

Clinical application to bone health assessment of a new MR-based technique enabling quantitative measurement of trabecular bone structure

Juliet Compston¹, Amanda Cox², Michael Stone³, Jane Turton³, Irene Debirim¹, and Kristin James²

¹School of Clinical Medicine, University of Cambridge, Cambridge, United Kingdom, ²Acuitas Medical, Swansea, United Kingdom, ³Llandough Hospital, Cardiff, United Kingdom

Introduction: Osteoporosis is becoming more prevalent—the number of hip fractures is expected to double in the next 50 years due to the aging population [1], and currently costs the NHS around £2 billion a year, a figure which is expected to triple by 2036 [2]. There is high morbidity associated with hip fracture—20% of those individuals sustaining hip fracture will die within 6 months and, of those that survive, only 1 in 3 will ever regain their previous level of mobility and independence [3]. Trabecular bone structure is known to change during osteoporosis, leading to increased risk of fragility fracture [1], but these structural changes are not currently used in diagnosis. DXA, the current gold standard of osteoporosis diagnosis, is not capable of evaluating changes in trabecular architecture [4] though it is thought that trabecular measurement would allow better assessment of fracture risk [5]. A new magnetic resonance-based technique, designed to measure biologic texture too fine to be resolved by conventional MR imaging, was evaluated for its ability to assess bone health through quantification of trabecular bone structure. The technique provides a measure of the characteristic distance between trabecular elements by signal analysis of a finely sampled one-dimensional, spatially encoded echo from a selectively excited internal volume. This analysis yields a spectrum of structural wavelengths present within the selected volume of bone or tissue. A clinical study applying the technique in the L1 vertebrae of 20 postmenopausal women was undertaken, testing its ability to distinguish patients with normal bone structure from those with abnormal. The vertebral body exhibits a larger percentage change in trabecular web structure with onset of osteoporosis, compared to other skeletal sites [6].

Methods: Twenty female postmenopausal women, mean age 64.4 years, who had not been treated with oral bisphosphonates for any longer than 6 months, were recruited for this study. Due to the difficulty in recruiting women with fracture who had not exceeded the time limit on bisphosphonates, the cohort comprised three groups, normal patients (n=6), osteopenic or osteoporotic patients with no fragility fracture (n=6), and osteopenic or osteoporotic patients with fragility fracture (n=8). These were assigned to groups by bone mineral density (BMD) T-score obtained at the lumbar spine and hip, and by fracture history. MR intensity data were acquired along the long axis of a prismatic volume 10mm x 10mm by 70mm, aligned in the LR direction across the L1 vertebral body, via the application of an in-house-developed pulse sequence. The resultant signal intensity profile was then analysed to yield a spectrum of structural wavelengths present along the sampled volume.

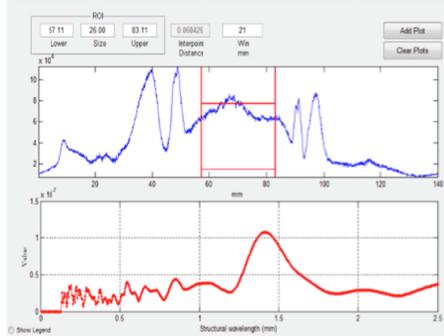


Figure 1. The region along the MR signal intensity profile used for analysis is indicated by the red goal posts overlaid on the MR signal intensity profile (top); bottom is the spectrum of textural wavelengths in mm obtained by fine structure analysis of the selected region.

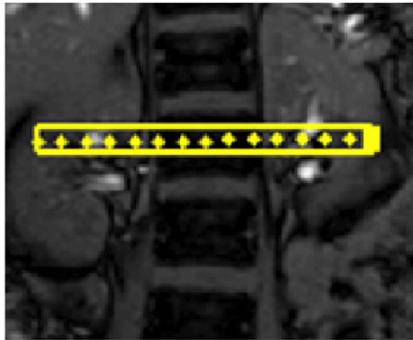


Figure 2. Overlay of prismatic volume along which complex MR echo intensity is measured on reference image of the L1 vertebra.

normal BMD (see figure 3). Biomarkers were developed to draw on these visual differences to provide a quantitative measure of bone health. Four of the developed biomarkers could significantly ($p<0.03$) separate women with normal BMD from those who were osteopenic or osteoporotic. These biomarkers were: 1) position of the highest intensity peak when the spectrum was truncated at 1mm, 2) position of the highest intensity peak when the spectrum was truncated at 2.5mm, 3) difference in intensity of the two highest intensity peaks in the wavelength spectrum, and 4) the average difference in intensity of the two dominant peaks in a set of spectra. All of these showed significant ($p<0.02$) correlation to both T-score and BMD in g/cm^2 but no significant correlation was found with patient age ($p>0.1$) for any biomarker. The biomarkers, when applied to wavelength spectra generated using our fine structure analysis technique, could classify patients with normal or osteopenic/osteoporotic BMD with success rates between 75% and 85%.

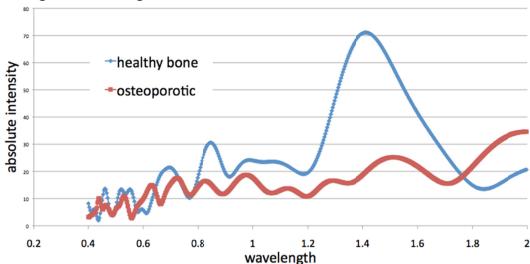


Figure 3. Spectra of fine structural textures generated for healthy (blue) and for osteoporotic bone (red).

fractures in postmenopausal women, partially independent of decreased BMD measured by DXA: The OFELY study. Journal of bone and mineral research, 2007. 22(3): p. 425-433.

5. Keaveny, T. and O. Yeh, Architecture and trabecular bone - Toward an improved understanding of the biomechanical effects of age, sex and osteoporosis. Journal of musculoskeletal neuron interaction, 2002. 2(3): p. 205-208.

6. Merck & Co., Inc. Pathophysiology of bone. 2004; Available from: <http://www.merckmedicus.com/pp/us/hcp/diseasemodules/osteoporosis/pathophysiology.jsp>

7. Welch, PD, The Use of Fast Fourier Transform for the Estimation of Power Spectra: A Method Based on Time Averaging Over Short, Modified Periodograms. IEEE Transactions on Audio Electroacoustics, 1967, AU-15: p. 70-73.