

Design of a four-channel array coil for dual high-resolution rat knee MR Imaging

Anne-Laure Perrier¹, Jean-Christophe Goebel¹, Astrid Pinzano², Emilie Roeder², Pierre Gillet², Denis Grenier¹, and Olivier Beuf¹
¹Creatis, Villeurbanne, France, ²PPIA, Vandoeuvre-les-Nancy, France

Introduction

In Magnetic Resonance Imaging (MRI), multi-channel coils are extensively used to improve Signal-to-Noise Ratio (SNR) in order to increase spatial and/or temporal image resolution. Recent decoupling techniques based on common conductor that do not require additional preamplifier for the decoupling between elements was achieved for the conception of two-channel surface transmitter coils (1-2). In this paper, based on this common conductor decoupling technique (3), a topology of a four-channel coil was described. Based on this concept, a four-channel surface receiver coil was designed to achieve simultaneous acquisition of both rat knee joints at 7T.

Material and Methods

The four-channel coil topology is described in Fig.1. The L_c - C_c and L_d - C_d sections, tuned to have null impedances at the operating frequency are departing the ground plane to black point 3. These perfect theoretical reports of ground plane in point 3 guarantee a perfect electrical decoupling between channels. A four-channel surface coil was designed for simultaneous imaging of both rat knee joints on a Bruker 7T Biospec MR scanner (Bruker, Ettlingen, Germany). Each element of the coil consists in a rectangular loop with $14 \times 15 \text{ mm}^2$ internal and $22 \times 23 \text{ mm}^2$ external dimensions. To decouple the receiver coil from the transmitter coil, each loop integrates an active decoupling circuit made with one Temex DH80055 PIN diode. Matching of each loop to 50Ω at $f_0=300 \text{ MHz}$ was realized using varicap diodes BB149 (Philips Semiconductors) for C_a and C_e capacitors.

$|S|$ parameter measurements of the four-channel surface coil (Fig 2 a)) were carried out with an Agilent E5071C four-port VNA (Agilent Technologies Inc., Santa Clara, CA, USA). The coil is matched in loading conditions using two cylindrical phantoms filled with saline water solution (NiSO₄ 1.25 g/L and NaCl 5 g/L) to mimic rat legs. HR-MR images of the rat knees were obtained using a 3D FLASH sequence with the following parameters: 30° flip angle, 50 ms TR, 3.6 ms TE, 27.8 kHz receiver bandwidth. A total of 256 partitions (98 μm thick) were acquired using a double slab volume selection, one for each knee, with a FOV of $1.25 \times 1.88 \text{ cm}^2$ and an acquisition matrix size of 256×384 . Because these large data set is not handle by the 32-bits Bruker paravision 5.1, a home-made script (Matlab 7.13a, Mathworks, Milwaukee, USA) was employed to finally obtain the reconstructed slices (in-plane pixel: $49 \times 49 \mu\text{m}^2$, thickness: 98 μm).

Results

Measured $|S_{ii}|$ parameters show a coil matching for each loop better than -30 dB at 300 MHz; $|S_{ij}|$ parameters better than -17 dB characterizing a good enough decoupling between loop pairs. Measured quality factors of each loop were 42, 40, 41 and 43 respectively. Fig. 2 b) shows a representative image of the left and right rat knee, respectively. To our knowledge, the voxel size reported here represents the highest spatial resolution achieved in vivo on two rat knee joints in for an acquisition time of 1h22min.

Conclusion

An equivalent electrical circuit of a four-channel NMR surface coil based on common conductor decoupling technique was proposed. The topology allowed good matching and good decoupling between elements without the use of additional low input impedance preamplifier and without additional capacitive network. The design of a four-channel surface coil with a particular wave-like topology for the simultaneous two rat knees imaging was realized at 300 MHz. The capacitor adjustments permit to obtain decoupling better than -17 dB between all element pairs. To our knowledge, this coil represents the first four-channel NMR surface coil based on common conductor not using the preamplifier decoupling technique. Performance of the coil was proved through the simultaneous HR-MRI of both knees joint of a rat. Voxel size of $49 \times 49 \times 98 \mu\text{m}^3$ was obtained for a 1h22min acquisition time. In future works, similar four-channel coils build with mechanical variable capacitors could be used as transceiver coil. In this case each channel phase and magnitude could be driven to achieve multi-transmit.

References

1. D. Gareis et al., Concepts M.R. Part B, M.R. Eng. **29B**:20-27 (2006).
2. M.A. Dieringer et al., JMRI **33**:736-41 (2011).
3. A.L. Perrier et al., IEEE Sensors Jour. **12**:1801-08 (2012).

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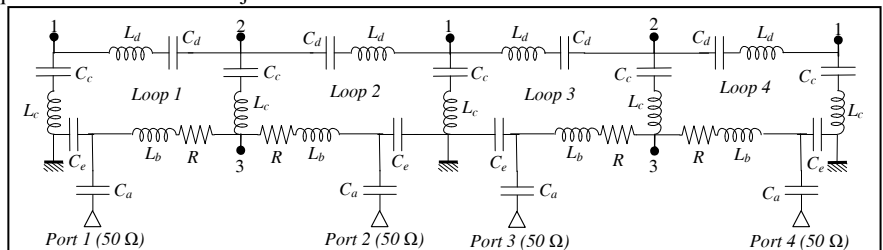


Fig. 1: Equivalent electrical circuit of a four-channel coil based on common conductor decoupling.

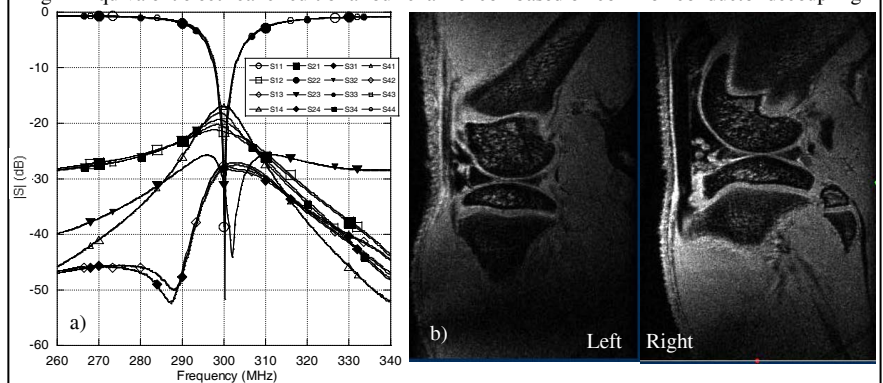


Fig. 2: a) $|S|$ parameters measurements. b) Rat knee imaging.