

# RESPIRATORY SELF-GATING FOR FREE-BREATHING QUANTITATIVE FAT/WATER IMAGING IN THE ABDOMEN

Tianjing Zhang<sup>1,2</sup>, Ning Jin<sup>1,3</sup>, Weiguo Li<sup>1,4</sup>, Xiaoming Yin<sup>1</sup>, and Andrew C. Larson<sup>1,2</sup>

<sup>1</sup>Radiology Department, Northwestern University, Chicago, Illinois, United States, <sup>2</sup>Biomedical Engineering Department, Northwestern University, Evanston, Illinois, United States, <sup>3</sup>Siemens Healthcare, Columbus, Ohio, United States, <sup>4</sup>University of Illinois at Chicago, Chicago, Illinois, United States

**Introduction:** For abdominal imaging applications, respiratory motion can lead to significant image quality deterioration and inaccurate measurements. While breath-holding (BH) is commonly employed to eliminate respiratory motion artifacts, overall slice coverage and spatial resolution are limited by the requisite BH duration. This work combines a free-breathing technology with a fat/water separation method. A revised multiple gradient echo sequence was implemented to acquire imaging data during free-breathing [1], followed by an off-line image reconstruction. A global optimization algorithm (VARPRO) was implemented for fat/water separation [2-6]. Conventional fat-water imaging methods and our free-breathing method were compared in 8 volunteers.

**Materials and method:** This work was carried out using a Siemens 1.5T MRI scanner (Espree). A revised multiple gradient echo sequence was implemented to acquire imaging data during free-breathing. The imaging parameters for this feasibility study were as follows: TR = 200-300ms, depending on individual respiratory rate; echo-train length=6; flip angle=25°; band-width=770Hz/pixel; matrix resolution =128×96pixels; slice thickness = 5mm; field of view=350×262.5; spatial resolution =2.7×2.7×5mm<sup>3</sup>; slice number = 1. TEs 2.5, 4.7, 6.9ms.

**Image processing:** An off-line image reconstruction algorithm [1] was implemented in Matlab (Mathworks, MA) for all images followed by a global optimization algorithm that imposed field map smoothness constraints for fat/water separation [7-8]. For comparison, conventional signal averaged images were generated by including all the sampled k-space data without consideration of the respiratory position. The fat-fraction (FF) value in each volunteer was calculated to quantitatively compare these for each of the three measurement approaches. For each volunteer, a region of interest (ROI) was drawn in the liver excluding blood vessels and mean FF measured within this ROI.

**Results:** Magnitude images and corresponding water maps for a representative volunteer are shown in Fig. 1 wherein RSG-BH stands for acquisition during breath-hold, RSG-FB images was acquired during FB with RSG and the RSG-AVG images included all data acquired during FB but with signal averaging rather than RSG. Magnitude images generated with RSG-AVG approach contained noticeable motion artifacts (ringing and/or blurring commonly observed). The RSG-FB method effectively mitigated motion artifacts, and provided qualitatively similar images as those generated with BH method.

Fig. 2 is a boxplot for the FF values calculated for each of the three methods. A Wilcoxon signed-rank test was performed with a significance level of 0.05 and a 95% confidence range to determine statistically significant differences between groups. The mean FF values within the liver measured using RSG-AVG were significantly lower than the values measured using RSG-BH (p = 0.036), while there was no significant difference between the mean FF measured using RSG-BH and RSG-FB (p = 0.4).

**Discussion and Conclusions:** In this work, we have qualitatively and quantitatively demonstrated the feasibility of applying the RSG-FB method for fat/water separation during abdominal imaging. The RSG-FB method successfully mitigated motion artifacts due to respiration and produced comparable fat-fraction values to BH approaches. In the future, these free-breathing fat/water separation methods may be valuable in clinical settings to avoid BH scan time limitations thus allowing superior spatial resolution, SNR, and imaging of sedated, non-compliant subjects.

**References:** 1.Ning J. et al, MRM, 66:207–212 (2011); 2.Huanyu Z. et al, MRM, 60:1122–1134 (2008); 3.Jingfei M., MRM, 52:415-419 (2004); 4. Clare P. Bernard et al, JMRI, 27:192–197 (2008); 5. D. Hernando et al, MRM, 59:571–580 (2008); 6. Katie H. Hansen et al, MRI, 30 (2012) 151–157; 7.Yin X et al, Radiology Jun; 263(3):714-22(2012); 8. Scott B. Reeder et al, MRM, 51:35–45 (2004);

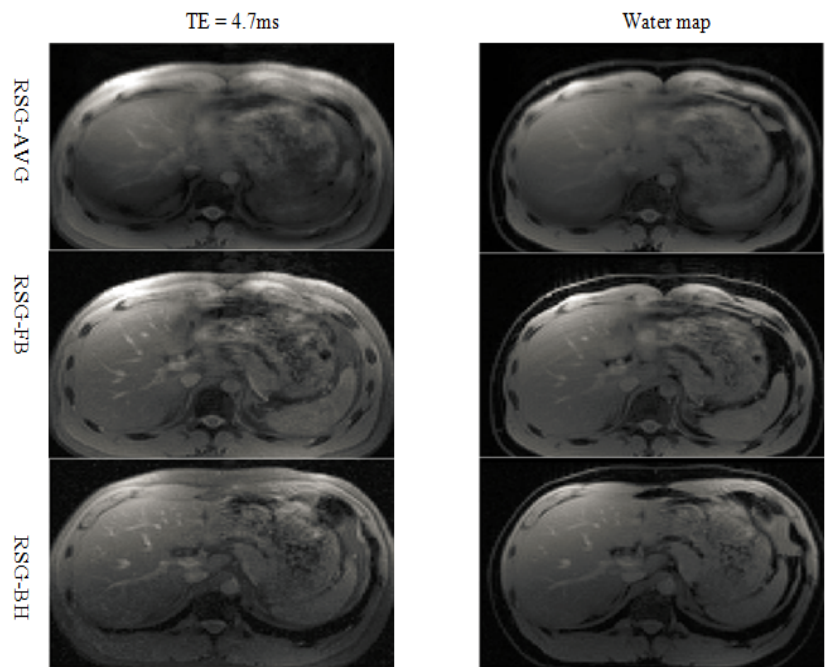


Figure 1 (a) (b) Magnitude and Water map images for three methods

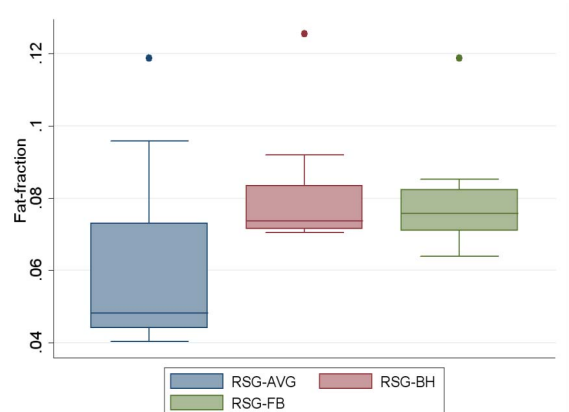


Figure 2 Liver Fat-Fraction Measurements from 8 Volunteers