

High Speed 3D Overhauser-Enhanced MRI using combined b-SSFP and Compressed Sensing

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Target Audience: Free radical imaging, hyper-polarization, MR method development and hardware

Purpose

Free radical imaging has been used to investigate physiological processes such as pO₂ mapping and to monitor the distribution and metabolism of free radicals in organs under oxidative stress. We present a new pulse sequence for rapid 3D imaging of free radicals using Overhauser-enhanced MRI (OMRI). In contrast to other OMRI methods that use a time consuming pre-polarization Overhauser irradiation step, the sequence presented here embeds the EPR pulses into the phase encode step of a balanced steady state free precession sequence (b-SSFP), greatly reducing the acquisition time. A further increase in temporal resolution is gained by undersampling of k-space and using compressed sensing reconstruction. This new OMRI sequence enables both improved spatial and temporal resolution of free radical distribution than other techniques.

Methods

Experiments were performed in a custom built, 6.5 mT, bi-planar electromagnet with bi-planar gradients. A 7 cm OD, 13 cm long Alderman-Grant coil was used to saturate the 140.8 MHz electron spin resonance of the nitroxide radical 4-hydroxy-TEMPO. The EPR coil was placed inside a 10 cm OD, 16 cm long solenoid coil for ¹H NMR excitation and detection. The EPR irradiation pulses were embedded into the phase encode and rewind steps of a fully balanced SSFP sequence as shown in Figure 1. 3D printed polycarbonate pieces 5.4 cm in diameter were used as a phantom (Figure 2a) with 2.5 mM TEMPO solution in water. Pieces were designed to evaluate the ability to resolve small feature in 3 dimensions. Image parameters were: matrix = 256x64x32, voxel size = 1x1x3.5mm, TR/TE = 54/27 ms, $\alpha = 90^\circ$, 70% undersampling rate, acquisition time = 65 s.

Results

Figure 2a) shows two segments of our phantom with the corresponding images in Figure 2b). The under-sampled data accurately reproduces the object, including the 1 mm diameter holes and 1 mm spacer. To confirm that this new sequence with imbedded EPR pulses is still a steady-state sequence, the sequence was run with only the read gradient while the echo amplitude was measured. After an initial buildup of polarization due to T₁, the signal reaches a steady-state amplitude that is ~ 30X larger than without embedded EPR pulses.

Conclusion

Embedding electron spin saturation into the phase encode step allows the use of a traditional b-SSFP sequence with no additional timings added. This is the first source of acceleration compared to traditional OMRI sequences that have a pre-polarization step of order T₁ before acquiring several lines of k-space. Further, for the phantom imaged here, only 30% of k-space is necessary to faithfully reproduce the image, reducing the acquisition time by a factor of 3. This technique will improve our ability to monitor physiological processes involving free radicals as the distribution of radicals can be tracked with greater spatial and temporal resolution.

Acknowledgement: Funded by DoD, Defense Medical Research and Development Program, Applied and Advanced Technology Development Award W81XWH-11-2-0076 (DM09094).

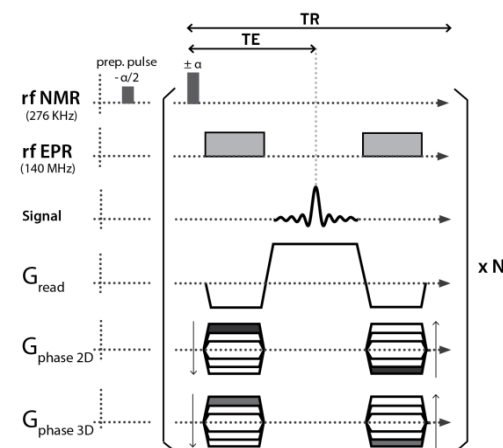


Figure 1. The 3D b-SSFP sequence with embedded EPR pulses.

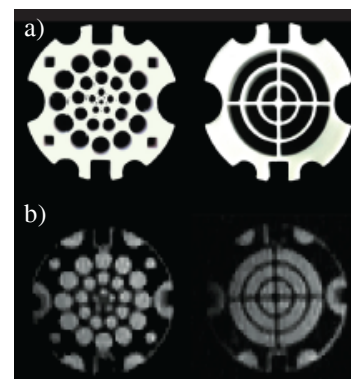


Figure 2. 2 slices from an OMRI image at 6.5 mT with 1x1x3.5 mm resolution over a 200 cm³ sample in 65 s. Phantom is 5.4 cm in diameter.