

# Model Free Approach to Kinetic Analysis of Real-Time Hyperpolarised $^{13}\text{C}$ MRS Data

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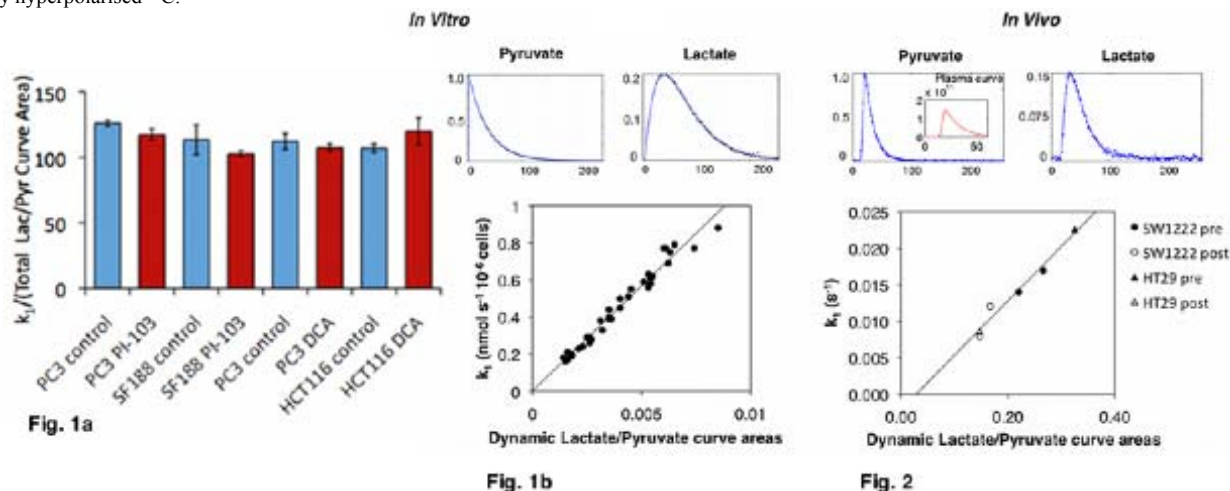
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**Introduction:** Dynamic Nuclear Polarisation (DNP) is revolutionising the use of  $^{13}\text{C}$  MRS, allowing real-time metabolic imaging both *in vitro* and *in vivo*<sup>1</sup>. A major application of hyperpolarised  $^{13}\text{C}$  MRS is to determine the apparent reaction rate constants governing pyruvate-lactate exchange (forward rate constant  $k_1$ ), which reflects lactate dehydrogenase activity, a key metabolic enzyme that is commonly upregulated in cancer cells. Therapy-induced changes in  $k_1$  have been suggested as an early biomarker of treatment response in cancer<sup>2</sup>. These apparent reaction rate constants are typically determined by kinetic modelling of the dynamic data using the modified Bloch equations<sup>2</sup>, a method that requires expertise in computer modelling and knowledge of the reaction mechanism. Seth et al.<sup>3</sup> use a model-free approach by reporting the ratios of maximum lactate/pyruvate signals to detect response to treatment *in vivo*. Here, we propose a potentially more robust model-free analysis method in which the ratio of the total integrated areas under the dynamic lactate to pyruvate curves is calculated. The utilisation of the entire data set should generate a metric with less associated error than using maximum recorded signal alone. In this study we compare  $k_1$ , calculated using an in-house kinetic model, to the ratio of the total areas under the lactate/pyruvate dynamic curves across a wide variety of cancer cell types (PC3, HCT116, SF188) and also in response to drug treatments (PI3K/mTOR inhibitor PI-103 and PDK inhibitor dichloroacetate (DCA)) *in vitro*. This comparison of analysis methods has also been applied to *in vivo* data sets of mice bearing subcutaneous HT29 or SW1222 colon cancer xenografts treated with DCA.

