

3D Dark Blood Cine Magnetic Resonance Imaging of the Carotid Arteries

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TARGET AUDIENCE: Vascular imagers of the carotid arteries.

PURPOSE: To propose and test a 3D dark-blood cine magnetic resonance imaging (MRI) pulse sequence capable of displaying the carotid arterial wall and its motion with fine temporal resolution and submillimeter spatial resolution over the cardiac cycle.

METHODS: This study was IRB approved. Imaging Sequence: A cardiac-gated 3D radial sequence was constructed to provide for a high spatial resolution static and cardiac-phase-resolved dynamic dark-blood imaging the carotid arterial wall (**Figure 1**). Radial views were sampled in a quasi-random order to support arbitrary temporal resolutions with minimal image undersampling artifact; sliding window reconstruction with the KWIC data weighting filter¹ was used generate a series of 20 temporal frames spanning the cardiac cycle. Temporal footprints (TF) of 10% to 40% of the total duration of the acquisition window were tested. Other imaging parameters were: non-selective RF excitation; cubic 22 cm field-of-view and 288 matrix; 0.8 mm isotropic spatial resolution; TR/TE/flip of 8.7 ms/4.2 ms/6°; 165 Hz/pixel bandwidth; ≈30,000 total projections; 50-88 projections acquired in each heartbeat (heart rate dependent); 393-464 s acquisition time, multiple motion sensitizing driven equilibrium (MSDE) preparations per heartbeat (1st order gradient moment of 982 mT·ms²/m); 9 fat saturation RF pulses per heartbeat.

Imaging Protocol: MRI was performed on a 32-channel 3T system (MAGNETOM Verio, Siemens) using a neck coil and a 4-channel carotid coil. The number of MSDE preparations applied in each heartbeat

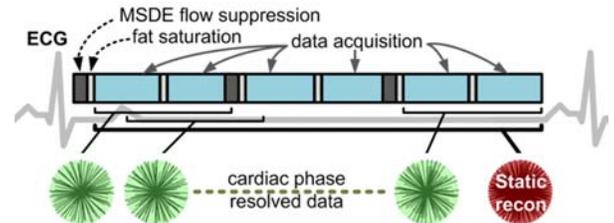


Figure 1. Timing diagram of the dark-blood 3D cine vessel wall imaging sequence. Subsets of radial views are grouped to generate the time-resolved 3D volumes; a static 3D volume is generated from all acquired views.

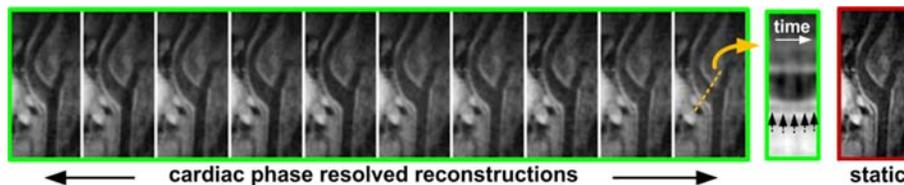


Figure 2. Select temporal frames (left) of the presented radial 3D dark blood cine method demonstrate the motion of the carotid wall throughout the cardiac cycle (arrowheads). The static reconstruction (right) derived from all projections displays the wall with improved spatial resolution.

RESULTS: The optimization study revealed that execution of 3 MSDE pulses each heartbeat minimized the coefficient of variation of signal within the carotid arterial lumen and provided near optimal contrast-to-noise ratio between the arterial wall and the lumen. Under this configuration, the method displayed the arterial wall and its pulsation over the cardiac cycle with submillimeter isotropic resolution (**Figure 2**). The image quality of the static reconstruction was comparable to that obtained with Cartesian 3D MERGE (**Figure 3**).

Arterial lumen areas obtained with the radial 3D dark-blood cine method agreed with values obtained using bright-blood 2D cine imaging (n=2060, Bland-Altman mean differences of 1.0% and 4.2% for TF of 10% and 40%, respectively). Arterial wall areas derived from the static reconstructions agreed with measurements obtained with Cartesian 3D MERGE MRI (n = 112; intraclass correlation coefficient of 0.946, P < 0.001; Bland-Altman mean difference of 0.96 mm²).

DISCUSSION: We demonstrated the feasibility of blood-suppressed 3D cine MRI of the carotid arteries. Because the presented method generates 3D static as well as cardiac phase-resolved data in a single acquisition, it has the potential to simultaneously quantify carotid stenosis, plaque volume, and characterize carotid plaque motion with fine spatial and temporal resolution. Given the association of all these indices with cerebrovascular risk³⁻⁶, future studies will seek to determine whether data provided by the proposed method can improve MRI-based assessment of cerebrovascular risk in patients with carotid atherosclerosis.

CONCLUSION: 3D dark-blood cine MRI of the carotid arteries with submillimeter isotropic spatial resolution and fine temporal resolution is feasible, and can provide a constellation of data for assessing cerebrovascular risk.

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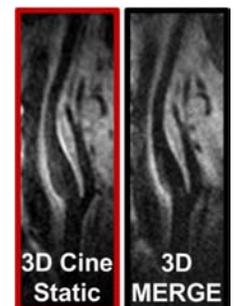


Figure 3. Static reconstruction of the proposed method (left) and the reference standard protocol (right) demonstrate similar image quality.