

Including a Third, Non-Exchanging Water Component in mcDESPOT

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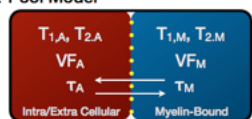
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INTRODUCTION: Assessment of myelin content through multi-component analysis of relaxation data (MCR) provides salient information in de-myelinating disease (such as multiple sclerosis), as well as neurological disorders arising from altered brain connectivity. T₂-based MCR analysis [1] consistently reveals at least 2 water compartments in brain parenchyma, attributed to water between the myelin bilayers; and intra/extra-axonal (IE) water [2]. A third pool, bulk free water (e.g., cerebral spinal fluid, CSF) may also be present [2]. Multi-component Driven Equilibrium Single Pulse Observation of T₁ & T₂ (mcDESPOT) [3] is an alternative MRC method that, unfortunately, assumes only two water pools. While informative, this model may fail in partial volume voxels, leading to a biased MWF estimate. Inclusion of a third, non-exchanging component to the mcDESPOT model may correct for these effects. (Fig. 1). Here we outline the mathematical framework and investigate results from a healthy adult and an elderly patient with Alzheimer's Disease (AD).

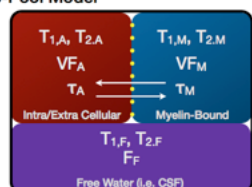
METHODS: The three-component SPGR and bSSFP magnetizations are given by:

$M_{SPGR}^{SS} = M_{SPGR} (I - e^{A_{SPGR} \times TR}) \sin \alpha \times (I - e^{A_{SPGR} \times TR} \cos \alpha)^{-1}$ and $M_{bSSFP}^{SS} = (e^{A_{bSSFP} \times TR} - I) A_{bSSFP}^{-1} C \times [I - e^{A_{bSSFP} \times TR} R(\alpha)]^{-1}$, where I is the 3x3 or 9x9 identity matrix, M_{SPGR} , M_{bSSFP} , A_{SPGR} , A_{bSSFP} , C and $R(\alpha)$ are 3x3 (SPGR) or 9x9 (bSSFP) matrices containing the relative volume fraction, relaxation, off-resonance, exchange rate, and excitation flip angle (α) terms.

2-Pool Model



3-Pool Model



$$A_{SPGR} = \begin{bmatrix} -\frac{1}{T_{1,M}} - k_{M \rightarrow IE} & k_{IE \rightarrow M} & 0 \\ k_{M \rightarrow IE} & -\frac{1}{T_{1,IE}} - k_{IE \rightarrow M} & 0 \\ 0 & 0 & -\frac{1}{T_{1,F}} \end{bmatrix}$$

$$C = \rho \begin{bmatrix} 0 & 0 & 0 & 0 & 0 & 0 & \frac{M_F}{T_{1,M}} & \frac{IE_F}{T_{1,IE}} & \frac{F_F}{T_{1,F}} \end{bmatrix}^T$$

$$A_{bSSFP} = \begin{bmatrix} -\frac{1}{T_{1,M}} - k_{M \rightarrow IE} & k_{IE \rightarrow M} & 0 & \Delta\omega & 0 & 0 & 0 & 0 & 0 \\ k_{M \rightarrow IE} & -\frac{1}{T_{1,IE}} - k_{IE \rightarrow M} & 0 & 0 & \Delta\omega & 0 & 0 & 0 & 0 \\ 0 & 0 & -\frac{1}{T_{1,F}} & 0 & 0 & \Delta\omega & 0 & 0 & 0 \\ -\Delta\omega & 0 & 0 & -\frac{1}{T_{1,M}} - k_{M \rightarrow IE} & k_{IE \rightarrow M} & 0 & 0 & 0 & 0 \\ -\Delta\omega & 0 & 0 & k_{M \rightarrow IE} & -\frac{1}{T_{1,IE}} - k_{IE \rightarrow M} & 0 & 0 & 0 & 0 \\ -\Delta\omega & 0 & 0 & 0 & 0 & -\frac{1}{T_{1,F}} & 0 & 0 & 0 \\ 0 & 0 & 0 & 0 & 0 & 0 & -\frac{1}{T_{1,M}} - k_{M \rightarrow IE} & k_{IE \rightarrow M} & 0 \\ 0 & 0 & 0 & 0 & 0 & 0 & k_{M \rightarrow IE} & -\frac{1}{T_{1,IE}} - k_{IE \rightarrow M} & 0 \\ 0 & 0 & 0 & 0 & 0 & 0 & 0 & 0 & -\frac{1}{T_{1,F}} \end{bmatrix}$$

Figure 1: Illustrations of the 2 and 3-pool models

Fitting of this model is performed via the stochastic region contraction approach outlined previously [4].

To demonstrate the method, *in vivo* sagittal adult data were acquired as: 22cm²x17cm FOV; 128x128x98 matrix. SPGR: TE/TR=2.4ms/5.4ms; α =(3, 4, 5, 6, 7, 9, 13 and 18)°; BW = 380 Hz/voxel bSSFP: TE/TR=2.2ms/4.4ms; α =(10, 13, 17, 20, 23, 30, 43 and 60)°. BW=560 Hz/voxel. A reduced resolution IR-SPGR image was

AD Patient

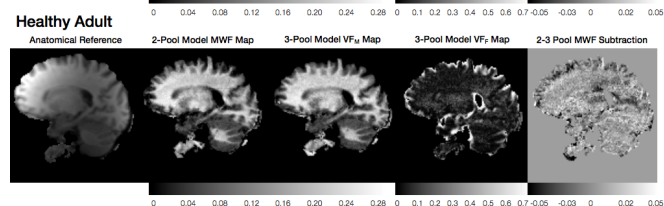
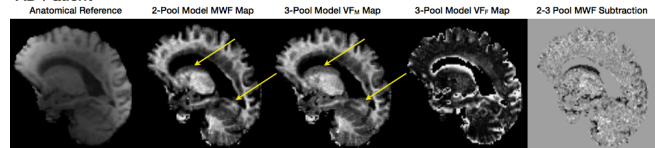


Figure 2: *In vivo* results from a healthy adult and an elderly patient with Alzheimer's Disease (AD). Significant CSF volume fraction is apparent surrounding the ventricles and the periphery of the brain.

white matter. These results suggest the original 2-pool mcDESPOT implementation may be insufficient in specific brain regions or pathologically altered tissue, yielding a biased and under-estimated MWF value. Qualitatively, the 3-pool approach appears to correct for these issues, and may be a more suitable choice for investigations of disease.

REFERENCES: [1] Kroeker RM, Henkelman RM. J. Magn. Reson. 1986; 69: 218-235. [2] Whittal KP, et al. Magn. Reson. Med. 1997; 37: 34-43. [3] Deoni SCL, et al. Magn. Reson. Med. 2008; 60: 1372-1387. [4] Deoni SCL. Magn. Reson. Med. 2011; 65: 1021-1035.