

# Potential of Relaxation-Weighted $^{23}\text{Na}$ -MRI for Brain Tumor Characterization

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## Introduction

In brain tumors, the average  $^{23}\text{Na}$ -concentration is typically increased due to edema and sustained cell depolarization, a precursor of cell division [1]. It was already shown that relaxation-weighted  $^{23}\text{Na}$ -MRI can be used to separate tumor compartments [2]. In this work it was evaluated whether relaxation-weighted  $^{23}\text{Na}$ -MRI can provide additional information for tumor grading. Therefore, 16 patients suffering from different brain tumors (14 WHO grade I – IV and 2 metastases) were examined at 7 Tesla with  $^{23}\text{Na}$ -MRI with different relaxation weightings.

## Methods

$^{23}\text{Na}$  images were acquired on a 7 T whole body system (Magnetom 7 T, Siemens Healthcare Solutions, Erlangen, Germany) using a double-resonant ( $^1\text{H}$ : 297.2 MHz;  $^{23}\text{Na}$ : 78.6 MHz) quadrature birdcage coil (Rapid Biomed GmbH, Rimpar, Germany). Anatomical images, including  $T_1$  weighted ( $T_{1w}$ ) images before and upon contrast media administration, were acquired in the clinical routine workup using a 3 Tesla MR system (Magnetom Tim Trio, Siemens Healthcare, Erlangen, Germany).

$^{23}\text{NaT}_N$ : Acquisition of the total sodium concentration with minimized relaxation-weighting ( $\text{TE}/\text{TR} = 0.3/120$  ms;  $\alpha = 90^\circ$ , readout length:  $T_{\text{RO}} = 10$  ms; nominal spatial resolution = (4 mm)<sup>3</sup>; acquisition time:  $T_{\text{AQ}} = 10$  min).

$^{23}\text{NaT}_H$ : To achieve a higher spatial resolution of (2.5 mm)<sup>3</sup> while maintaining an acceptable image acquisition time, TR was shortened resulting in minor  $T_1$  -weighting ( $\text{TE}/\text{TR}/T_{\text{RO}} = 0.5/25/20$  ms;  $\alpha = 55^\circ$ ;  $T_{\text{AQ}} = 13$  min 20 s).

$^{23}\text{NaR}_R$ : An inversion recovery (IR) preparation was applied to exploit  $T_1$ -differences of  $^{23}\text{Na}$  ions. Signal arising from  $^{23}\text{Na}$  compartments with longitudinal relaxation times like in CSF ( $T_1 = 64$  ms) was suppressed by using an inversion time of  $\text{TI} = 41$  ms ( $\text{TE}/\text{TR}/T_{\text{RO}} = 0.6/0.8/185/10$  ms; (5.5 mm)<sup>3</sup>;  $T_{\text{AQ}} = 10$  min).

$^{23}\text{NaR}_{\text{SUB}}$ : A fast ( $T_{\text{AQ}} = 2$  min 30 s)  $^{23}\text{Na}$  multi-echo sequence was applied to exploit differences in  $T_2^*$ -relaxation times ( $\text{TR}/T_{\text{RO}} = 30/10$  ms;  $\alpha = 68^\circ$ ; (5 mm)<sup>3</sup>). Images with echo times  $\text{TE}_A = 0.6$  ms and  $\text{TE}_B = 13$  ms were subtracted using a weighted difference. The weighting factor  $e^{+(T_{E_B}-T_{E_A})/T_2^*(\text{CSF})}$  was chosen such that  $T_2^*$ -times like in CSF ( $T_2^*(\text{CSF}) = 56$  ms) were fully suppressed. All  $^{23}\text{Na}$ -MRI measurements used a density-adapted 3D radial projection pulse sequence [3].

To keep the total exam time short, not all sequences were applied for each individual patient ( $^{23}\text{NaT}_N$ ,  $^{23}\text{NaT}_H$ ,  $^{23}\text{NaT}_{\text{IR}}$ , and  $^{23}\text{NaT}_{\text{SUB}}$  imaging were applied to 12, 6, 14, and 10 out 16 patients, respectively). Results from  $^{23}\text{Na}$  imaging were correlated with the Mib-1 proliferation rate of tumor cells. For comparability, signal of tumor, edema and CSF ( $^{23}\text{NaX}_Y$ ) normalized to healthy brain tissue ( $^{23}\text{NaX}_{\text{healthy}}$ ) was calculated according to following equation:  $^{23}\text{NaX}_Y [\%] = (^{23}\text{NaX}_Y - ^{23}\text{NaX}_{\text{healthy}}) / ^{23}\text{NaX}_{\text{healthy}}$

## Results

In 15 out of 16 patients  $^{23}\text{NaT}$  imaging revealed elevated total  $^{23}\text{Na}$  signals of tumor tissue, whereas an increased relaxation-weighted  $^{23}\text{Na}$  tumor signal was found in five out of 16 patients (Fig. 1a). Perifocal edema (present in six patients) exhibited hyperintense signals in  $^{23}\text{NaT}$  imaging and hypointense signals in  $^{23}\text{NaR}$  imaging (Fig. 1b). The pattern of signal changes in  $^{23}\text{NaT}$  and  $^{23}\text{NaR}$  was consistent for all WHO grade I – III brain tumors with elevated  $^{23}\text{NaT}$  and decreased  $^{23}\text{NaR}$  signals of tumor tissue. In all five glioblastomas the  $^{23}\text{NaR}$  signal was higher than the maximal  $^{23}\text{NaR}$  signal of WHO grade I – III tumors (Fig. 1a). Exemplarily images of a glioblastoma are shown in Fig. 2. Regression analysis revealed a positive correlation between normalized  $^{23}\text{NaR}$  signal of tumors and Mib-1 proliferation rate ( $R^2 = 0.74$ ,  $p_{\text{corr}} < 0.00$ ) (Fig. 3a), whereas no correlation was found between  $^{23}\text{NaT}$  signal and Mib-1 proliferation rate (Fig. 3b). Also, no correlations were found between normalized  $^{23}\text{Na}$  signal and other histopathological markers such as mitotic activity, cell density and vascularization.

