#### ISMRM 2011 Sunrise Educational Course on Image Reconstruction

Parallel Imaging Reconstruction I: Cartesian

Jonathan R. Polimeni, Ph.D. Athinoula A. Martinos Center for Biomedical Imaging Massachusetts General Hospital, Charlestown, MA, U.S.A. jonp@nmr.mgh.harvard.edu

## Syllabus

The goal of this presentation is to briefly introduce the central concepts in parallel imaging reconstruction for *k*-space data that is sampled on a Cartesian grid.

#### **Cartesian Sampling**

Cartesian sampling refers to an acquisition in which Fourier-encoded or *k*-space data is sampled on a rectangular lattice with regular spacing, i.e., on a set of points defined on a Cartesian coordinate system. This basic sampling scheme is commonly used because of its straightforward implementation and because the mapping of the *k*-space data into the image domain via a uniform Discrete Fourier Transform can be carried out extremely efficiently and rapidly with the Fast Fourier Transform algorithm—which is a major advantage of Cartesian sampling methods.

#### Parallel Imaging with Receive Coil Arrays

Parallel imaging is a broad category of data acquisition and image reconstruction techniques that exploit the redundant information obtained when measuring *k*-space data with an array of radio frequency (RF) detectors (a.k.a., a "phased-array" of RF coil detectors). The foundation of hardware design considerations and software image reconstruction approaches required when using these receive coil arrays was originally laid out in a now-classic article by Roemer *et al.* [1]. In this article, the authors described how each coil element in the detector array *in parallel* receives the Fourier-encoded image from a different perspective and a different region of the imaged object, and how these individual images can be combined to form a full image that optimizes the final image signal-to-noise ratio (SNR) provided two additional pieces of information: the spatial *sensitivity profile* of each individual coil element in the image domain, and the *noise covariance* of the thermal noise measured between all pairs of coil elements. It was demonstrated that arrays of small coil elements placed close to the object being imaged could provide dramatic improvements in image SNR compared to conventional single-channel volume coils.

### **Accelerated Parallel Imaging**

Beyond the SNR benefits afforded by receive coil arrays, the partially redundant information collected by the coil array can also be exploited to *accelerate* the image encoding by skipping some of the encoding steps during the acquisition and then estimating this missing information during image reconstruction, thereby reducing the time required for the acquisition [2–5]. In the Cartesian sampling setting, this acceleration consists of uniformly undersampling the *k*-space data in some region of *k*-space, which leads to a violation of the Nyquist criterion and consequently results in aliasing in the image domain. So, for example, to accelerate a single two-dimensional, Cartesian-sampled, Fourier-encoded image acquisition by a factor of 2, every other *k*-space phase encoding line would be omitted during the measurement, which effectively halves the image field of view; similarly, to accelerate by a factor of *R* only every *R*th line is acquired. The goal of accelerated parallel imaging reconstruction algorithms is to remove the aliasing from the resulting image data by leveraging the partially independent information about the imaged object from the array of RF coil detectors.

# **Two Categories of Accelerated Parallel Imaging Methods**

There is a wide variety of accelerated parallel imaging methods that each estimate this skipped data in different ways in order to remove the image aliasing. What these algorithms have in common is that they all require some information about the spatial sensitivity profile of each coil element in the array. Accelerated parallel imaging reconstruction methods can be lumped into two categories: methods that require explicit estimates of the coil sensitivity profiles of the array, and "auto-calibrated" methods that can estimate the coil sensitivity profiles from a small amount of Nyquist-sampled calibration data that is acquired together with the image data. Of all of the accelerated parallel image reconstruction methods available, the two methods that are most commonly used are the SENSE method [6-8] and the GRAPPA method [9, 10], which are both implemented and made available by the MR scanner manufacturers for online reconstruction of accelerated parallel imaging data. The SENSE method is an example of a reconstruction approach that requires explicit estimates of the coil sensitivity profiles and is a natural extension of the original parallel imaging combination methods introduced by Roemer et al. [1]. The GRAPPA method is an example of an autocalibrated approach that is based on SMASH theory [11–14]. For these reasons, the central concepts of accelerated parallel imaging reconstruction will be presented via a detailed discussion of these two well-known algorithms.

### **Benefits and Applications of Cartesian Parallel Imaging**

Today, due to the ubiquity of receive coil arrays and the availability of online image reconstruction methods, accelerated parallel imaging is routinely used in conventional imaging in both standard clinical and research settings. Accelerated parallel imaging not only shortens scan session duration and enables faster temporal sampling in dynamic imaging [15], but it has also been applied to improve image quality by, for example: reducing image artifacts [16–20], enhancing image resolution [21], reducing vulnerability to susceptibility distortion while reducing voxel sizes in echo-planar imaging [22, 23], and increasing the sensitivity of diffusion-weighted imaging by shortening the echo time [24].

