## Dynamic Radial Imaging of Inhaled <sup>129</sup>Xe and <sup>3</sup>He

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**Introduction:** <sup>129</sup>Xe ventilation and diffusion lung imaging [1, 2] show the clinical potential to replace <sup>3</sup>He as a cheaper, more accessible alternative. Dynamic radial <sup>3</sup>He imaging [3] has been shown to capture the dynamics of gas ventilation and can give information about lung motion and gas trapping [4]. In this study, <sup>129</sup>Xe and <sup>3</sup>He dynamic radial imaging of an inhalation and exhalation manoeuvre were compared in a healthy volunteer.

**Methods:** A healthy volunteer was scanned using a 3T whole body MRI system (Philips Intera, Best, Netherlands). A 2D time resolved radial sequence was used to image an inhalation and exhalation of gas over 20 seconds for both  $^{129}$ Xe and  $^{3}$ He gases. A coronal full lung projection was acquired with TR=14ms, FOV=384mm, matrix=96 and  $\theta$ =5°. Consecutive radial k-space lines were rotated by the golden angle (111.246°) to allow flexible spatial-temporal reconstruction of the data [5] with sliding window reconstruction.

 $^{129}$ Xe imaging:  $^{129}$ Xe was polarised to  $^{\sim}$ 14% [6] with a home-built regulatory-approved spin exchange polariser [7]. The volunteer was positioned in a  $^{129}$ Xe transmit-receive vest coil (CMRS) and inhaled 400ml of xenon mixed with 600ml of N<sub>2</sub>. A receive bandwidth of 8kHz and a TE of 7ms were used.

 $^{3}$ He imaging:  $^{3}$ He was polarised to  $^{2}$ 5% with a Helispin polariser (GE). The volunteer was positioned in a  $^{3}$ He transmit-receive birdcage coil (Rapid Biomedical) and inhaled 250ml of hyperpolarised  $^{3}$ He mixed with 750ml of N<sub>2</sub>. Due to the higher diffusivity of  $^{3}$ He, a receive bandwidth of 48kHz was used to limit signal loss from diffusion during the readout (TE=1.7ms).

**Results and Discussion:** Dynamic radial images of <sup>129</sup>Xe and <sup>3</sup>He from the same healthy volunteer are shown in figure 1. Comparable lung movement and gas filling is seen in both sets of images. Despite the lower SNR of the <sup>129</sup>Xe images they still convey the necessary information, and even show a small ventilation defect in the volunteer's mid-right lung which becomes apparent in the last two frames of exhalation.

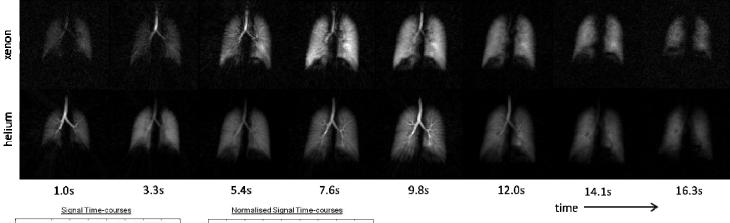


Figure 1 129Xe (top) and 3He (bottom) dynamic radial images from the same healthy volunteer

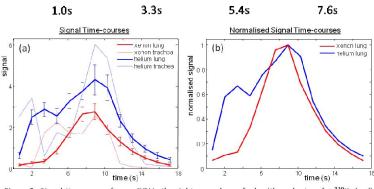


Figure 2 shows the  $^{129}$ Xe and  $^{3}$ He signal behaviour as a function of time for a region of interest in the right upper lobe. (a) shows mean signal  $\pm$  standard deviation and (b) shows signal normalised to the peak signal. The rate of signal increase at the beginning of the inhalation was greater for  $^{3}$ He than for  $^{129}$ Xe. This may be due to the fact that  $^{129}$ Xe is denser which will affect flow dynamics and requires more inspiratory effort to inhale through the 5mm tubing of the Tedlar bag. The rate of exhalation was similar for both gases.

**Figure 2** Signal-time curves from a ROI in the right-upper lung of a healthy volunteer for  $^{129}$ Xe (red) and  $^3$ He (blue). Trachea ROIs are shown with dotted lines.

**Conclusions:** <sup>129</sup>Xe provides useful information about lung motion and filling similar to that provided by <sup>3</sup>He in dynamic radial imaging. Future studies will focus on the regional kinetics and gravitational flow effects of these two gases of different densities.

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References: [1] Mugler et al, MRM 37:809-815 (1997); [2] Dregley et al, JMRI 33:1052-1062 (2011); [3] Wild et al, MRM 49:991-997 (2003); [4] Holmes et al, JMRI 26:630-36 (2007); [5] Winkelmann et al, IEEE Trans Med Imaging 26:68-76 (2007); [6] Norquay et al, proc. British Chapter ISMRM, Manchester 2011; [7] Parnell et al, J Appl Phys 108:064908 (2010);