

# The anomalous diffusion parameter $\alpha$ provides the most relevant information of structural complexity in heterogeneous media

Marco Palombo<sup>1,2</sup>, Andrea Gabrielli<sup>3</sup>, Giancarlo Ruocco<sup>1,2</sup>, and Silvia Capuani<sup>1,2</sup>

<sup>1</sup>Physics Department, Sapienza University, Rome, Rome, Italy, <sup>2</sup>CNR IPCF UOS Roma, Sapienza University, Rome, Rome, Italy, <sup>3</sup>ISC-CNR, Rome, Rome, Italy

**Target audience.** This study is addressed to researchers involved in the development of advanced diffusion NMR technique to probe microstructures in tissue.

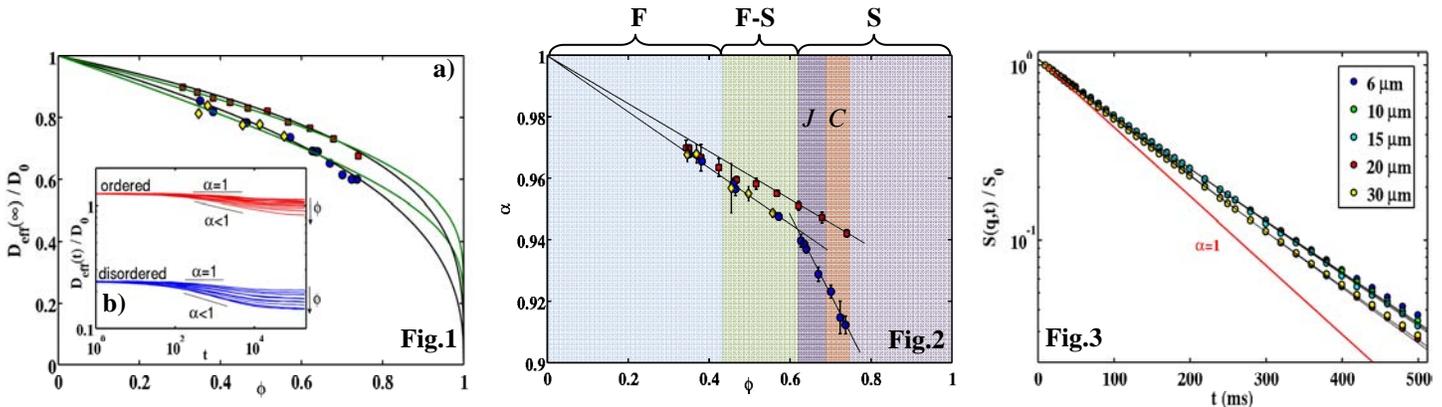
**Purpose.**  $\alpha$  anomalous diffusion parameter, which quantifies sub-diffusion processes<sup>1</sup>, is easily measurable by using diffusion-time varying NMR techniques<sup>1,2</sup>. Our aim was to show that  $\alpha$  provides microstructural information related to the disorder degree of complex systems. Toward this goal we performed numerical simulations to investigate diffusion as a function of time,  $D(t)$ , and  $\alpha$  behavior as a function of the sphere-density  $\phi$  in micro-beads mono-dispersed in water. Then, by employing a diffusion-time varying pulse field gradient (PFG) technique<sup>1</sup> we obtained experimental results and compared them with results from numerical simulations.

**Methods. Theory:** The PFG signal attenuation,  $S(q,\Delta)$ , which depends on both the diffusion gradient strength,  $g$  (through the wave vector  $q = 1/(2\pi)\gamma g \delta$  with  $\gamma$  the gyromagnetic ratio and  $\delta$  the pulse gradient duration) and the diffusion time  $\Delta$ , is the Fourier Transform (FT) of the motion propagator (MP). When the MP is Gaussian,  $S(q,\Delta)$  as a function of  $b=q^2\Delta$  follows a mono-exponential decay. On the other hand, when the MP is not Gaussian,  $S(q,\Delta)$  deviates from the mono-exponential decay. It is well known that  $D(t)$  in heterogeneous systems shows three different behaviours: it is constant and equal to bulk diffusivity  $D_0$  (when the MP is Gaussian) for very short diffusion times,  $t$ ; it is not constant:  $D(t) \propto t^{(\alpha-1)}$  with  $\alpha < 1$  (when the MP is non-Gaussian and water diffusion is sub-diffusive) for short  $t$ ; and it is constant again but equal to  $D(\infty) < D_0$  for long  $t$ .