## Errors and Error Characterization in Accelerated Parallel Imaging

While accelerated parallel imaging has many apparent benefits, it is also important to consider the limitations of the approach. The degree of acceleration is fundamentally limited by the number of coil elements in the array, and in practice the acceleration factor is far smaller than the number of elements for conventional parallel imaging methods using Cartesian sampling. The ability of these methods to synthesize data that is skipped during the accelerated acquisition is primarily limited by the degree of independence between the information carried by the elements of the array—the more unique the coil sensitivity profiles, the more degrees of freedom are in the coil array data and the more flexibility the array has to estimate missing data [25]. Two types of errors gradually arise when the acceleration increases beyond the capacity of the array: statistical errors in the form of noise amplification imparted by the reconstruction process, and systematic errors in the form of unresolved aliasing artifacts in the image domain. There is an intrinsic loss of SNR inherent in any accelerated acquisition relative to conventional, fully-sampled acquisitions due to the reduced number of k-space samples acquired for each image. The intrinsic SNR penalty is the square root of the acceleration factor R. The additional noise amplification (beyond the intrinsic VR) has been well characterized for the SENSE algorithm [6], where it is primarily dependent on the geometry of the coil array; for this reason the level of noise amplification at a particular image pixel is denoted as the geometry factor or *g*-factor at that pixel. G-factor maps across all image pixels can therefore provide an estimate of the noise amplification incurred by the SENSE image reconstruction. Analogous noise amplification maps can be estimated for the GRAPPA-like reconstruction algorithms [26–30]. Unresolved aliasing artifacts can also arise and are primarily due to errors in the estimates of the coil sensitivity profiles; these errors can be more challenging to detect, but error estimates based on artifact power and bias calculations have been proposed [28, 31, 32].

### New Directions: Massively Parallel Imaging with Cartesian Sampling

New techniques are emerging that are capable of dramatically increasing the acceleration for parallel imaging which also employ Cartesian sampling schemes. Threedimensional image encoding provides two phase encoding directions along which to accelerate which enables either higher acceleration factors or reduced errors at conventional acceleration factors [7, 33]. Accelerated parallel imaging can therefore be employed for three-dimensional single-shot "echo-volumar imaging" (i.e., the three-dimensional generalization of echo-planar imaging) that can collect an entire *k*-space volume with each excitation while maintaining a short total acquisition time [34, 35]. Some techniques have been demonstrated that omit the phase encoding in one direction entirely, thereby using acceleration factors that are far beyond the number of elements available in modern RF coil arrays through incorporating heavy amounts of prior information via regularization to make the image reconstruction tractable [36–39]. Similar approaches have been taken with multi-slice two-dimensional imaging that exploit the three-dimensional acceleration capabilities of modern RF coil arrays by acquiring multiple slices simultaneously then extracting each of the superimposed slices using accelerated parallel imaging reconstruction techniques [40–42]. These massively accelerated acquisitions and associated image reconstruction methods are still under development, but their potential to dramatically reduce acquisition times and thereby substantially boost temporal sampling rates makes them attractive for high-temporal-resolution functional neuroimaging applications [34–38, 41, 42].

# For More Information...

For those interested, there are many in-depth reviews of parallel imaging methodology and applications (e.g., Refs. 43, 44) and comparisons between the existing methods (e.g., Refs. 45–50). While this presentation is focused specifically on parallel imaging methods for Cartesian sampling acquisition, advanced techniques for more general acquisition schemes that are not constrained to Cartesian sampling grids will be discussed in the following presentation.

# References

[1] Roemer PB, Edelstein WA, Hayes CE, Souza SP, Mueller OM. The NMR phased array. Magn Reson Med. 1990; 16(2):192-225.

[2] Hutchinson M, Raff U. Fast MRI data acquisition using multiple detectors. Magn Reson Med. 1988; 6(1):87-91.

[3] Kwiat D, Einav S, Navon G. A decoupled coil detector array for fast image acquisition in magnetic resonance imaging. Med Phys. 1991; 18(2):251-65.

[4] Carlson JW, Minemura T. Imaging time reduction through multiple receiver coil data acquisition and image reconstruction. Magn Reson Med. 1993; 29(5):681-7.

[5] Ra JB, Rim CY. Fast imaging using subencoding data sets from multiple detectors. Magn Reson Med. 1993; 30(1):142-5.

[6] Pruessmann KP, Weiger M, Scheidegger MB, Boesiger P. SENSE: sensitivity encoding for fast MRI. Magn Reson Med. 1999; 42(5):952-62.

[7] Weiger M, Pruessmann KP, Boesiger P. 2D SENSE for faster 3D MRI. MAGMA. 2002; 14(1):10-9.

