

In Vivo ^{17}O Measurements of Water Rotational Correlation Time and Hydrodynamic Radius in Rat Brain

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Introduction

Water content is extremely high in a biological system. It plays essential roles in maintaining normal cellular functionalities, and is sensitive to the microscopic environment of intra- and extra-cellular spaces. This study exploits new MR approaches for noninvasively assessing the rotational correlation time (τ_c) and hydrodynamic radius (R_h) of the brain tissue water. *In vivo* ^{17}O MRS was used to measure the longitudinal relaxation time (T_1) of the quadrupolar ^{17}O spin of water, and the T_1 value can be used to calculate water τ_c according to a simple, field-independent relation. ^1H MRI was applied to image the brain translational diffusion coefficient (D_i), and the D_i/T_1 ratio can be used to determine R_h . These approaches were tested and evaluated at 9.4T using the rat brain model with varied brain temperature.

Theory

^{17}O spin has a quantum number of $I = 5/2$ and possesses an electric quadrupolar moment that can interact with local electric field gradients. The temporal fluctuation in this interaction induced by molecular motion dominates the ^{17}O relaxation process. For the water molecule with the extreme narrowing limit (i.e., $\tau_c\omega \ll 1$, ω is the ^{17}O Larmor frequency), there is a simple relation between water T_1 (unit: ms) and τ_c (unit: picosecond) according to Eqs. [1] and [2]:

$$\frac{1}{T_1} = \frac{3\pi^2}{10} \left(\frac{2I+3}{I^2(2I-1)} \right) \left(1 + \frac{\eta^2}{3} \right) \left(\frac{e^2Qq}{h} \right)^2 \tau_c \quad [1]; \quad \tau_c = \frac{13.8}{T_1} \text{ (ps)} \quad [2]; \quad \tau_c D_i = 2R_h^2/9 \quad [3]; \quad R_h = 78.8 \sqrt{D_i/T_1} \quad [4],$$

where e^2Qq/h (≈ 8.1 MHz) is the ^{17}O quadrupolar coupling constant, η is an asymmetry parameter and they are constant and field independent^{1,2}.

The relation between the translational diffusion coefficient (D_i : mm^2s^{-1} unit), τ_c and R_h (unit: Å) can be derived using the Stokes-Einstein and the Debye-Stokes-Einstein equations³, leading to Eq. [3] indicating that $\tau_c D_i$ should be a constant. Solving Eqs. [2] and [3] gives Eq. [4], in which D_i can be imaged using conventional DTI with two b factors, thus, R_h can be calculated according to Eq. [4].

Methods

All NMR experiments were conducted using Male Sprague-Dawley rats on a 9.4 T animal magnet interfaced to a Varian INOVA console. A dual surface-coil probe consisting of a butterfly-shape ^1H coil (400 MHz) and an oval-shape ^{17}O coil ($\sim 1\text{cm} \times 2\text{cm}$, 54.25 MHz) was used for acquiring ^1H and ^{17}O data, respectively. Non-localized ^{17}O MR spectroscopy with inversion recovery pulse sequences and 8 inversion recovery times were applied for measuring T_1 values of natural abundance H_2^{17}O in the rat brains (6 animals) with varied body temperature (T : 27-37°C, or 300-310 K). ^1H MR images were acquired using adiabatic spin-echo sequence with two b-values (0 and 668 s/mm^2) to measure D_i in the ROI covering a large brain region and its temperature dependence (2 animals).

Results

Figure 1A shows the relation between the ^{17}O T_1 of brain tissue water and the inverse of temperature ($1/T$) from different rat measurements. It indicates that the increasing temperature resulted in a longer T_1 . The relation obeys a linear function ($R^2=0.983$). Figure 1B shows the relation between the rotational correlation time, τ_c , and the inverse of temperature ($1/T$), indicating a reversed linear relation ($R^2=0.976$), i.e., the increasing temperature shortened τ_c . Figure 2 displays the results of R_h measurements across the temperature range of 27-37°C., indicating an independent relation of R_h on temperature. Both rats had a similar trend though one animal (Rat A) showed a slightly higher R_h value compared to the other. The average R_h from two animals was $1.00 \pm 0.01 \text{ Å}$.

Discussion and Conclusion

In this study, we tested novel MR-based approaches for *in vivo* measurements of two important parameters of rotational correlation time and hydrodynamic radius that reflect the brain tissue water dynamics at the molecular scale. It was found that the brain water τ_c was in a range of several picoseconds and is sensitive to the brain temperature change; the measured τ_c values were longer than the bulk water τ_c . For instance, based on the linear relation shown in Fig. 1B, we predicted the tissue water τ_c value of 3.5 ps at 25°C in the rat brain, which was significantly longer than that of bulk water (≈ 2.7 ps) at the same temperature¹. This result reveals that τ_c is sensitive to microscopic environment in the biological system as one would expect. The measured R_h values were stable across a large range of brain temperature (see Fig. 2). This result provides convincing evidence in supporting the validity of Eq. [3] and the methods proposed herein for *in vivo* measurements of brain water τ_c and R_h . The measured R_h value of $\sim 1 \text{ Å}$ was in line with the size of water molecular radius ($\sim 1.3 \text{ Å}$). This work indicates excellent utilities of *in vivo* ^{17}O MRS methods for potentially imaging the microscopic dynamics and cellular environment of brain tissue water *in vivo*.

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References [1] Glasel (1966) *Proc Natl Acad Sci U S A* 55:479-85; [2] Zhu & Chen (2011) *Prog Nucl Magn Reson Spectrosc* 59:319-35; [3] Yao et al. (2008) *Biophys Chem* 136:145-51.

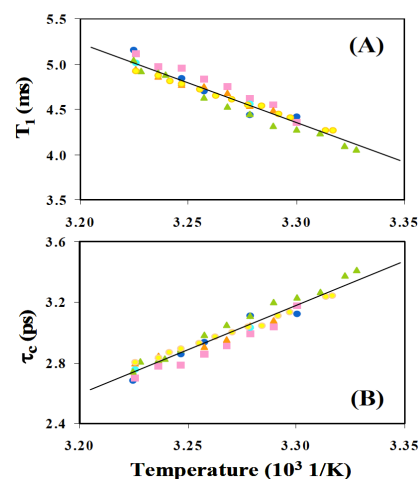


Fig. 1 Temperature dependence on (A) ^{17}O T_1 and (B) rotational correlation time τ_c of rat brain tissue water. The colors present the data from different rats and solid lines present the linear regression for all data.

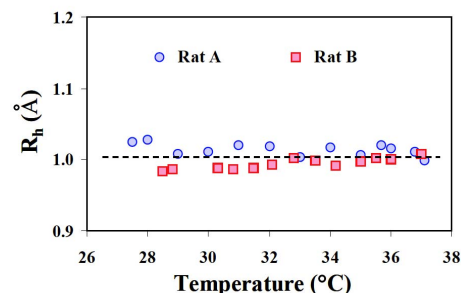


Fig. 2 Temperature independence of water hydrodynamic radius (R_h) measured in two rat brains. The solid line presents the average of R_h measurements.