

Determination of the pK_a of a Hyperpolarized H¹³CO₃⁻ pH Probe

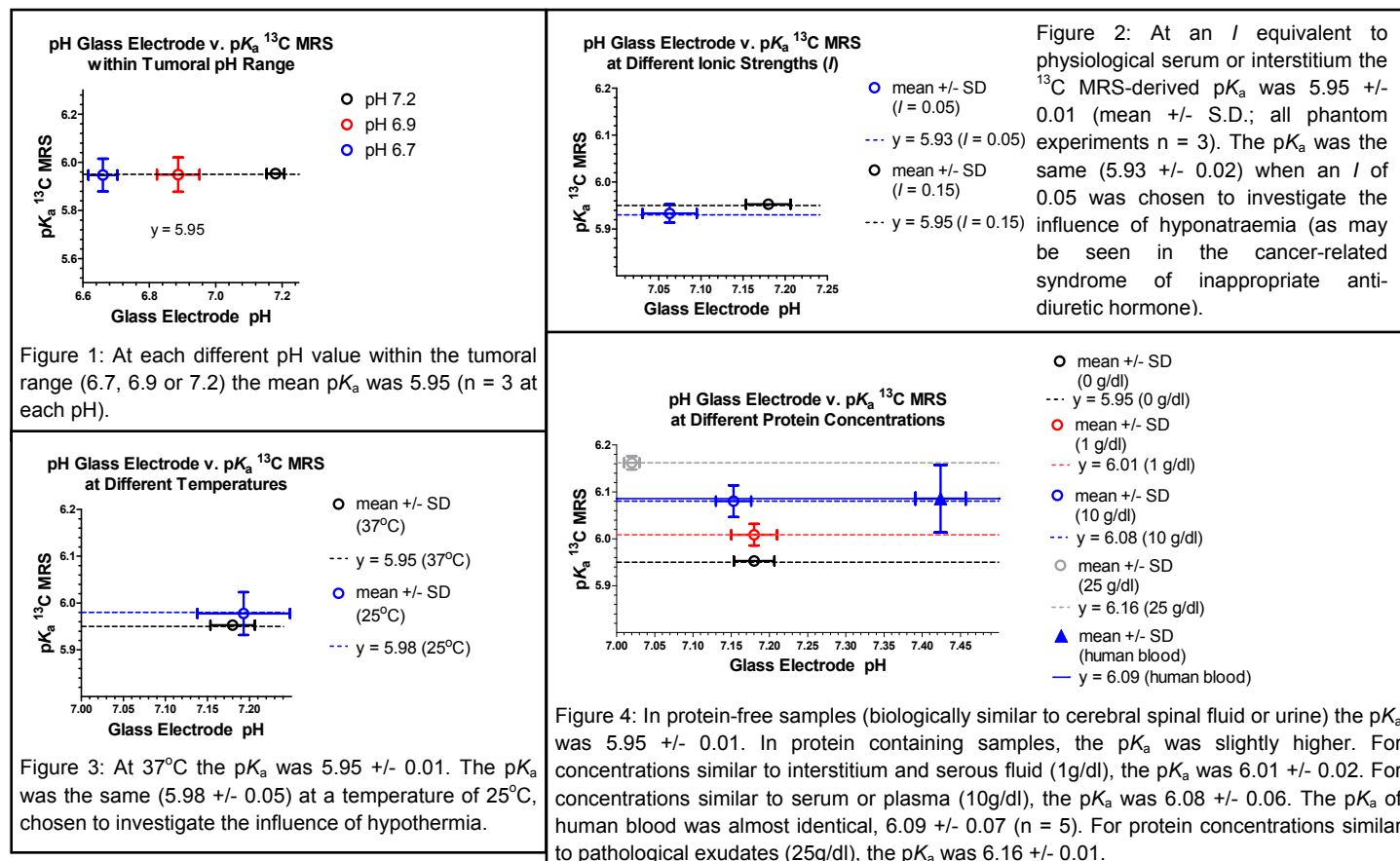
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Introduction: Tissue pH_e can be determined using ¹³C MRS and hyperpolarized ¹³C-labelled bicarbonate (H¹³CO₃⁻).¹ Using an assumed pK_a, the H¹³CO₃⁻ and ¹³CO₂ signal intensities allow pH determination using the Henderson-Hasselbalch equation. With a view to future clinical application we compared pH derived by DNP NMR with direct potentiometric measurement of H⁺ activity using a glass electrode. Using pK_a' = pH - log ([H¹³CO₃]/[¹³CO₂]), we assigned the pH determined potentiometrically as the standard and determined whether the ¹³C MRS derived pK_a diverges when there is alteration of ionic strength (*I*), pH, temperature and protein concentration within a clinically relevant range of values. Additionally, the pK_a in human blood was determined.

