

# Frequency band-selective spiral CSI: application to imaging cardiac metabolism with hyperpolarized [2-<sup>13</sup>C]pyruvate

Sonal Josan<sup>1,2</sup>, Ralph Hurd<sup>3</sup>, Yi-Fen Yen<sup>2</sup>, Adolf Pfefferbaum<sup>1,4</sup>, Daniel Spielman<sup>2</sup>, and Dirk Mayer<sup>1,2</sup>

<sup>1</sup>SRI International, Menlo Park, CA, United States, <sup>2</sup>Radiology, Stanford University, Stanford, CA, United States, <sup>3</sup>GE Healthcare, <sup>4</sup>Psychiatry and Behavioral Sciences, Stanford University, Stanford, CA, United States

## Introduction

Spectroscopic imaging with hyperpolarized <sup>13</sup>C substrates has been widely used to measure metabolic processes in real time in vivo. The most widely used substrate, [1-<sup>13</sup>C]pyruvate (Pyr), allows the assessment of pyruvate dehydrogenase (PDH) flux, which converts pyruvate to acetyl-CoA releasing the <sup>13</sup>C label as <sup>13</sup>CO<sub>2</sub>/<sup>13</sup>C-bicarbonate. There has also been growing interest in using hyperpolarized [2-<sup>13</sup>C]Pyr, to follow the <sup>13</sup>C label into downstream metabolic products including [5-<sup>13</sup>C]glutamate (Glu), which is in fast exchange with α-ketoglutarate in the tricarboxylic acid (TCA) cycle, [1-<sup>13</sup>C]citrate (Cit), [1-<sup>13</sup>C]acetylcarnitine (ALCAR) and [1,3-<sup>13</sup>C]acetoacetate (Aca)<sup>1-5</sup>, indicating incorporation of acetyl-CoA into different metabolic pathways. Previous studies with hyperpolarized [2-<sup>13</sup>C]Pyr and [1,2-<sup>13</sup>C]Pyr<sup>1-3</sup> used a surface coil for localization, obtaining spectra from the entire sensitive volume. Chemical shift imaging (CSI) with [2-<sup>13</sup>C]Pyr is challenging given the wide spectral dispersion of the resonances, e.g. ~150 ppm from [2-<sup>13</sup>C]alanine (Ala) to [2-<sup>13</sup>C]Pyr, i.e. ~4800 Hz at 3T. Hence, a slice-selective acquisition<sup>4</sup> suffers from severe chemical shift displacement artifact. This work uses a spectrally selective excitation to perform 3D CSI of frequency sub-bands containing metabolites of interest. The frequency sub-band from 170-185 ppm containing Glu, Cit, ALCAR, Aca along with [1-<sup>13</sup>C]Pyr is of particular interest. Dynamic data were acquired alternately from multiple sub-bands in vivo in rat heart.

## Methods

All measurements were performed on a GE 3T MR scanner with a high-performance insert gradient coil (500 mT/m, 1865 mT/m/ms) using a custom-built <sup>13</sup>C transmit/receive surface coil (dia=28 mm) placed over the heart. Three rats were injected i.v. with approximately 3 ml of 80-mM solution of [2-<sup>13</sup>C]Pyr, which was hyperpolarized using HyperSense (Oxford Instruments, UK). Dichloroacetate (DCA) infusion (150 mg/kg) was administered i.v. prior to Pyr injection to stimulate PDH activity and allow Aca detection<sup>3,5</sup>.

A spatially non-selective RF pulse was used (4-ms long, 10° flip angle, passband=190 Hz with 1% ripple). The spectral profile is shown in Fig. 1. With the passband centered approximately midway between Glu and [1-<sup>13</sup>C]Pyr, passband (referred to as Glu band hereon) magnitude at Glu and <sup>13</sup>C<sub>1</sub>-Pyr resonances was 90% and [2-<sup>13</sup>C]Pyr signal was suppressed (ripple ~10<sup>-5</sup> at 968 Hz from passband center).

Dynamic 3D <sup>13</sup>C data were acquired with FOV=80×80×60 mm<sup>3</sup>, 5×5×5 mm<sup>3</sup> nominal resolution, 12 z-phase-encoding steps, 2 x-y spiral interleaves, spectral width=607 Hz, 64 spectral points, T<sub>acq</sub>=2.8s. Imaging started at the same time as Pyr injection. 24 time-points were acquired every 2.8s with the RF passband alternately placed at Glu and [2-<sup>13</sup>C]Pyr bands (or Glu and [2-<sup>13</sup>C]lactate (Lac) bands) for successive acquisitions. For the Lac band, the transmit frequency was centered on the down-field peak of the doublet which led to <1% ripple at the Ala doublet to avoid signal contamination from Ala into Lac given the 607 Hz spectral width.

