

Sparse Tikhonov-Regularized SENSE MRI Reconstruction

Il Yong Chun¹ and Thomas Talavage^{1,2}

¹School of Electrical and Computer Engineering, Purdue University, West Lafayette, Indiana, United States, ²Weldon School of Biomedical Engineering, Purdue University, West Lafayette, Indiana, United States

INTRODUCTION: The reconstruction of MRI data acquired using parallel approaches can be considered as solving a linear system formulated through the sensitivity encoding (SENSE) approach in the image domain [1]. Under this approach, the system can become ill-conditioned as the reduction factor increases, and residual aliasing artifacts and noise amplification become more significant. Regularization represents an important technique to overcome this problem. A well-known regularization method is Tikhonov regularization [2]; however, direct Tikhonov regularization is computationally demanding, especially for obtaining the optimal regularization parameter [2]. Such a limitation is expected to grow with SENSE reduction factor. Here, we present a pre-computation-allowable sparse Tikhonov-regularized SENSE MRI reconstruction technique based on QR decomposition, fast regularization parameter estimation using a new L-curve [4], and sparse matrix representation.

METHOD: Our approach to Tikhonov-regularized SENSE reconstruction consists of “pre-computation” and “reconstruction” steps for the full-FOV image, x , from the reduced-FOV image, y . The reduced-FOV image is a folded version of the full-FOV image and formulated as $y = Ax$, where A is a folding matrix. Considering SNR optimization from [1] and [2], this system can be represented as $\tilde{y} = \tilde{A}x$, with whitened observation $\tilde{y} = \Lambda^{-1/2}Q^H y$, whitened folding matrix $\tilde{A} = \Lambda^{-1/2}Q^H A$, receiver noise covariance matrix $\Psi = Q\Lambda Q^H$, and H denotes the transposed complex conjugate. From this, the Tikhonov-regularized solution can be written as $x^* = \underset{x}{\operatorname{argmin}}\{\|\tilde{A}x - \tilde{y}\|_2^2 + \lambda^2\|L(x - x_0)\|_2^2\}$, where x_0 is the prior information of x ,

L is the Tikhonov matrix, and λ^2 is a regularization parameter. The analytical Tikhonov-regularized solution in matrix form is $x^* = V\Gamma U^H \tilde{y} + V\Phi U^H x_0$ (**Eq 1**), where $L = I$, $\tilde{A} = UDV^H$, $\Gamma_{ii} = \sigma_i/(\sigma_i^2 + \lambda^2)$, $\Phi_{ii} = \lambda^2/(\sigma_i^2 + \lambda^2)$, and σ_i denotes the i^{th} diagonal elements of D . For the “pre-computation” step, there are three techniques to reduce the computational burden. **1) QR Decomposition:** One major problem of singular value decomposition (SVD) is its computational cost. Therefore, we estimate singular values and vectors by two applications of QR decomposition rather than a single SVD factorization. Thus we consider the decomposition of \tilde{A} as $\tilde{A} = \tilde{U}\tilde{D}\tilde{R}^H = \tilde{U}\tilde{D}\tilde{V}^H$, where \tilde{U} , \tilde{D} , and \tilde{V} are approximated U , D , and V ; and R is a well-conditioned upper triangular matrix. Then **Eq 1** is modified to obtain $x^* = \tilde{V}\tilde{\Gamma}\tilde{U}^H \tilde{y} + \tilde{V}\tilde{\Phi}\tilde{U}^H x_0$ (**Eq 2**), where $L = I$, $\tilde{A} = \tilde{U}\tilde{D}\tilde{V}^H$, $\tilde{\Gamma}_{ii} = \hat{\sigma}_i/(\hat{\sigma}_i^2 + \lambda^2)$, $\tilde{\Phi}_{ii} = \lambda^2/(\hat{\sigma}_i^2 + \lambda^2)$, and $\hat{\sigma}_i$ denotes the i^{th} diagonal elements of \tilde{D} . This was accomplished by modifying the original framework in [3] to achieve computational cost reduction. **2) Fast Regularization Parameter Estimation Using A New L-curve:** From the traditional L-curve regularization parameter estimation method [5], we estimate the regularization parameter by finding the corner of the L-shape curve from $(\|x_\lambda - x_0\|_2^2, \|\tilde{A}x_\lambda - \tilde{y}\|_2^2)$, where $\|x_\lambda - x_0\|_2^2 = \sum_{i=1}^n \hat{f}_i^2 \left(\frac{\hat{u}_i^H \tilde{y}}{\hat{\sigma}_i} - x_0\right)^2$, $\|\tilde{A}x_\lambda - \tilde{y}\|_2^2 = \sum_{i=1}^n (1 - \hat{f}_i)^2 (\hat{u}_i^H \tilde{y})^2$, and $\hat{f}_i = \frac{\hat{\sigma}_i^2}{\hat{\sigma}_i^2 + \lambda^2}$. More efficiently, we use $(\lambda^2, \|x_\lambda - x_0\|_2^2)$ to form the L-curve and calculate its curvature [4]. Note, however, that we cannot precisely compute $\|x_\lambda - x_0\|_2^2$ during the pre-computation step and thus approximate $\hat{u}_i^H \tilde{y}$ as $\hat{\sigma}_i^{p+1}$, where p is a behavior-controlling real number [5]. **3) Sparse Matrix Representation:** The SMT (Sparse Matrix Transformation) has shown performance benefits in reconstruction [6]; however, the computational burden to sparsify the matrix during the pre-computation step is high. Here, we propose a Matrix Sparsifier (MS) which is an element-wise weighted sampling method based on the calculated probability of each element. It is computationally efficient and takes advantage of the structure of the regularized inverse of the block-diagonal matrix A . If we pre-compute $H \triangleq \tilde{V}\tilde{\Gamma}\tilde{U}^H$ and $h \triangleq \tilde{V}\tilde{\Phi}\tilde{U}^H x_0$ (described in **Eq 2**), the reconstruction step consists of a simple matrix-vector multiplication and vector summation: $x^* = H\tilde{y} + h$.

