

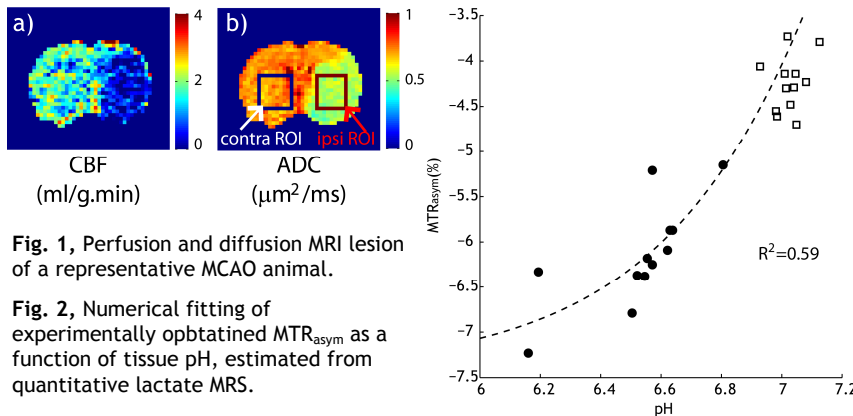
# Imaging acute ischemic tissue acidosis with quantitative in vivo amide proton transfer (APT) MRI

Phillip Zhe Sun<sup>1</sup>, Enfeng Wang<sup>1</sup>, and Jerry S Cheung<sup>1</sup>

<sup>1</sup>Department of Radiology, Athinoula A. Martinos Center for Biomedical Imaging, Charlestown, MA, United States

**Introduction** Amide proton transfer (APT) imaging is sensitive to pH with significantly higher spatiotemporal resolution than spectroscopy<sup>1-3</sup>. In vivo APT MRI contrast is often calculated using the magnetization transfer (MT) asymmetry analysis ( $MTR_{asym}$ ), which is complex due to relaxation and concomitant RF irradiation effects. APT contrast approximately scales with  $T_1$  relaxation time. In addition to the pH-dependent APT contrast,  $MTR_{asym}$  is susceptible to slightly asymmetric magnetization transfer effects<sup>4-6</sup>. Moreover, the experimentally obtained CEST MRI contrast strongly varies with RF irradiation power, which can be described using the saturation/labeling coefficient and RF spillover effects<sup>7</sup>. We postulated that tissue pH can be reasonably quantified from pH-weighted APT MRI by taking into account major concomitant RF irradiation effects.

**Materials and Methods** Animal model: Permanent middle cerebral artery occlusion (MCAO) was induced in adult male Wistar rats (n=12). MRI: All experiments were conducted at 4.7T within 90 min after MCAO. Point-resolved spectroscopy (PRESS) was obtained from a region of interest (ROI) of 3.5 mm<sup>3</sup> (TR/TE=2000/144ms, NA=512) within the DWI lesion. Multi-parametric perfusion, diffusion, pH-weighted APT,  $T_1$  and  $T_2$  MRI (5 slices, 2mm/slice) were obtained (FOV: 25x25mm, matrix: 64x64, bandwidth 200kHz). Specifically, we acquired perfusion (TR/TS/TE=6500/3250/14.8ms, NA=32)<sup>7</sup>, APT (NA1/NA2=8/32, TR/TE=6500/14.8ms)<sup>8</sup>, diffusion (TR/TE=3250/54ms, b=250 and 1000 s/mm<sup>2</sup>, NA=16)<sup>9</sup>,  $T_1$  (inversion recovery, TI from 250 to 3000 ms, NA=4) and  $T_2$  (SE MRI, TR/TE1/TE2=3250/30/100 ms, NA=16). We have  $MTR_{asym} = \Delta MTR_{asym} + f \cdot k / (R_{1w} + f \cdot k) \cdot \alpha \cdot (1 - \sigma)$ , where  $\alpha$  is labeling coefficient,  $\sigma$  is the RF spillover effect, f and k are the amide proton concentration and exchange rate, and  $R_{1w}$  is the bulk tissue water relaxation time.

