

# In vivo Relaxation Parameters of Oxygen-17 ( $^{17}\text{O}$ )

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## INTRODUCTION

Cellular energy production is closely connected to the metabolism of oxygen ( $\text{O}_2$ ) to water (oxidative phosphorylation). Direct  $^{17}\text{O}$ -MRI can assess the *in vivo* concentration of  $\text{H}_2^{17}\text{O}$  metabolized from inhaled  $^{17}\text{O}$  gas. Thus, it measures the oxygen turnover providing functional tissue information [1]. However, the MR-sensitivity of the  $^{17}\text{O}$  nucleus ( $I = 5/2$ ) is poor because of the low gyromagnetic ratio ( $\gamma_{^{17}\text{O}} = \gamma_{^1\text{H}}/7.4$ ) and the fast relaxation due to the quadrupolar coupling. Information on the relaxation parameters of the imaging object is therefore crucial for optimizing the imaging sequence in terms of signal-to-noise ratio (SNR) and the determination of *in vivo*  $\text{H}_2^{17}\text{O}$  concentrations [2]. As the optimal SNR per unit acquisition time is proportional to  $(T_2^*/T_1)^{1/2}$ , both relaxation parameters,  $T_1$  and  $T_2^*$ , are affecting the SNR. In this study we measured the *in vivo*  $^{17}\text{O}$  relaxation times in the human brain at  $B_0 = 7\text{ T}$  to optimize imaging protocols for  $\text{CMRO}_2$  (cerebral metabolic rate of oxygen consumption) measurements. Non-localized detection ( $T_1$ ,  $T_2$ ) was carried out in 10 healthy volunteers and 3D  $T_2^*$  determination and anatomical mapping to  $^1\text{H}$  images was performed in one subject.

## MATERIAL & METHODS

Measurements were carried out on a 7 Tesla whole-body MR-system (Magnetom 7T, Siemens, Erlangen, Germany). Direct  $^{17}\text{O}$ -MRI of the natural abundance  $^{17}\text{O}$  concentration in the human head was performed using a custom-built quadrature  $^{17}\text{O}$  Tx/Rx head coil. Anatomical  $^1\text{H}$  data was acquired in a separate measurement using a 24-channel Tx/Rx head coil (Nova Medical, Inc., Wilmington, USA) and a spoiled gradient echo sequence. A 3D radial ultrashort echo time sequence with adapted k-space sampling density was applied for  $^{17}\text{O}$  imaging [3].

**$T_2^*$ -mapping:** Data sets of 9 different echo times (0.65 ms – 8.00 ms) with a nominal spatial resolution of  $(6\text{ mm})^3$  were acquired in a total acquisition time of 67:30 min ( $\text{TR} = 18\text{ ms}$ , readout time = 5.6 ms, pulse duration = 1 ms, projections = 25k, averages = 1). A flip angle of  $\alpha = 65^\circ$  was used to meet SAR requirements. A mono-exponential decay function was fitted to the data.

**Non-localized meas.:** Non-localized spin-echo and inversion recovery sequences were applied to determine global  $T_1$  and  $T_2$  values, respectively.

**$^{17}\text{O}$ -imaging:** An SNR optimized *in vivo* imaging protocol was prepared from the relaxometry results and  $^{17}\text{O}$  imaging of the human head was carried out. Natural abundance  $^{17}\text{O}$  images with an isotropic nominal spatial resolution of  $(5.5\text{ mm})^3$  were acquired in  $T_{\text{AQ}} = 9:54\text{ min}$  ( $\text{TR} = 11\text{ ms}$ ,  $\text{TE} = 0.7\text{ ms}$ , readout time = 5.04 ms,  $\alpha = 64^\circ$ , pulse duration = 1.2 ms, projections = 27k, averages = 2).

## RESULTS AND DISCUSSION

$T_2^*$  relaxation time maps of a central transversal and sagittal slice are displayed in Fig. 1. Image co-registration of anatomical  $^1\text{H}$  and  $^{17}\text{O}$  imaging data was applied for separating brain regions in the  $T_2^*$  analysis (Fig. 2). A region of interest analysis of the  $^{17}\text{O}$   $T_2^*$  maps showed: Gray/white matter  $T_2^* = 2.02 \pm 0.17\text{ ms}$ , CSF  $T_2^* = 3.12 \pm 0.20\text{ ms}$ , eyes  $T_2^* = 3.68 \pm 0.15\text{ ms}$  and cerebellum  $T_2^* = 1.91 \pm 0.24\text{ ms}$ .

Additionally, averaged non-localized relaxation times of  $T_1 = 5.77 \pm 0.14\text{ ms}$  and  $T_2 = 2.71 \pm 0.14\text{ ms}$  were found ( $n = 10$ ). The average brain matter value of  $T_2^* = 2.02\text{ ms}$  was used to determine an optimum-SNR readout duration of  $T_{\text{RO}} = 5.02\text{ ms}$  when applying a Hamming filter to the images [4]. Natural abundance *in vivo*  $^{17}\text{O}$  images acquired with an optimized protocol are shown in Fig. 3. An average SNR = 30 was determined for white/gray matter, SNR = 38 was found in fluid filled spaces (CSF, eyes).

## CONCLUSION

In this study we investigated the *in vivo* relaxation parameters of  $^{17}\text{O}$  in the human head at  $B_0 = 7\text{ T}$ . Optimum imaging parameters were determined from the data and applied in an SNR optimized  $^{17}\text{O}$ -MR imaging protocol for  $\text{CMRO}_2$  studies.

## REFERENCES

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- [3] Nagel, et al., Magn Reson Med, 2009; 62(6):1565-1573.
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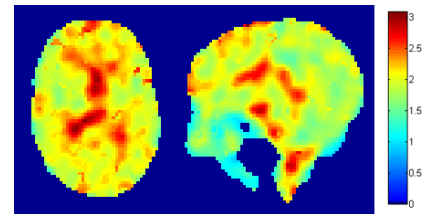


Fig.1: 3D mapping of the  $^{17}\text{O}$   $T_2^*$  [ms] relaxation times in the human brain acquired at  $B_0 = 7\text{ T}$ . A representative transversal and sagittal slice are shown.

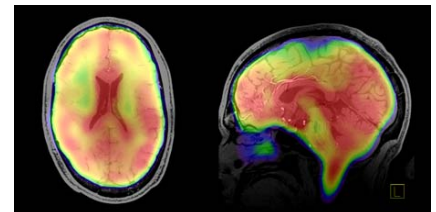


Fig.2: Image co-registration of nat. ab.  $^{17}\text{O}$  data (color) to  $^1\text{H}$  images (grayscale) for delineation of anatomical structures.

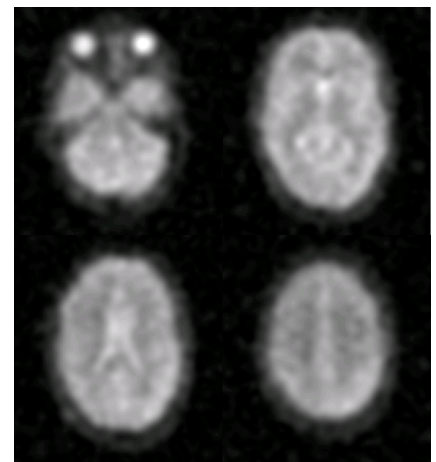


Fig.3: Natural abundance  $^{17}\text{O}$  images of the human head with an isotropic spatial resolution of  $(5.5\text{ mm})^3$  and  $\text{SNR}_{\text{mean}} = 32$ .