**Simulations:** three dimensional (3D) molecular dynamics simulations with periodic boundary conditions were performed to mimic systems comprised of mono-sized hard spheres ordered on an fcc lattice (ordered system) and randomly displaced at different  $\phi$  values, ranging from 0.33 to 0.74 (disordered system at different degree). Water diffusion in these 3D obstructed media was modeled as a 3D random flight process by employing a Monte Carlo algorithm. To estimate the ratio  $D_{eff}(t)/D_0$ , where  $D_{eff}(t) = \langle r^2(t) \rangle / (6t)$ , with  $\langle \cdot \rangle$  the ensemble average and  $r(t)$  the particle space displacement,  $5 \cdot 10^4$  trajectories were collected.

**Experiments:** five 10mm NMR tubes were filled with polystyrene beads of diameters:  $30.0 \pm 1.0$ ,  $20.0 \pm 1.0$ ,  $15.0 \pm 1.0$ ,  $10.00 \pm 0.50$  and  $6.00 \pm 0.50$   $\mu\text{m}$  mono-dispersed in a solution of Tween 20 at  $10^{-6}\text{M}$  and deionized water, and investigated 4 months after their preparation at fixed temperature of 293K.

The fractional exponent  $\alpha$  was measured by collecting  $S(q,\Delta)$  as a function of  $\Delta$  and by using the asymptotic expression of the FT of the MP for the sub-diffusive regime derived in <sup>1</sup>:  $S(q,\Delta) \propto \exp(-Kq^2\Delta^\alpha)$  [1], which hold when  $q^2 \ll 1/(K\Delta^\alpha)$  is kept constant, with  $K$  a generalized diffusion constant. A spectroscopic PFG Stimulated Echo (PFG-STE) sequence with  $\delta=2.2\text{ms}$ ,  $g=0.10\text{T/m}$  (i.e.  $q=11240\text{m}^{-1}$ ) along x, y and z directions,  $TR=2.5\text{s}$ ,  $NS=32$  and 48 values of  $\Delta$  in the range (10–500)ms was used to extract the  $\alpha_{i=x,y,z}$  values. Then the mean value,  $\alpha$ , was computed by averaging over the three directions. A second spectroscopic PFG-STE with  $\Delta\delta=400/2.2\text{ms}$ ,  $TR=2.5\text{s}$ ,  $NS=16$  and 48 gradient amplitude steps from 0.026 to 1.02T/m along x, y and z directions were used to measure the effective diffusion coefficient at long time



$D_{eff}(\infty)$ , from the slope of  $\ln(S(q,\Delta)/S_0)$  at low  $q$  values along each direction and then averaging over the three directions. A Spin Echo imaging sequence with  $TR=2.5\text{s}$ , 48 values of  $TE$  in the range (3–130)ms,  $NS=16$ ,  $STH=1\text{mm}$ , field of view  $FOV=8 \times 8\text{mm}$  and an in plane resolution of  $62.5\mu\text{m}$  were used to estimate  $\phi$  in each sample, as described in <sup>3</sup>.