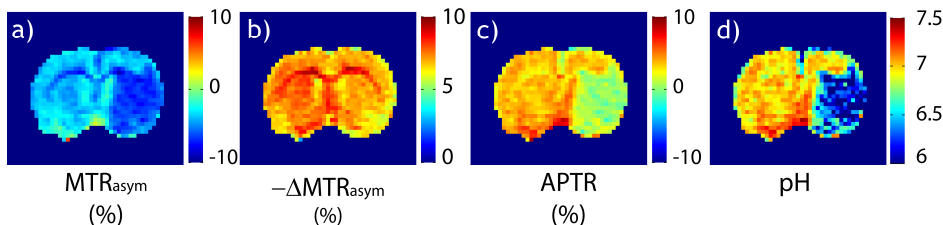


**Fig. 1**, Perfusion and diffusion MRI lesion of a representative MCAO animal.

**Fig. 2**, Numerical fitting of experimentally obtained  $MTR_{asym}$  as a function of tissue pH, estimated from quantitative lactate MRS.

**Results and Discussion** Fig. 1 shows CBF and ADC images from a representative stroke animal. CBF decreased from  $2.3 \pm 0.54$  ml/g.min in the contralateral normal area to  $1.13 \pm 0.57$  ml/g.min in the ischemic lesion, representing a relative decrease of  $52 \pm 19\%$  ( $P < 0.01$ ). pH-weighted  $MTR_{asym}$  was  $-4.3 \pm 0.3\%$  in the contralateral normal ROI, which decreased to  $-6.1 \pm 0.6\%$  upon ischemia ( $P < 0.01$ ). In addition, ADC decreased from  $0.72 \pm 0.03$  to  $0.56 \pm 0.03$   $\mu\text{m}^2/\text{ms}$  ( $P < 0.01$ ). Lactate was measured from an ROI within the ADC lesion. the ischemic lesion showed elevated lactate signal, with a Choline and Creatine normalized lactate peak (i.e., Lac/(Cho+Cr)) being  $0.80 \pm 0.21$ .

The ipsilateral ischemic ROI-based  $MTR_{asym}$  is plotted as a function of pH in Fig. 2. The lactate concentration [Lac] was calculated from PRESS MRS, with Creatine and Choline concentration being 4.79 and 9.35 mmol/kg, respectively (Florian et al., 1996). Tissue pH was estimated from the lactate concentration at  $\text{pH} = -0.0593 \cdot [\text{Lac}] + 7.2$ , as shown by results of Chang et al.<sup>8</sup> in vivo  $MTR_{asym}$  was negative due to the baseline shift of  $\Delta MTR'_{asym}$ .  $K_{sw}$  was calculated using  $k_{sw} = 5.57 \cdot 10^{\text{pH}-6.4}$  and two parameters,  $\Delta MTR'_{asym}$  and f, were numerically solved from Eq. 2, being  $-7.44\%$  and  $1:867$ , respectively. We calculated the contralateral normal tissue pH from quantitative APT MRI, and overlaid it in Fig. 2 (open squares). This shows that the proposed quantitative pH MRI can reasonably describe in vivo APT MRI contrast, both contralateral normal and ipsilateral ischemic regions.



**Fig. 3**, Derivation from pH-weighted  $MTR_{asym}$  (a),  $\Delta MTR_{asym}$  shift (b), pH-weighted APT MRI (c) and quantitative tissue pH (d).

the corpus callosum in the  $MTR_{asym}$  map. Fig. 3c shows the endogenous APT map (i.e.,  $\text{APTR} = MTR_{asym} - \Delta MTR'_{asym}$ ). Indeed, the pH map clearly depicts tissue acidification in the ischemic lesion (Fig. 3d). Ischemic tissue pH estimated from APT MRI was  $6.44 \pm 0.24$ , in good agreement with that estimated from lactate MRS of  $6.53 \pm 0.18$ . In comparison, the contralateral normal tissue pH was  $7.03 \pm 0.05$ , and the pH difference between the ischemic and contralateral normal regions was  $-0.59 \pm 0.22$  ( $P < 0.01$ ).

**References** 1)Zhou et al., Nat. Med 2003; 9:1085-90. 2)Jokivarsi et al, MRM 2007; 57 (4):647-53. 3)Sun et al. JCBFM 2011; 65:1743-50. 4)Pekar et al. MAM 1996;35:70-79. 5)Hua et al. MRM 2007;58:786-93. 6) Mougin et al. Neuroimage 2010;49:272-81. 7) Sun et al. MRM 2007;57:405-10. 8) Chang et al. MRM 1990;13:6-13.