the LV is the cardiac chamber that most strongly correlates with survival [1]. Despite the importance of AF-induced LV dysfunction, it is under-diagnosed clinically, and its mechanisms are not clearly understood. To date, no study has confirmed the development of LV fibrosis induced by irregular rhythm of AF. Late gadolinium enhanced (LGE) cardiac T<sub>1</sub> mapping [2-5] is the only proven method for quantification of diffuse cardiac fibrosis, where LGE T<sub>1</sub> directly correlates with the amount of contrast agent contained in the expanded extracellular matrix. We sought to measure the development of LV fibrosis induced by irregular rhythm in a canine model with chronic AF, using a customized LGE cardiac T<sub>1</sub> mapping pulse sequence.

**METHODS:** Our research center is conducting a longitudinal study of canine models to study the relationship between myocardial fibrosis and AF. For the longitudinal study, mongrel dogs were implanted with a pacemaker to induce chronic AF via rapid atrial pacing (RAP, 30 Hz) [6], and each animal was imaged in sinus rhythm (after cardioversion if required) and under anesthesia on 3T scanners (TIM Trio and Verio, Siemens Healthcare, Erlangen, Germany) at baseline and once per month (up to 20 months) after RAP. We enrolled eleven dogs at different stages of AF for this study. As such, the range of temporal data points per dog was 1 – 5. For LGE T<sub>1</sub> mapping, we developed a new cardiac T<sub>1</sub> mapping pulse sequence (Fig. 1) based on B<sub>1</sub>-insensitive saturation recovery (SR) magnetization preparation and two single-shot balanced steady-state free precession (b-SSFP) image acquisitions (proton density (I<sub>PD</sub>) and T<sub>1</sub>-weighted (I<sub>T1</sub>)) with centric k-space ordering, where T<sub>1</sub> is calculated from a ratio of I<sub>T1</sub> and I<sub>PD</sub> to cancel T<sub>2</sub> effects. In addition, this pulse sequence is insensitive to arrhythmia and rapid (2-3 heart beats per 2D image). We performed T<sub>1</sub> mapping at baseline and 15 min post contrast agent (0.15 mmol/kg of Gd-BOPTA) administration. T<sub>1</sub> maps were calculated from I<sub>T1</sub> and I<sub>PD</sub>, using the Bloch equation governing T<sub>1</sub> relaxation of an ideal SR experiment:  $T_1 = -TD/\ln(1 - I_{T1}/I_{PD})$ . The relevant imaging parameters were: spatial resolution = 1.8 mm X 1.8 mm, temporal resolution = 217 ms, and TD = 600 ms. T<sub>1</sub> maps were analyzed to calculate blood T<sub>1</sub> and myocardial T<sub>1</sub> values at baseline and post contrast; each T<sub>1</sub> was determined by averaging the region of interest segmented manually on LV myocardium and blood pool in short axis view using a customized software in MATLAB (MathWorks, Inc., Natick, MA). The corresponding partition coefficient (λ) [4,5] was calculated as:  $\lambda = \Delta R_{1, Myocardium} / \Delta R_{1, Blood}$ , where  $R_1 = 1/T_1$  and Δ is difference between post-contrast and pre-contrast. We also acquired biopsy samples from the right ventricular (RV) septal wall via a catheter. The expanded extracellular space was assessed qualitatively by an experienced pathologist, and fibrosis severity was classified into four grades: I (normal, <10% fibrosis of extracellular volume), II (mild, 10-20%), and III (severe, >20%).

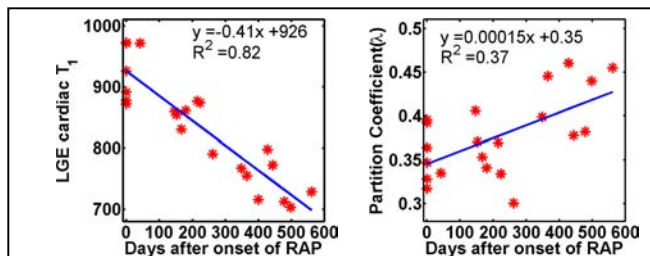


**Figure 1.** Cardiac T<sub>1</sub> mapping pulse sequence scheme with two b-SSFP image acquisitions.

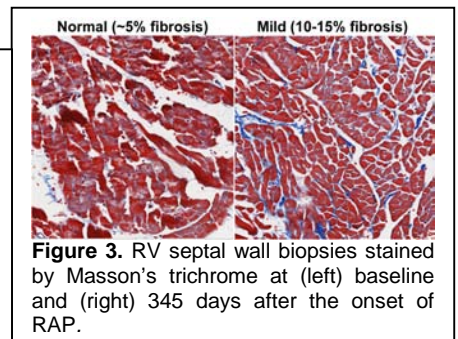
**RESULTS:** LGE cardiac T<sub>1</sub> values decreased with days after the onset of RAP, whereas λ increased with days after the onset of RAP (Fig. 2). These two results confirmed that myocardial fibrosis increased with days after the onset of RAP. In addition, these MRI findings were corroborated with histological assessment of Masson's trichrome stained tissue specimens in RV (Fig. 3).

**CONCLUSIONS:** Our experimental were rate controlled (maximum heart rate: 96.4 ± 12.3 bpm) and yet developed LV fibrosis, confirming the impact of irregular rhythm on LV fibrosis development and progression. New cardiac T<sub>1</sub> mapping method can be used to non-invasively assess LV fibrosis induced by AF. The correlation between LGE cardiac T<sub>1</sub> and days after the onset of RAP was stronger than that between λ and days after the onset of RAP, suggesting λ has more inter-subject variability.

**REFERENCES:** [1] Curtis, JP, et al. J AM Coll Cardiol 2003; 42(4):736-742. [2] Mewton, N, et al. J Am Coll Cardiol 2011; 57(8):891-903. [3] Messroghli DR, et al. MRM 2004; 52(1):141-146. [4] Broberg CS, et al. Circ Cardiovasc Imaging 2010; 3(6):727-34. [5] Jerosch-Herold M, et al. Am J Physiol Heart and Circ Physiol 2008; 295(3):H1234-H1242. [6] Nishida K, et al. Europace 2010; 12(2):160-172.



**Figure 2.** LGE cardiac T<sub>1</sub> and λ with days after the onset of RAP



**Figure 3.** RV septal wall biopsies stained by Masson's trichrome at (left) baseline and (right) 345 days after the onset of RAP.