

# Feasibility of Temperature Imaging of Fat and Water based on Methylen T1 and Water Proton Resonance Frequency

K. Kuroda<sup>1,2</sup>, M. Lam<sup>3</sup>, T. Iwabuchi<sup>1</sup>, M. Obara<sup>4</sup>, M. Honda<sup>5</sup>, K. Saito<sup>1</sup>, and Y. Imai<sup>5</sup>

<sup>1</sup>Graduate School of Engineering, Tokai University, Hiratsuka, Kanagawa, Japan, <sup>2</sup>Medical Device Development Center, Foundation for Biomedical Research and Innovation, Kobe, Hyogo, Japan, <sup>3</sup>Image Sciences Institute, University Medical Center Utrecht, Utrecht, Netherlands, <sup>4</sup>MR Marketing, Philips Electronics Japan Medical Systems, Shinagawa, Tokyo, Japan, <sup>5</sup>Department of Radiology, Tokai University, Isehara, Kanagawa, Japan

## INTRODUCTION

Noninvasive temperature imaging of fat is desired for thermal therapies such as high intensity focused ultrasound (HIFU) for breast and other tissue locations with high fat contents. Based on the temperature dependence of  $T_1$  of methylene ( $\text{CH}_2$ ) or methyl ( $\text{CH}_3$ ) protons(1), we have proposed a technique(2) using multiple flip angle(3), multipoint Dixon acquisitions and a least square estimation(4) (5). This technique can be combined with the water temperature imaging technique based on the proton resonance frequency (PRF) shift, because the intra-voxel signal fractions of water and fat protons can be obtained once the proton components are separated. Thus it is possible to combine the PRF-based water temperature map and the  $T_1$ -based methylene temperature maps. In this paper, feasibility of such an integrated temperature imaging technique is demonstrated.

## METHODS

A spoiled gradient recalled acquisition in steady state (SPGR) was designed to evaluate  $T_1$  of  $\text{CH}_2$  and/or  $\text{CH}_3$ . In the first shot, echoes with different TE's were acquired at a certain flip angle ( $\alpha_i$ ) to obtain real and imaginary parts of water,  $\text{CH}_2$  and  $\text{CH}_3$  signals based on the multipoint Dixon scheme(4). In the following shots, similar echo sets were obtained with different flip angles. Each data set was reconstructed separately to have the complex water,  $\text{CH}_2$  and  $\text{CH}_3$  images with different flip angles. The  $\text{CH}_2$  image sets were used to obtain  $T_1$  maps, which were then converted to temperature change maps. The complex water images were used to calculate the phase change corresponding to the PRF shift and thus temperature change maps. Then the PRF-based water temperature images and the  $T_1$ -based  $\text{CH}_2$  temperature images were combined as a weighted sum of the two different temperature maps. Phantom experiments were conducted at 3T (Achieva, Philips) with mayonnaise tubes in a water bath. Temperature in the phantom was monitored with a fiberoptic thermometer (Model 3000, Luxtron). One of the mayonnaise tubes was heated up to around 55 degree, while the other bottles were kept at room temperature (27°C). The following parameters were used; TR, 36 ms, TE,  $n \cdot \text{TE}_0$  with  $n = 1, 2, \dots, 16$  and  $\text{TE}_0 = 1.00, 1.05, \dots, 1.30$  ms; number of echoes, 16; flip angles, 20, 50 and 70 degrees; spatial matrix,  $128 \times 128$ ; SENSE factor, 2. The acquisitions were repeated in the cooling period of the sample. In order to obtain the relationship between  $T_1$  of  $\text{CH}_2$  and temperature, inversion-prepared single-voxel PRESS MRS was performed with the following parameters; TR, 12,000 ms; TI, 50, 100, 200, 300, 500, 700, 1000 and 12,000ms; voxel size,  $15 \times 15 \times 15 \text{ mm}^3$ .