**Methods:** MRS was performed at 37°C on a Bruker 500MHz (*in vitro*) or Bruker 300MHz (*in vivo*) spectrometer. **Hyperpolarised  $^{13}\text{C}$ :** 18mg/26mg (*in vitro/in vivo*) [ $1\text{-}^{13}\text{C}$ ] pyruvic acid (99% isotopically enriched containing 15mM trityl free radical OX63) was polarised in a HyperSense® DNP polariser for 1h. The polarised sample was dissolved in 4ml aqueous buffer (*in vitro*: 50mM sodium lactate, 50mM NaOH, 1mM EDTA; *in vivo*: Trizma buffer containing 80mM NaOH, 1mM EDTA) resulting in a 50mM/80mM (*in vitro/in vivo*) pyruvate solution at pH 7, 37°C. *In vitro*, 100µl of this solution was mixed with a 500µl cell suspension, during which  $^{13}\text{C}$  spectra were acquired every 2s using a single scan and a 10° flip angle. *In vivo*, 150µl 80mM hyperpolarised [ $1\text{-}^{13}\text{C}$ ] pyruvate was administered *in situ* via a lateral tail vein over approximately 5s and a series of  $^{13}\text{C}$  spectra were recorded at 75MHz every 2s using a 20° slice selective pulse-and-acquire sequence (1 transient, 32k time domain points, 15kHz spectral width). ***In vivo* tumour implantation and DCA treatment:** Human HT29 adenocarcinoma or SW1222 colorectal carcinoma cells ( $5 \times 10^6$ ) were propagated subcutaneously in NCr nude mice. Tumours were scanned (day one), then mice were treated on days two and three with 200mg/kg DCA p.o. and a final dose was given on day four, one hour before the post-treatment scan. **Data analysis:** Spectra were phase and baseline corrected, and peaks of interest selected and integrated over the time course of the experiment. **Kinetic modelling:** The integrals of the hyperpolarised [ $1\text{-}^{13}\text{C}$ ] resonances of pyruvate and lactate were fitted to the modified Bloch Equations for two-site exchange<sup>2</sup> and normalised to pyruvate signal intensity at time  $t=0$ . Kinetic modelling was performed using Matlab. **Dynamic Curve Area:** The time courses of integrals from each hyperpolarised metabolite signal were summed and the ratios of the lactate/pyruvate curves were calculated.

**Results and Discussion:** Fig. 1 shows that there is no significant difference between the ratio of  $k_1$  vs dynamic lactate/pyruvate curve areas *in vitro*, indicating that the methods measure equivalent changes upon drug treatment and are therefore of comparable sensitivity. Figures 1b and 2 show the dynamic profiles of MRS signals derived from the injection of hyperpolarised [ $1\text{-}^{13}\text{C}$ ] pyruvate *in vitro* and *in vivo*, with kinetic model fits overlaid;  $k_1$  is determined from the kinetic model and can be compared to the relative areas under these dynamic curves. Figures 1b and 2 show that changes in the ratio of lactate/pyruvate dynamic peak area is proportional to the changes in forward apparent rate constant,  $k_1$ . The Pearson correlation coefficient ( $r$ ) for *in vitro* data is  $r = 0.97$  and  $P < 0.0001$  and for *in vivo* data  $r = 0.993$  and  $P < 0.0001$ , showing that in both cases the correlation between data sets is highly significant.

**Conclusions:** We have shown that a model-free approach of measuring the ratio of the lactate/pyruvate dynamic curve areas can detect therapy-induced changes across different cancer cell lines and drug treatments both *in vitro* and *in vivo*, with equivalent sensitivity to changes in  $k_1$  determined by kinetic modelling. This model-free approach is found to be proportional to the measured kinetics, with highly significant Pearson correlation coefficient ( $r = 0.97$ ,  $P < 0.0001$  *in vitro* and  $r = 0.993$ ,  $P < 0.0001$  *in vivo*), offers a simple alternative for the analysis of hyperpolarised metabolic data, and will prove useful for assessing drug induced metabolic changes measured by hyperpolarised  $^{13}\text{C}$ .



**Figure 1. *In vitro*:** a. The ratio of  $k_1$  vs. lactate/pyruvate dynamic peak area is consistent between cell types ( $n=3$  per group) and upon various drug treatments *in vitro*; the model-free approach and kinetic model display equivalent sensitivity to treatment effects. b. **Top:** Peak integrals (dots) and kinetic modelling (line) of *in vitro* dynamic  $^{13}\text{C}$  spectra from pyruvate and lactate. **Bottom:** Apparent rate constant of pyruvate-lactate exchange ( $k_1$ ) plotted against the ratio of total dynamic curve areas of lactate/pyruvate for *in vitro* studies shows the methods detected comparable response across all the cell lines; Pearson correlation coefficient is  $r=0.97$  and  $P<0.0001$ .

**Figure 2. *In vivo*:** **Top:** Peak integrals (dots) and kinetic modelling (line) of *in vivo* dynamic  $^{13}\text{C}$  spectra from pyruvate and lactate. **Bottom:** Apparent rate constant of pyruvate-lactate exchange ( $k_1$ ) plotted against the ratio of total dynamic curve areas of lactate/pyruvate for *in vivo* studies. HT29 or SW1222 cancer xenografts are indicated, and pre and post DCA treatment data points are distinguished. The Pearson correlation coefficient is  $r=0.99$  and  $P<0.0001$ .

**References.** (1) Ardenkjaer-Larsen, J.H., et al. *Proc Natl Acad Sci* (2003) (2) Day, S.E., et al. *Nat Med* (2007) (3) Seth, P., et al. *Neoplasia* (2011)

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