## Results and Discussion

Figure 2 shows representative time-averaged <sup>13</sup>C metabolic maps of [2-<sup>13</sup>C]Pyr, Glu, ALCAR, Aca and Lac from a slice through the heart and superimposed onto <sup>1</sup>H SPGR images. The Lac image is from a separate injection. The spectrum for the Glu band is shown in Fig. 3 along with metabolite time-courses, both from an ROI in the heart. All results were acquired 15 min post-DCA except Lac, which was 2 h post-DCA.

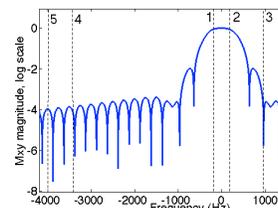


Figure1: Spectral profile of the RF pulse. Lines 1 and 2 indicate chemical shifts of <sup>13</sup>C<sub>1</sub>-Pyr and Glu in the passband with ALCAR, Aca and Cit located between them. Signal from <sup>13</sup>C<sub>2</sub>-Pyr (line 3) is suppressed. Lines 4 and 5 mark <sup>13</sup>C<sub>2</sub>-Lac and <sup>13</sup>C<sub>2</sub>-Ala respectively.

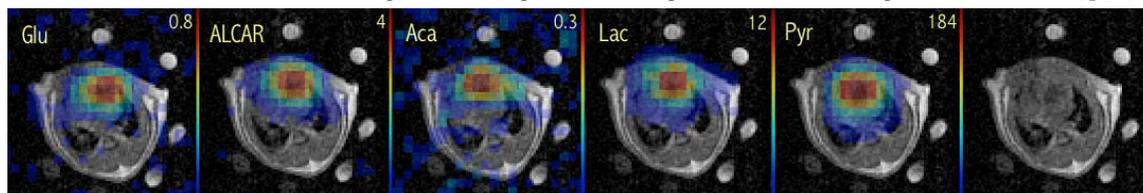


Figure2: Time-averaged <sup>13</sup>C metabolic maps of a slice through the heart from a 3D dataset.

Signal from <sup>13</sup>C<sub>1</sub>-Pyr (at 1% natural abundance) in the Glu band may be sufficient to provide an estimate of the substrate signal. All 3 sub-bands were not acquired in one dataset as interleaving multiple sub-band acquisitions would lower temporal resolution. While the current implementation performs CSI on all spectral sub-bands, Pyr and Lac can be acquired using imaging rather than a spectroscopic readout to reduce scan time. Given high inflow in heart and limited excitation profile of the surface coil, a 10° flip angle with 24 excitations/volume was used, though a smaller flip angle may be more SNR optimal for other organs. The sequence also allows using different flip angles for Pyr and the metabolic products. As a non-selective RF excitation was employed to avoid chemical shift displacement artifact, the sensitivity profile of the receive coil determines the FOV, in particular the number of slice-encoding steps.

## Conclusion

This work presents a sequence for 3D CSI of hyperpolarized [2-<sup>13</sup>C]Pyr using frequency sub-band selective excitation and demonstrates results from an in vivo application to rat heart. It provides a method for dynamic volumetric measurement of metabolism and allows imaging of the downstream metabolic products of acetyl-CoA following a single [2-<sup>13</sup>C]Pyr injection.

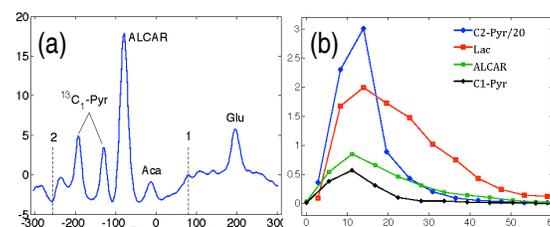


Figure3: (a) Time-averaged spectrum showing Glu, Aca, ALCAR and natural abundance <sup>13</sup>C<sub>1</sub>-Pyr doublet. Line 1 shows chemical shift of Cit, though it did not have sufficient SNR here. Line 2 indicates <sup>13</sup>C<sub>2</sub>-Pyr signal excited by RF stopband ripples aliased into Glu band. Baseline roll in spectrum is from linear phase correction. (b) Metabolite signal time-courses from heart ROI. Lac was acquired in a separate injection. SNR of Glu and Aca were insufficient to plot time-courses.

**References:** [1] Schroeder et al, Circ Cardiovasc Imaging 2012, p201 [2] Chen et al, NMR Biomed 2011, p305 [3] Josan et al, ISMRM 2012, p4322 [4] Park et al, ISMRM 2012, p4323 [5] Hu et al, ISMRM 2012, p4331

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