## Discussion

An increased signal in both  $^{23}\text{NaT}$  and  $^{23}\text{NaR}$  imaging suggests tissue with an elevated concentration of sodium ions with short relaxation times. This signal increase might be due to an increase of the intracellular  $^{23}\text{Na}$  concentration indicating a breakdown of the  $\text{Na}^+/\text{K}^+$ -ATPase and / or the  $\text{Na}^+$  co-transporter, e.g. in tumors with high proliferation rates as indicated by the positive correlation of  $^{23}\text{NaR}$  signal and Mib-1 proliferation rate (Fig. 3a). Results from published animal studies also suggest an intracellular weighting of the  $^{23}\text{NaR}_{\text{IR}}$  signal [4]. An elevated signal in  $^{23}\text{NaT}$  imaging along with a decreased signal in  $^{23}\text{NaR}$  imaging might be compatible with an increased extracellular volume fraction (e.g. due to edema, c.f. Fig. 1b). It should be noted, that a pathologically altered density of the intra- or extracellular matrix might evoke changes in  $^{23}\text{NaR}$  signal intensities as well. Although this study is not suited for describing the physiological processes behind the  $^{23}\text{NaR}$  signal, our results allowed for a correct separation of all gliomas into WHO grade I – III and WHO grade IV tumors. This indicates that  $^{23}\text{NaR}$  imaging reveals valuable physiological tissue characteristics different from  $^{23}\text{NaT}$  imaging and might provide significant information for a functional *in vivo* tissue characterization.

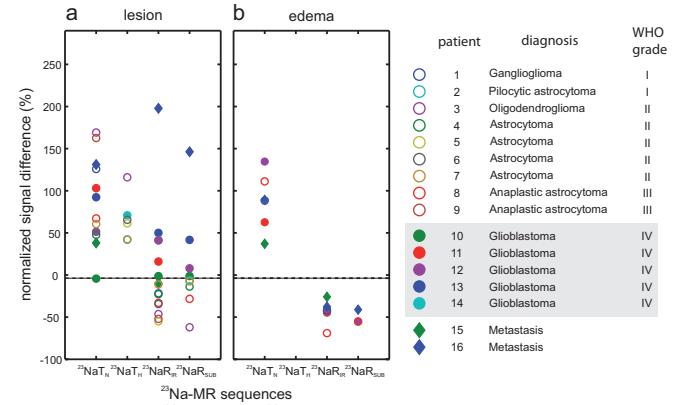


Fig. 1. Relative  $^{23}\text{NaT}$  and  $^{23}\text{NaR}$  signal intensities of the lesion (a) and perifocal edema (b). All glioblastomas exhibited  $^{23}\text{NaR}$  signals higher than the WHO grade I – III tumors (a). Perifocal edema (b) showed hyperintense signals in  $^{23}\text{NaT}$  and hypointense signals in  $^{23}\text{NaR}$  imaging.

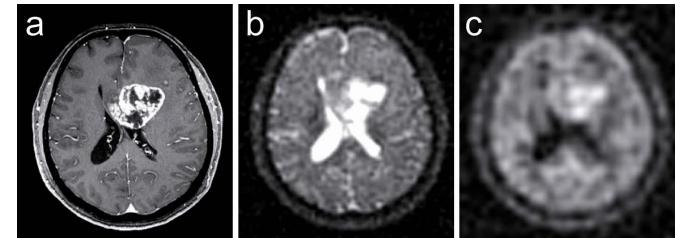


Fig. 2. Glioblastoma (WHO grade IV). (a)  $T_{1w}$  imaging revealed rim enhancement upon contrast media administration. (b)  $^{23}\text{NaT}_H$  imaging demonstrated an increased signal of tumor tissue. (c)  $^{23}\text{NaR}_{\text{IR}}$  imaging yielded elevated signals mainly of the central tumor portion.

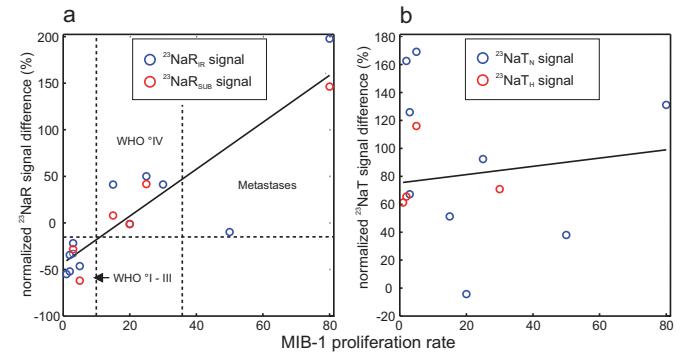


Fig. 3. Linear regression analysis demonstrated a positive association between  $^{23}\text{NaR}$  signal and Mib-1 proliferation rate (a). There was no association between  $^{23}\text{NaT}$  signal and Mib-1 proliferation rate (b).

## References

- Boada FE, et al. Curr Top Dev Biol (2005) 70: p. 77.
- Nagel AM, et al. In Proc. ISMRM 2010, p. 727.
- Nagel AM, et al. Magn Reson Med (2009) 62: p. 1565.
- Kline RP, et al. Clin Cancer Res (2000) 6: p. 2146.

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