## RESULTS

The proton spectra of the mayonnaise obtained by MRS is shown in Fig. 1. The signal ratio between water,  $\text{CH}_2$ ,  $\text{CH}_3$  and other proton components were 1 : 2.13 : 0.102 : 0.685 in the particular phantom at room temperature. The temperature coefficient of  $T_1$  of  $\text{CH}_2$  was 1.39 %/°C at 30°C as shown in Fig. 2. The value was close to that obtained in a 11T spectrometer experiments(1). Total time for the 3-flip angle SPGR acquisitions were 6 seconds. Successful separation of the chemical species and calculation of  $T_1$ 's for  $\text{CH}_2$  were performed by using the first 5 echoes. Temperature images obtained by the  $\text{CH}_2$   $T_1$  only and by both  $\text{CH}_2$   $T_1$  and water PRF are shown in Fig. 3.

## DISCUSSIONS

As a first implementation of the technique, three components model including  $\text{H}_2\text{O}$ ,  $\text{CH}_2$  and  $\text{CH}_3$  were used. The resultant temperature images in the upper row of Fig. 3 exhibited larger error in temperature estimation at higher temperature elevations, partly because of the incomplete setting of the TE values at such temperature range. The error became somewhat smaller when temperature estimation with water PRF was included. The results demonstrated the feasibility of the combined temperature imaging technique based on both methylene  $T_1$  and water PRF. Although the fatty acid proton components other than  $\text{CH}_2$  and  $\text{CH}_3$  were not considered here, it is preferable to include those components. Also, the frequency separations between the signal components can be unknown in order to avoid the signal separation error induce by the incomplete setting of TE's. These optimization(6) procedures are under our current examination.

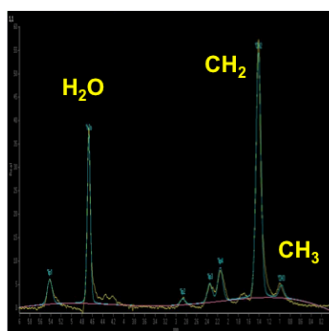


Fig. 1 Typical proton spectra of the mayonnaise sample at 3T.

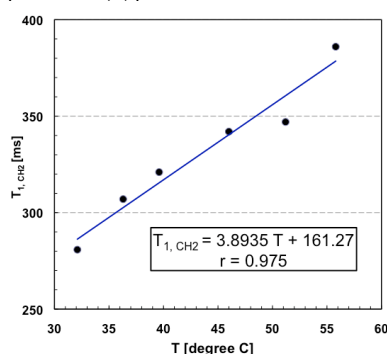


Fig. 2 Relationship between temperature and  $T_1$  of  $\text{CH}_2$  obtained by MRS at 3T.

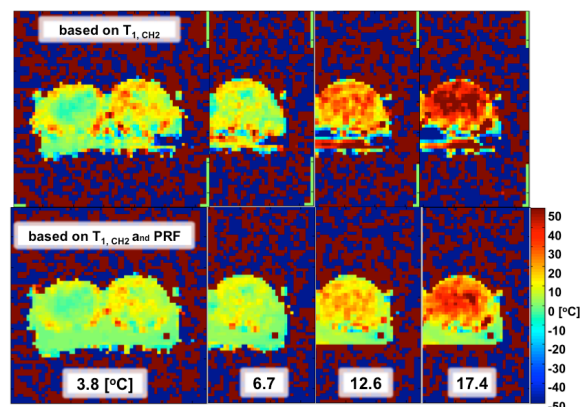


Fig. 3 Temperature elevation maps of the mayonnaise phantom based on  $T_1$  of  $\text{CH}_2$  (upper row) and both  $T_1$  of  $\text{CH}_2$  and PRF of water (bottom row). Numbers on the labels show the temperature elevation values measured by the optical thermometer.

## CONCLUSION

The basic function of the proposed technique with multipoint Dixon and multiple flip angle scheme was demonstrated. The technique can image temperature based on  $T_1$  of  $\text{CH}_2$  and PRF of water in 6 second, which seemed to be practical for monitoring temperature in breast under HIFU. Optimization of the echo spacing and component separation process are necessary to improve the accuracy of the measurement.

## REFERENCES

1. Kuroda K et al. Magn Reson Med Sci. accepted.
2. Kuroda K et al. Proc Joint Annual Meeting, ISMRM-ESMRMB. 2010;p. 1818.
3. Deoni SCL et al. Magn Reson Med. 2003;49:515-26.
4. Reeder SB et al. Magn Reson Med. 2004;51:35-45.
5. Liu CY et al. Magn Reson Med. 2007;58(2):354-64.
6. Pineda AR et al. Magn Reson Med. 2005;54:625-35.