Robust estimation of pulse wave transit time using group delay

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<u>Introduction.</u> Aortic pulse wave velocity (PWV) is considered as the "gold standard" measurement of arterial stiffness and is commonly calculated as the ratio between the distance separating two locations along the artery and the transit time (Δt) needed for the pressure or velocity wave to cover this distance [1]. PWV is increasingly assessed by means of cardiovascular magnetic resonance (CMR) [2,3]. Our goal was evaluate the efficiency of a novel method for Δt estimation, based on the principle of group delay (TT-GD method) [4].

Materials and methods. 30 patients with hemoglobinopathies (25.2±9.8 years) were scanned using a 1.5T scanner (GE Signa CVi; GE Healthcare, Waukesha, WI) with a phased array torso coil. Phase contrast (PC) data were acquired using a retrospectively ECG-gated breathhold GRE sequence providing phase-related pairs of modulus and velocity-encoded images (100 phases). Images were analyzed with the FLOW image analysis software (Medis, Leiden, the Netherlands) to extract ascending and descending aorta flow and velocity curves. The Δt was calculated from blood flow curves using a custom-built software platform developed in Matlab (The Mathworks, Natick, MA). The TT-GD method operates in the frequency domain and models the ascending aortic waveform as an input passing through a discrete-component "filter", producing the observed descending aortic waveform, so that the GD of that filter represents the average time-delay. This method was compared with two previously described time-domain methods: TT-point using the half-maximum of the curves [2,5] and TT-wave using cross correlation [6]. To study the effect of the temporal resolution on ΔT estimates, the flow curves were downsampled of a factor of 2, 3 and 4.

Results. Mean Δts obtained with the three methods were comparable (TT-GD: 28.18 ± 5.36 ms, TT-point: 27.02 ± 5.32 ms, TT-wave: 26.93 ± 4.41 ; P=0.561).

The TT-GD method was the most reproducible (Table 1).

While the TT-GD as well as the TT-wave produced comparable results for velocity and flow waveforms (coefficient of variability or CoV: 4.81% and 5.04, respectively), the TT-point resulted in significant shorter Δt values when calculated from velocity waveforms (CoV=8.71%, mean difference: 1.78 ± 2.73 ms).

The TT-GD method was the most robust to reduced temporal resolution (Table 2).

Table 1.

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	TT- GD	TT- POINT	TT- FLOW	
Intra-operator reproducibility				
CoV (%)	3.38	5.66	3.40	
ICC	0.982	0.954	0.978	
BA bias (ms)	0.04	-0.42	0.10	
BA limits	-2.8 to	-4.7 to	-2.5 to	
(ms)	2.9	3.8	2.7	
Inter-operator reproducibility				
CoV (%)	3.67	8.17	5.04	
ICC	0.981	0.892	0.949	
BA bias (ms)	0.06	-0.41	0.15	
BA limits	-2.8 to	-6.6 to	-3.7 to	
(ms)	3.0	5.8	4.0	

Table 2.

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	Downsampling	Downsampling	Downsampling		
	by 2	by 3	by 4		
TT-GD					
Difference, mean ± SD (ms)	-0.08 ± 1.34	-0.10 ± 1.83	0.97 ± 2.52		
P (paired test)	0.746	0.756	0.074		
CoV (%)	3.33	4.52	6.57		
ICC	0.985	0.970	0.937		
Correlation, r (P-	0.970	0.941	0.893		
value)	(P<0.0001)	(P<0.0001)	(P<0.0001)		
BA limits (ms)	-2.7 to 2.6	-3.7 to 3.5	-4.0 to 5.9		
TT-POINT					
Difference, mean ± SD (ms)	-0.03 ± 4.63	-0.52 ± 5.28	1.74 ± 6.6		
P (paired test)	0.971	0.597	0.159		
CoV (%)	11.91	13.78	17.04		
ICC	0.798	0.794	0.559		
Correlation, r (P-	0.659	0.683	0.406		
value)	(P<0.0001)	(P<0.0001)	(P=0.026)		
BA limits (ms)	-9.1 to 9.0	-10.9 to 9.8	-11.2 to 14.7		
TT-FLOW					
Difference, mean ± SD (ms)	-0.61 ± 2.01	-0.13 ± 2.27	1.04 ± 2.66		
P (paired test)	0.108	0.757	0.040		
Correlation, r (P-	0.899	0.876	0.818		
value)	(P<0.0001)	(P<0.0001)	(P<0.0001)		
CoV (%)	5.49	5.89	7.24		
ICC	0.944	0.935	0.889		
BA limits (ms)	-4.6 to 3.3	-4.6 to 4.3	-4.2 to 6.2		

<u>Conclusion.</u> Compared to the traditional TT-point and TT-wave methods, the TT-GD approach was more reproducible and more robust to the waveform type and the choice of temporal resolution.

References.

[1] Laurent S et al. Eur Heart J 2006;27:2588-605. [2] Groenink M et al. Am J Cardiol 1998;82:203-8. [3] Vulliemoz S et al. Magn Reson Med 2002;47:649-54. [4] Papoulis A. Signal Analysis. McGraw-Hill;1977. [5] Kraft KA et al. Magn Reson Med 2001;46:95-102. [6] Ibrahim el SH et al. J Cardiovasc Magn Reson 2010;12:26.