[8] Pruessmann KP, Weiger M, Börnert P, Boesiger P. Advances in sensitivity encoding with arbitrary k-space trajectories. Magn Reson Med. 2001; 46(4):638-51.

[9] Griswold MA, Jakob PM, Heidemann RM, Nittka M, Jellus V, Wang J, Kiefer B, Haase A. Generalized autocalibrating partially parallel acquisitions (GRAPPA). Magn Reson Med. 2002; 47(6):1202-10.

[10] Wang Z, Wang J, Detre JA. Improved data reconstruction method for GRAPPA. Magn Reson Med. 2005; 54(3):738-42. Erratum in: Magn Reson Med. 2006; 56(1):234.

[11] Sodickson DK, Manning WJ. Simultaneous acquisition of spatial harmonics (SMASH): fast imaging with radiofrequency coil arrays. Magn Reson Med. 1997; 38(4):591-603.

[12] Jakob PM, Griswold MA, Edelman RR, Sodickson DK. AUTO-SMASH: a self-calibrating technique for SMASH imaging. SiMultaneous Acquisition of Spatial Harmonics. MAGMA. 1998; 7(1):42-54.

[13] Sodickson DK. Tailored SMASH image reconstructions for robust in vivo parallel MR imaging. Magn Reson Med. 2000; 44(2):243-51.

[14] Heidemann RM, Griswold MA, Haase A, Jakob PM. VD-AUTO-SMASH imaging. Magn Reson Med. 2001; 45(6):1066-74.

[15] Niendorf T, Sodickson DK. Parallel imaging in cardiovascular MRI: methods and applications. NMR Biomed. 2006; 19(3):325-41.

[16] Bydder M, Larkman DJ, Hajnal JV. Detection and elimination of motion artifacts by regeneration of k-space. Magn Reson Med. 2002; 47(4):677-86.

[17] Larkman DJ, Atkinson D, Hajnal JV. Artifact reduction using parallel imaging methods. Top Magn Reson Imaging. 2004; 15(4):267-75.

[18] Atkinson D. Incoherent artefact correction using PPI. NMR Biomed. 2006; 19(3):362-7.

[19] Kellman P, McVeigh ER. Phased array ghost elimination. NMR Biomed. 2006; 19(3):352-61.

[20] Kim YC, Nielsen JF, Nayak KS. Automatic correction of echo-planar imaging (EPI) ghosting artifacts in real-time interactive cardiac MRI using sensitivity encoding. J Magn Reson Imaging. 2008; 27(1):239-45.

[21] Griswold MA, Jakob PM, Chen Q, Goldfarb JW, Manning WJ, Edelman RR, Sodickson DK. Resolution enhancement in single-shot imaging using simultaneous acquisition of spatial harmonics (SMASH). Magn Reson Med. 1999; 41(6):1236-45.

[22] Golay X, de Zwart JA, Ho YC, Sitoh YY. Parallel imaging techniques in functional MRI. Top Magn Reson Imaging. 2004; 15(4):255-65.

[23] de Zwart JA, van Gelderen P, Golay X, Ikonomidou VN, Duyn JH. Accelerated parallel imaging for functional imaging of the human brain. NMR Biomed. 2006; 19(3):342-51.

[24] Jaermann T, Crelier G, Pruessmann KP, Golay X, Netsch T, van Muiswinkel AM, Mori S, van Zijl PC, Valavanis A, Kollias S, Boesiger P. SENSE-DTI at 3 T. Magn Reson Med. 2004; 51(2):230-6.

[25] Buehrer M, Pruessmann KP, Boesiger P, Kozerke S. Array compression for MRI with large coil arrays. Magn Reson Med. 2007; 57(6):1131-9.

[26] Sodickson DK, Griswold MA, Jakob PM, Edelman RR, Manning WJ. Signal-to-noise ratio and signal-to-noise efficiency in SMASH imaging. Magn Reson Med. 1999; 41(5):1009-22.

[27] Yeh EN, McKenzie CA, Ohliger MA, Sodickson DK. Parallel magnetic resonance imaging with adaptive radius in k-space (PARS): constrained image reconstruction using k-space locality in radiofrequency coil encoded data. Magn Reson Med. 2005; 53(6):1383-92.

[28] Polimeni JR, Wiggins GC, Wald LL. Characterization of artifacts and noise enhancement introduced by GRAPPA reconstructions [Abstract]. Proc ISMRM. 2008; 16.

[29] Robson PM, Grant AK, Madhuranthakam AJ, Lattanzi R, Sodickson DK, McKenzie CA. Comprehensive quantification of signal-to-noise ratio and g-factor for image-based and k-space-based parallel imaging reconstructions. Magn Reson Med. 2008; 60(4):895-907.