To further reduce the reconstruction computational complexity, we sparsify the dense matrix H to generate sparse matrix \tilde{H} , further simplifying computation of x^* .

RESULT: Using our proposed methods on 256x256 simulation data obtained from <http://www.nmr.mgh.harvard.edu/~fhlin> (3T MPRAGE images obtained with an 8-channel head coil array), the computational cost for the actual reconstruction is reduced by 71% when the reduction factor $R=3$ and by 98% when $R=4$ (see **Table 1**), with good image quality and visible reduction in amplified noise and residual aliasing artifacts (see **Fig 1**).

CONCLUSION: We have presented a sparse Tikhonov-regularized SENSE technique that accelerates image reconstruction through pre-computation and sparsification of the dense inverse matrix, and significantly reduces residual aliasing artifacts and noise amplification for ill-posed cases (e.g. when the reduction factor approaches the number of coils).

REFERENCE: [1] K. Pruessmann, et al., Magn Reson Med 1999; 42(5):952. [2] F.H. Lin, et al., Magn Reson Med 2004; 51(3):559. [3] T. Kitagawa, et al., BIT Num Math 2001; 41(5):1049. [4] M. Rezghu & S. Hosseini, et al., Compt and Appl Math 2009; 231(2):914. [5] P. Hansen, Compt Inv Prob in Electrocardiology 2001; Ch4:119. [6] J. Speciale, et al., Proc. Intl Soc Mag Reson Med 2011; 19:2871.

	S.T. Reg. (R=3)	S.T. Reg. (R=4)
RMSE	0.016531 (No Reg. = 0.019323)	0.019619 (No Reg. = 0.042852)
Computational Reduction (%)	71.1	98.3

Table 1. Error and computational reduction

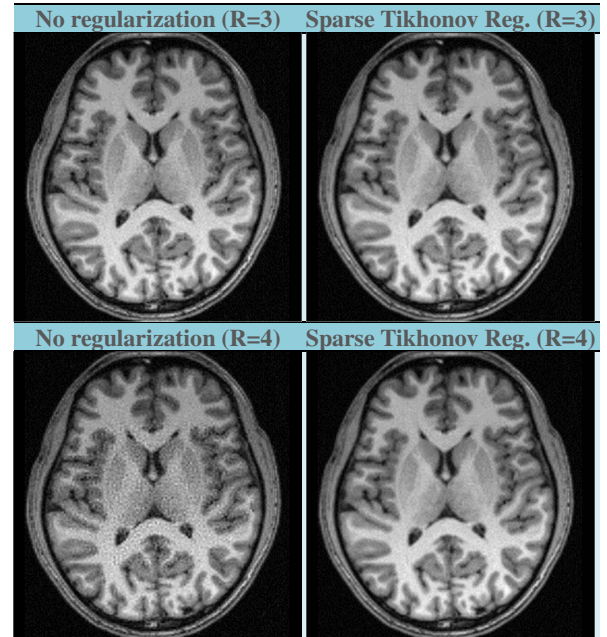


Fig 1. Reconstructed images