

T2* and ADC Simultaneous Measurements of in vivo Symptomatic and Asymptomatic carotid atherosclerotic plaques Using 2D ss-SGE-DWEPI Technique

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INTRODUCTION: Many Studies have shown that hemorrhage is highly correlated with neurologic events in patients with carotid stenosis ⁽¹⁻²⁾. Hemorrhage is therefore an important plaque component and can be detected with MR thrombus imaging ⁽³⁾. It has been reported that Type I (fresh) hemorrhage occurred more often in patients with symptomatic plaques ⁽⁴⁾. A previous ex vivo DWI study reported that the ADC in hemorrhage varies according to the processes that occur during the successive phases of aging ⁽⁵⁾. Our 2D-IMIV-DWEPI sequence has demonstrated the ability of in vivo DWI to separate hemorrhage, lipid and arterial wall ⁽⁶⁾. Iron has consistently been found in higher concentrations in atherosclerotic plaque compared to vessel tissue ⁽⁷⁾. Iron may be incorporated into hemoglobin or bound to the storage proteins ferritin and hemosiderin, both of which cause measurable changes in local magnetic field homogeneity ⁽⁶⁾. It has been reported that intraplaque T₂* measurement distinguished symptom-producing from non-symptomatic plaques in patients with carotid atherosclerosis ⁽⁸⁾. We have developed a novel 2D singleshot spin-/gradient echo- diffusion weighted EPI (2D ss-SGE-DWEPI) sequence that can measure simultaneously the diffusivity and T₂* of water protons in carotid plaque. The purpose of this study was to determine retrospectively if T₂* and ADC value obtained from a 2D ss-SGE-DWEPI sequence can simultaneously depict differences between symptomatic and asymptomatic carotid atherosclerotic plaque.

METHOD: 2D ss-IMIV-DWEPI was modified to create the additional readout of a gradient echo (GE EPI) as shown in Fig.1. A pair of refocusing and inversion (RI) 180° RF pulses immediately follows the excitation 90° pulse to confine the reduced phase FOV for interleaved multiple slice imaging (IMIV). The diffusion sensitized gradients were applied before and after the RI pulses. After a diffusion weighted spin echo (SE EPI) is formed at TE, this signal further evolves with T₂* decay. A gradient echo (GEPI) provides the signal of T₂* decay during ΔTE caused by local field variation. The signal equations of two echoes are described in Eqs (1) and (2). To evaluate the feasibility of T₂* measurement with 2D ss-SGE-DWEPI, MRI studies of five symptomatic and five asymptomatic patients with hemorrhage positive atherosclerosis were performed on a Siemens Trio 3T MRI scanner with home built carotid coils. The imaging parameters for 2D ss SGE-DWEPI were: ΔTE=42ms TR=3000ms, imaging matrix = 160x40, 2 mm slice thickness. The in-plane spatial resolution for data acquisition was 1.0x1.0mm. Scan time was 2:24 min for 42 magnitude averages. DWI with b=0 and 500 s/mm² were interleaved. The ADC and T₂* maps were calculated and displayed using IDL. While ADC maps were created only using SE DWI, T₂* maps were created using two echoes images with b=0. 3D MPRAGE and T1w images were acquired at the same slice locations as the ADC and T₂* maps.

$$S_{SE}(\vec{r}, t) = S_0(\vec{r})e^{-b \cdot D}e^{-\frac{TE}{T_2^*(\vec{r}, t)}} \quad (1)$$

$$S_{GE}(\vec{r}, t) = S_{SE}(\vec{r}, t)e^{-\frac{\Delta TE}{T_2^*(\vec{r}, t)}} \quad (2)$$

RESULTS: Table 1 Mean T₂*, T₁ and ADC values from 10 patients

	Symptomatic	Asymptomatic	P value
T2*(ms)	23±3.8	39±5.8	p<0.001
ADC (10 ⁻³ mm ² /s)	0.85±0.24	1.41±0.48	p=0.003

Three ROIs per each patient were selected in visible plaque. The mean T₂* and ADC values for plaque obtained from the 10 subjects are summarized in Table 1. Symptomatic compared to asymptomatic patients had significantly lower plaque T₂* (p<0.001) and ADC (p=0.003) values. Our T₂* value is close to the value reported previously ⁽⁸⁾. Fig 2 displays 3D MPRAGE, T1w images, T₂* and ADC maps from a symptomatic and an asymptomatic subject, each with intramural hemorrhage. The T₂* and ADC values obtained from the red ROIs in Fig. 2 were 24/35 ms and 0.91/1.25x10⁻³mm²/s, respectively.

DISCUSSION: We found that symptomatic plaque has a significantly lower ADC compared to values obtained from asymptomatic plaque. Previous ex vivo study reported that the ADC of fresh hemorrhage (0.72x10⁻³mm²/s) is lower than the ADC (1.33x10⁻³mm²/s) of organized hemorrhage ⁽⁵⁾. Our ADC results are thus consistent with the expectation that the fresh hemorrhage is found significantly more often in patients with symptomatic plaques. The observation of a shortened T₂* in symptomatic patients is also consistent with the expectation that symptomatic subjects should show a shift of the type of iron complexes present. The shortened T₂* suggests a shift to aggregate iron complexes that have greater local effects on magnetic susceptibility. The small sample size is a limitation of this study. Further study will include identifying changes in the amount, species, and chemistry of intra-plaque iron during the course of atherosclerosis development. The measurements of T₂* and ADC obtained from 2D ss-SGE-DWEPI in our study revealed significant differences in the hemorrhage morphology of symptomatic and asymptomatic plaques. This approach might be used to characterize high-risk plaque and ultimately identify at-risk patients.

ACNOWLEDGEMENT: : Supported by HL 48223, HL 53696, Siemens Medical Solutions, The Ben B. and Iris M. Margolis Foundation, and the Clinical Merit Review Grant from the Veterans Administration health Care System.

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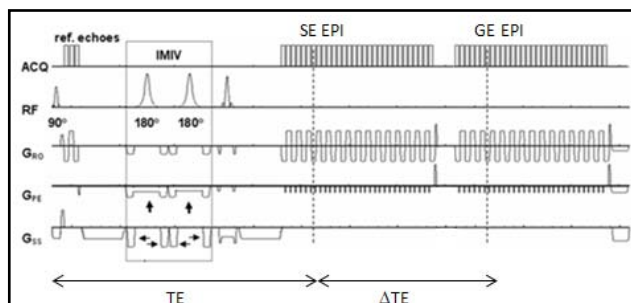


Fig.1 2D ss-SGE-DWEPI pulse sequence diagram

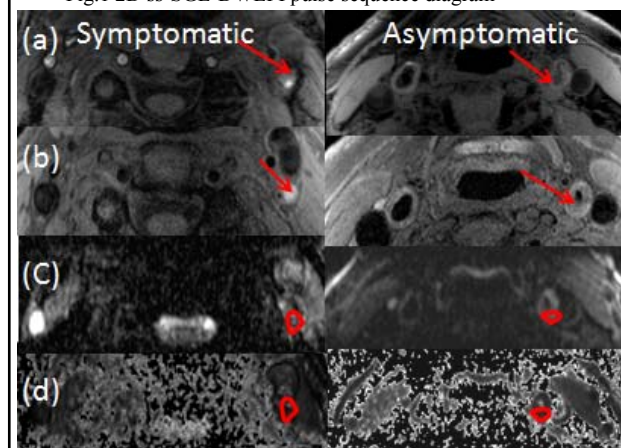


Fig.2 MP RAGE (a), T1w (b), ADC (c) and T₂* (d) maps from symptomatic and asymptomatic patients.