

# Phase sensitive PC-bSSFP: simultaneous quantification of $T_1$ , $T_2$ and spin density $M_0$

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**Introduction:** The fast and simultaneous quantification of MR parameters with a single sequence (IR-bSSFP [1]) has been proposed several years ago. The method is not suitable for 3D imaging due to long magnetization recovery interruptions. The used bSSFP-sequence is highly sensitive to off-resonance effects resulting in banding-artifacts and leading to over and underestimation of the parameters. Especially at higher fields, off-resonances cannot be avoided anymore. Here we propose a new approach for simultaneous quantification of  $M_0$ ,  $T_1$  and  $T_2$  based on phase-cycled bSSFP in 3D. The new proposed method yields its dynamics from the signals phase and offers intrinsic off-resonance compensation. This work presents the new theory and shows an experimental validation.

**Methods:** Experimental data-signal  $p$  from a phase-cycled bSSFP-sequence can pixel-wise fitted into a common ellipse equation:

$p = x_0 + iy_0 + (x \cdot \sin(\Phi) + iy \cdot \cos(\Phi)) \cdot e^{i\gamma}$ . Five data-points are required to determine an unambiguous fit. The common complex bSSFP steady-state equation can be recast into[3]:

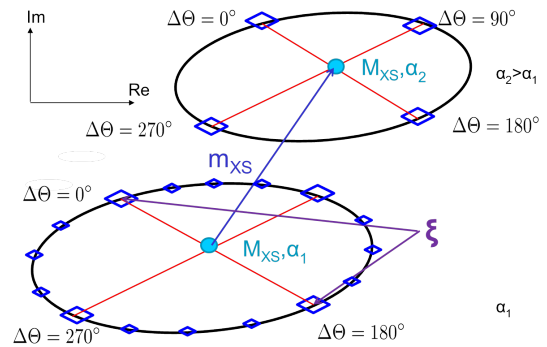
$$S_{bSSFP,\Theta} = M_{XS} \frac{1 - E_2 \cdot e^{i\Theta}}{1 - b \cdot \cos \Theta} \text{ with } \Theta = \Delta\Theta + \Delta\omega \cdot TR, b = b(T_1, T_2, TR, \alpha),$$

$M_{XS} = M_{XS}(M_0, T_1, T_2, TR, \alpha)$ ,  $\Delta\Theta$  as used phase-cycle. The shape of the function is similar to an ellipse equation and is a function of  $M_0$ ,  $T_1$ ,  $T_2$ , flip-angle  $\alpha$  and TR. The ellipse shape allows to interpolate to any arbitrary off-resonance  $\Delta\omega$  and hence to off-resonance free signals of measurements with  $\Theta = \{0^\circ, 180^\circ\}$  for every pixel.

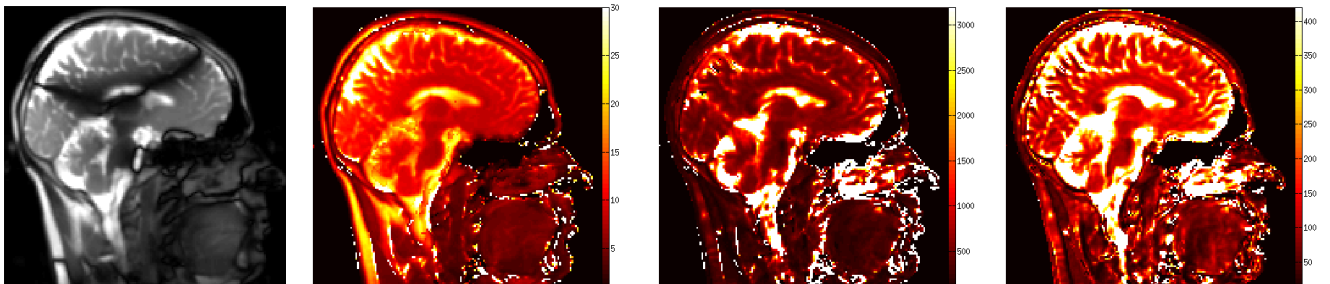
The ratio  $\xi = \xi(\alpha_1, T_1, T_2, TR) = S_{bSSFP,\Theta=180^\circ} / S_{bSSFP,\Theta=0^\circ}$  can be used as the first fit variable. The second fit variable is the slope  $m_{XS} = m_{XS}(\alpha, T_1, T_2, TR)$  of demodulated magnetization [2, 3]  $M_{XS}$  between two flip-angles analogous to [2, 5]. The demodulated magnetization can be calculated from four data-points with perpendicular phase-cycles applying the Cross-Solution(XS)[3]. Both variables  $\xi$  and  $m_{XS}$  only depend on  $T_1$ ,  $T_2$  as well as the parameters TR and  $\alpha_1$ . Therefore the parameters can be obtained by numerical fits. Spin density  $M_0$  can be calculated from the demodulated magnetization  $M_{XS}$  as well as  $\Delta\omega$  from signal equation.

**Experiments:** *In-vivo* measurements were performed on a healthy volunteer using a 1.5T clinical scanner. A bSSFP-sequence with non-selective super-balanced RF-pulses[4] was used. Two flip-angles of  $33^\circ$  and  $50^\circ$  were used as well as a TR-time of 8ms. 8 different phase-cycles were measured to overdetermine the ellipse. 4 more images were acquired for the second flip-angle. Total imaging time for a  $192 \times 192 \times 44$  matrix was approximately 14min. An exemplary raw data image is shown on the figure below.

**Results:** The data was analyzed using custom made MATLAB functions. The center slice was used for analysis. Other slices lead to similar results. As proposed the obtained  $M_0$ -,  $T_1$ - and  $T_2$ -maps do not suffer from banding-artifacts, see in the figure below. The obtained  $T_1$ - and  $T_2$ -times show good agreement for lower values.



**Fig. 1:** Two complex ellipses are shown. The lower one at flip-angle  $\alpha_1$  is fully sampled by 16 phase-cycles in opposite to the upper one at flip-angle  $\alpha_2$  whose Cross-Solution is used to determine the slope  $m_{XS}$ . The lower ellipse allows to determine the ratio  $\xi$ .



(a) raw data image with severe banding-artifacts (b)  $M_0$ -map(arb. units) of a human head (c)  $T_1$ -map(ms) of a human head (d)  $T_2$ -map(ms) of a human head

**Conclusion:** In this work we have shown that phase sensitive PC-bSSFP measurements can be used to obtain  $T_1$ ,  $T_2$ ,  $\Delta\omega$  and  $M_0$ . The method is a 3D and suitable for higher field strength. In contrast to DESPOT2[5], all measurements can be done simultaneous with one imaging sequence, no  $T_1$ -information is required a prior. A thorough analysis about accuracy and robustness as well as optimal flip-angles is subject of current research. Parallel imaging methods may be applied for speed up.

**References:** [1] Schmitt et al., 2004 MRM, 51:661–667 [2] M.Ott et al., 2011 ESMRMB [3] Q-S. Xiang and M.N. Hoff 2010 ISMRM [4] O. Bieri, 2011 MRM, in press [5] S. Deoni et al, 2003, MRM 49, 515-526

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