MR/OPTICAL IMAGE-GUIDED TWO-COMPONENT NANO-DELIVERY SYSTEMS TARGETING HER2/NEU OVEREXPRESSING CANCER CELLS

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Introduction

The overexpression of Her2/neu, epidermal growth factor receptor (EGFR), which regulates the cell proliferation and differentiation, leads to the poor prognosis in human breast cancer [1]. The affinity of cancer therapeutics can be increased by the targeted drug delivery followed by controlled internalization in the cancer cells. The two-component delivery system overcomes the barriers of extravasation from vessels and diffusion to the target site. The first component is a high-affinity targeting molecule such as functionalized monoclonal antibody (mAb). The secondary component cross links the primary components forming a network only on the targeted receptor overexpressing cancer cells which leads to the macro-scale internalization and efficient delivery of high dose of therapeutics to the cytoplasm. This strategy exhibits the low effect on non-specific binding sites and on normal cells expressing basal levels of the receptor. The new two-component delivery system consists of a target specific biomolecule/antibody and a carrier molecules/platform. As a first targeting component, we selected the antibody, trastuzumab (Herceptin®) which specifically binds extracellular domain of the Her2/neu receptors. It also provides secondary binding motif for cargo molecule/platform. The cargo-carrier is a multi-task molecule/platform which transports of therapeutic, carries imaging agents for optical/MRI imaging, and can chemoselectively bind to the target-specific biomolecule. It acts as a biocompatible nanoparticle carrier systems similar to nanocapsules and nanospheres [2].

Methods

The target specific trastuzumab was functionalized with terminal azido PEGylated linkers and labeled with fluorochrome (Rhodamine for *in vitro* and NIR CF-680 for *in vivo* studies). The degree of functionalization and labeling was determined and optimized by MALDI-TOF and absorbance/fluorescence methods. The cargo carrier, BSA was substituted with DTPA and Gd, functionalized with strained promoted alkyne, dibenzocyclooctyne (DIBO) and labeled with fluorophores (Alexa-488 for *in vitro* and NIR CF-750 for *in vivo* studies). The degree of valency, DTPA-Gd substitution and fluorescent marker labeling was determined and optimized by MALDI-TOF, quantitative MRI, and aborbance/fluorescence methods. The two-component *nano*-delivery system was studied *in vitro* using Her2/*neu* overexpressing, human breast cancer BT-474 cells. The cells were first treated with modified Herceptin, Her(PEG₄-Az)₂₂(Rhod)₂ (10 µg/mL) and incubated at 37° for 30 min for immunolabelling on Her2/*neu* receptors. The secondary component, BSA(DIBO)₁₀(Alexa-488)₂ was added (2 µM) and imaged using a confocal fluorescent microscopy. The carrier molecule was also substituted with the DTPA ligand followed by Gd to obtain BSA(DTPA-Gd)₁₂(DIBO)₁₀(Alexa-488)₂.

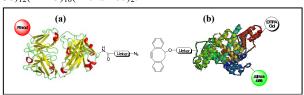


Figure 1. Two delivery components (a) Her(PEG₄- Az)₈ (Rhod/CF 680)₂ (b) BSA(DTPA- Gd)₁₂(DIBO)₁₀(Alexa 488/CF750)₂

Results

In the *in vitro* cell labeling fluorescent experiment, the colocalization of two spectral fluorescent images exhibits the presence of two components in same physical location after 1,2-dipolarcycloaddition forming a stable and bio-neutral 1,2,3-triazole linker. The MRI cell pellet study of the delivery system exhibits the significant drop in T_I compared to the control. For the BT-474 human breast cancer xenograft, SCID/nude mice were implanted with the pellets containing 0.72 mg of 17α -estradiol (sustained released 90 days) using a trocar and inoculated with BT-474 cells $(5\times10^6$ cells, mixed with equal volume of Matrigel) in left thoracic mammary pad. The xenographed mouse was injected with modified herceptin via tail vein followed after 4 h by the secondary component. Quantitative T_I maps were

reconstructed from 3D T_1 -weighted RARE sequence acquired pre-injection and at 1,3,6, and 12 h post-injection of modified BSA with TR = 250 ms, 500 ms, 1s, 2s, and 4s using a 9.4T Bruker MRI spectrometer. *In vivo* optical images of mice were obtained using a KODAK *in vivo* multispectral imaging system.

Discussion

Confocal fluorescent images of BT-474 cells in *in vitro* study exhibit the strong emission signal of two fluorophors ($\Delta \lambda_{emi}$ / $\Delta \lambda_{emi}$ =64/56 nm) and good spatial colocalization of two components after cell labeling with the two-component delivery system. Efficient cell surface labeling demonstrates the high affinity binding of the receptor by functionalized trastuzumab. The cargo-carrier can also chemoselectively bind with the modified mAb under physiological conditions. Based on encouraging MRI imaging results of cell pellets, we applied two-component delivery system

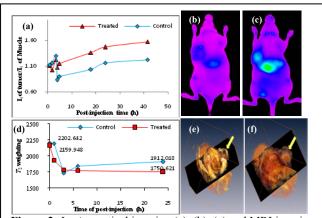


Figure 2. *In vivo* optical imaging (a), (b), (c) and MRI imaging (d), (e), (f) of two-component *nano*-delivery

to *in vivo* imaging and delivery study using Her2/*neu* overexpressing BT-474 xenografts in mouse models. The change of fluorescent intensity in the specifically labeled tumor with respect to the control is shown in Figure 2 (a). *In vivo* NIR fluorescent imaging are shown in Figure 2 (b) control and (c) treated mice. A mouse without PEG₄-Az on Herceptin was used as the control. The change of the mean tumor T_I times in control and treated mice are shown in Figure 2 (d). MRI images of mice highlighting the tumor-sites are shown in Figure 2 (e) control and (f) treated mice. Initial increase of fluorescent intensity and drop of T_I in both control and treated mice can be interpreted by EPR effect, but clearance was significantly faster in controls. MRI imaging exhibits specific T_I reduction for the two component delivery system, suggesting possible translational role of non-invasive image-guided strategy for cancer therapy.

References

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