**Results.**  $D_{eff}(\infty)/D_0$  vs  $\phi$  from both simulations and experiments is shown in Fig.1a. Red, blue and yellow data points represent the fcc ordered simulated samples, the disordered simulated samples and the experimental values, respectively. The lines represent the theoretical relations by Lerman<sup>4</sup> (green) and Boudreau<sup>5</sup> (black) derived from local geometrical properties of media. Fig.1b shows the simulated time behavior of  $D_{eff}(t)/D_0$  vs  $t$  (in simulation units, arbitrarily shifted to improve readability) with the behaviors when  $\alpha=1$  and  $\alpha<1$  displayed.  $\alpha$  values vs  $\phi$  obtained from simulation and experimental data is shown in Fig.2 where red, blue and yellow data points represent the fcc ordered simulated samples, the disordered simulated samples and the experimental values, respectively. The graph in Fig.3 shows  $S(q,t)/S_0$  vs  $t=\Delta\delta/3$ . The red line represents the  $S(q,t)/S_0$  vs  $t$  behavior when  $\alpha=1$ , while the black lines represent the relation [1] with  $\alpha<1$  fitted to the experimental data for all the investigated samples (see the inserted panel in Fig.3).

**Discussion.** The simulated ordered (red points) and disordered (blue points) systems mimic very well the samples investigated (see Fig.1a). Moreover, both measured (in yellow) and simulated (in blue and in red) values of  $D_{eff}(\infty)/D_0$  perfectly lie on the theoretical curves predicted in <sup>4,5</sup>. From Fig.3 it is evident that the theoretical relation [1] well fit to the data and in Fig.1b) it is possible to clearly distinguish the three diffusion regimes typically observed in heterogeneous media. The main results of this work are summarized in Fig.2. By analyzing the behavior of  $\alpha$  as a function of  $\phi$  it is possible to assert that  $\alpha$  value quantifies global structural complexity and enables a classification of different kinds of disorder. Indeed,  $\alpha$  values in Fig.2 obtained in micro-beads samples allow to observe the jamming transition occurring at  $\phi \approx 0.6$ , the full jamming state region J, and allow to classify all the microscopic states of the systems: from random fluid state, F ( $\alpha > 0.96$ ) to mixed fluid-solid state, F-S ( $0.94 < \alpha < 0.96$ ) up to crystal, C, and solid state in general, S ( $\alpha < 0.94$ ). On the other hand,  $D_{eff}(\infty)/D_0$  is only affected by local properties, as suggested by results in Fig.1a). As a consequence  $D_{eff}(\infty)/D_0$  does not provide the most relevant information of structural complexity. Moreover, it is possible to measure  $\alpha$  in a faster way compared to  $D_{eff}(t)/D_0$  vs  $t$  measurement, by performing a  $\Delta$ -varying PFG experiment<sup>1</sup>. Last but not least, the spectroscopic protocol to measure  $\alpha$  is easily convertible in an imaging protocol<sup>2</sup>.

**Conclusion.** In this work we demonstrated that unlike conventional tortuosity investigations based on long diffusion time behavior of  $D(t)/D_0$ ,  $\alpha$  quantifies the global structural complexity (disorder) of heterogeneous systems. Moreover, we show here that  $\alpha$  can be measured by using  $\Delta$ -varying PFG experiment<sup>1</sup> which is faster than the diffusion time behavior of  $D(t)/D_0$  study. As a consequence we speculate that our approach could be used as a new tool to probe changes in microstructural properties in healthy and pathological tissues.

**References.** <sup>1</sup>Palombo M, Gabrielli A, De Santis S et al. Spatio-temporal anomalous diffusion in heterogeneous media by NMR. J. Chem. Phys. 2011;135:034504-034511. <sup>2</sup>Capuani S, Palombo M, Gabrielli A, et al. Spatio-temporal anomalous diffusion imaging: results in controlled phantoms and in excised human meningiomas. Magn. Reson. Imag. 2012, in press, doi: <http://dx.doi.org/10.1016/j.mri.2012.08.012>. <sup>3</sup>Turney MA, Cheung MK, McCarthy MJ et al. Magnetic resonance imaging study of sedimenting suspensions of noncolloidal spheres. Phys. Fluids 1995;7(5):904-911. <sup>4</sup>Lerman A. Geochemical processes: water and sediment environments, 1979, Wiley, New York. <sup>5</sup>Boudreau PB. The diffusive tortuosity of fine-grained un lithified sediments. Geochim. Cosmochim. Acta 1996;60:3139-3142.