[30] Breuer FA, Kannengiesser SA, Blaimer M, Seiberlich N, Jakob PM, Griswold MA. General formulation for quantitative G-factor calculation in GRAPPA reconstructions. Magn Reson Med. 2009; 62(3):739-46.

[31] Pipe JG, Duerk JL. Analytical resolution and noise characteristics of linearly reconstructed magnetic resonance data with arbitrary k-space sampling. Magn Reson Med. 1995; 34(2):170-8.

[32] McKenzie CA, Yeh EN, Ohliger MA, Price MD, Sodickson DK. Self-calibrating parallel imaging with automatic coil sensitivity extraction. Magn Reson Med. 2002; 47(3):529-38.

[33] Blaimer M, Breuer FA, Seiberlich N, Mueller MF, Heidemann RM, Jellus V, Wiggins G, Wald LL, Griswold MA, Jakob PM. Accelerated volumetric MRI with a SENSE/GRAPPA combination. J Magn Reson Imaging. 2006; 24(2):444-50.

[34] Rabrait C, Ciuciu P, Ribés A, Poupon C, Le Roux P, Dehaine-Lambertz G, Le Bihan D, Lethimonnier F. High temporal resolution functional MRI using parallel echo volumar imaging. J Magn Reson Imaging. 2008; 27(4):744-53.

[35] Witzel T, Polimeni JR, Wiggins GC, Lin F-H, Biber S, Hamm M, Seethamraju R, Wald LL. Single-shot echo-volumar imaging using highly parallel detection [Abstract]. Proc ISMRM. 2008; 16.

[36] Lin FH, Wald LL, Ahlfors SP, Hämäläinen MS, Kwong KK, Belliveau JW. Dynamic magnetic resonance inverse imaging of human brain function. Magn Reson Med. 2006; 56(4):787-802.

[37] Hennig J, Zhong K, Speck O. MR-Encephalography: Fast multi-channel monitoring of brain physiology with magnetic resonance. Neuroimage. 2007; 34(1):212-9.

[38] Lin FH, Witzel T, Mandeville JB, Polimeni JR, Zeffiro TA, Greve DN, Wiggins G, Wald LL, Belliveau JW. Event-related single-shot volumetric functional magnetic resonance inverse imaging of visual processing. Neuroimage. 2008; 42(1):230-47.

[39] McDougall MP, Wright SM. 64-channel array coil for single echo acquisition magnetic resonance imaging. Magn Reson Med. 2005; 54(2):386-92.

[40] Breuer FA, Blaimer M, Heidemann RM, Mueller MF, Griswold MA, Jakob PM. Controlled aliasing in parallel imaging results in higher acceleration (CAIPIRINHA) for multi-slice imaging. Magn Reson Med. 2005; 53(3):684-91.

[41] Moeller S, Yacoub E, Olman CA, Auerbach E, Strupp J, Harel N, Uğurbil K. Multiband multislice GE-EPI at 7 tesla, with 16-fold acceleration using partial parallel imaging with application to high spatial and temporal whole-brain fMRI. Magn Reson Med. 2010; 63(5):1144-53.

[42] Setsompop K, Gagoski BA, Polimeni JR, Witzel T, Wedeen V, Wald LL. Blipped CAIPIRHINA for simultaneous multi-slice EPI with reduced g-factor penalty [Abstract]. Proc ISMRM. 2010; 18(551).

[43] Pruessmann KP. Encoding and reconstruction in parallel MRI. NMR Biomed. 2006; 19(3):288-99.

[44] Larkman DJ, Nunes RG. Parallel magnetic resonance imaging. Phys Med Biol. 2007; 52(7):R15-55.

[45] Wang Y. Description of parallel imaging in MRI using multiple coils. Magn Reson Med. 2000; 44(3):495-9.

[46] Sodickson DK, McKenzie CA. A generalized approach to parallel magnetic resonance imaging. Med Phys. 2001; 28(8):1629-43.

[47] Bydder M, Larkman DJ, Hajnal JV. Generalized SMASH imaging. Magn Reson Med. 2002; 47(1):160-70.

[48] Heidemann RM, Ozsarlak O, Parizel PM, Michiels J, Kiefer B, Jellus V, Müller M, Breuer F, Blaimer M, Griswold MA, Jakob PM. A brief review of parallel magnetic resonance imaging. Eur Radiol. 2003; 13(10):2323-37.

[49] Blaimer M, Breuer F, Mueller M, Heidemann RM, Griswold MA, Jakob PM. SMASH, SENSE, PILS, GRAPPA: how to choose the optimal method. Top Magn Reson Imaging. 2004; 15(4):223-36.

[50] Hoge WS, Brooks DH. On the complimentarity of SENSE and GRAPPA in parallel MR imaging. Conf Proc IEEE Eng Med Biol Soc. 2006; 1:755-8.