Method: Cs H¹³CO₃ was prepared, polarized and dissolved using a method similar to that described previously.¹ Following dissolution, 2ml of 29mM H¹³CO₃⁻ was added to a 5ml phantom and the solution mixed. Phantoms consisted of a solution of 4-(2-hydroxyethyl)-1-piperazineethanesulfonic acid (HEPES, Sigma), NaOH and NaCl to give a physiological *I* of 0.15. To investigate low ionic strength an alternative *I* of 0.05 was used. 12.5 Wilbur-Anderson units/ml of carbonic anhydrase (Sigma) was added to all phantoms. For experiments designed to simulate the range of pHs in tumors, the final pH was 6.7, 6.9 or 7.2 (measured immediately after addition of H¹³CO₃⁻). For all other phantom experiments the final pH was 7.1-7.2. For protein concentration experiments, 0g/dl, 1g/dl, 10g/dl or 25g/dl of bovine serum albumin (BSA, Sigma) were added. Samples were prepared at 37°C and this temperature was maintained for the duration of each experiment. Additionally, samples maintained at 25°C were investigated. A direct potentiometer (Radiometer) with a protein-compatible glass electrode (VWR) was calibrated with new buffer reagents using the manufacturer's standards. For human blood experiments a portable direct potentiometer (i-STAT, Abbott, NJ) was calibrated using the manufacturer's standards. After venepuncture, blood was heparinised and used immediately.

The NMR tube was placed in a 10mm broadband probe (Varian, Palo Alto, CA) tuned to 100.6MHz, in a vertical 9.4T, 8.9cm bore magnet (Oxford Instruments, UK) interfaced to a Varian INOVA spectrometer. Spectra of the hyperpolarized ¹³C label using low flip-angle pulses (5°), 2μs pulse width, 1 sec repetition time, 1 transient per spectrum, 6 kHz spectral width collected into 2048 data points. 120 spectra were acquired and processed with 10Hz exponential line broadening.

Results:



Discussion: The negative logarithm of the apparent dissociation constant of carbonic acid (H₂¹³CO₃) pK_a' is influenced by temperature, pH and ionic strength.^{2,3} It is a composite constant including factors such as the activity and degree of dissociation of the H¹³CO₃⁻ ion.² It was not known whether a pK_a derived by ¹³C MRS diverges from that derived by direct potentiometry within a clinically relevant range of values. The results demonstrated that within this range, the ¹³C MRS-derived pK_a appears invariant to *I*, pH and temperature. We also showed that pK_a increases as protein concentration increases. However, given the small variation throughout an entire spectrum of clinically relevant protein concentrations this variation is unlikely to be clinically relevant for the purposes of imaging pH. If pH_e derived by ¹³C MRS is weighted by capillary pH rather than tumor interstitial pH then it might be prudent to adopt a 'blood' or 'plasma' pK_a of 6.1 rather than an 'interstitial' pK_a of 6.0 for oncological imaging – this will ensure direct equivalence with pH determined potentiometrically.

¹Gallagher FA et al Nature (2008) 453: 940-943. ²Severinghaus J et al Appl Physiol (1956) 9:201-204. ³Deane and Smith J Biol Chem (1957) 227: 101-106.