

Potential of Relaxation-Weighted ^{23}Na -MRI for Brain Tumor Characterization

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Introduction

In brain tumors, the average ^{23}Na -concentration is typically increased due to edema and sustained cell depolarization, a precursor of cell division [1]. It was already shown that relaxation-weighted ^{23}Na -MRI can be used to separate tumor compartments [2]. In this work it was evaluated whether relaxation-weighted ^{23}Na -MRI can provide additional information for tumor grading. Therefore, 16 patients suffering from different brain tumors (14 WHO grade I–IV and 2 metastases) were examined at 7 Tesla with ^{23}Na -MRI with different relaxation weightings.

Methods

^{23}Na images were acquired on a 7 T whole body system (Magnetom 7 T, Siemens Healthcare Solutions, Erlangen, Germany) using a double-resonant (^1H : 297.2 MHz; ^{23}Na : 78.6 MHz) quadrature birdcage coil (Rapid Biomed GmbH, Rimpf, Germany). Anatomical images, including T₁ weighted (T1w) images before and upon contrast media administration, were acquired in the clinical routine workup using a 3 Tesla MR system (Magnetom Tim Trio, Siemens Healthcare, Erlangen, Germany).

$^{23}\text{NaT}_N$: Acquisition of the total sodium concentration with minimized relaxation-weighting (TE/ TR= 0.3/ 120 ms; α = 90°, readout length: T_{RO} = 10 ms; nominal spatial resolution = (4 mm)³; acquisition time: T_{AQ} = 10 min).

$^{23}\text{NaT}_H$: To achieve a higher spatial resolution of (2.5 mm)³ while maintaining an acceptable image acquisition time, TR was shortened resulting in minor T₁-weighting (TE/ TR/ T_{RO} = 0.5/ 25/ 20 ms; α = 55°; T_{AQ} = 13 min 20 s).

$^{23}\text{NaR}_{IR}$: An inversion recovery (IR) preparation was applied to exploit T₁-differences of ^{23}Na ions. Signal arising from ^{23}Na compartments with longitudinal relaxation times like in CSF (T₁ = 64 ms) was suppressed by using an inversion time of TI = 41 ms (TE/ TR/ T_{RO} = 0.6–0.8/ 185/ 10 ms; (5.5 mm)³, T_{AQ} = 10 min).

$^{23}\text{NaR}_{SUB}$: A fast (T_{AQ} = 2 min 30s) ^{23}Na multi-echo sequence was applied to exploit differences in T₂^{*}-relaxation times (TR/ T_{RO} = 30/ 10 ms; α = 68°; (5 mm)³. Images with echo times TE_A = 0.6 ms and TE_B = 13 ms were subtracted using a weighted difference. The weighting factor $e^{-(TE_B - TE_A)/T_2^{*,CSF}}$ was chosen such that T₂^{*}-times like in CSF (T₂^{*} (CSF) = 56 ms) were fully suppressed. All ^{23}Na -MRI measurements used a density-adapted 3D radial projection pulse sequence [3].

To keep the total exam time short, not all sequences were applied for each individual patient ($^{23}\text{NaT}_N$, $^{23}\text{NaT}_H$, $^{23}\text{NaT}_{IR}$, and $^{23}\text{NaT}_{SUB}$ imaging were applied to 12, 6, 14, and 10 out of 16 patients, respectively). Results from ^{23}Na imaging were correlated with the Mib-1 proliferation rate of tumor cells. For comparability, signal of tumor, edema and CSF ($^{23}\text{NaX}_Y$) normalized to healthy brain tissue ($^{23}\text{NaX}_{healthy}$) was calculated according to following equation: $^{23}\text{NaX}_Y [\%] = (^{23}\text{NaX}_Y - ^{23}\text{NaX}_{healthy}) / ^{23}\text{NaX}_{healthy}$

Results

In 15 out of 16 patients ^{23}NaT imaging revealed elevated total ^{23}Na signals of tumor tissue, whereas an increased relaxation-weighted ^{23}Na tumor signal was found in five out of 16 patients (Fig. 1a). Perifocal edema (present in six patients) exhibited hyperintense signals in ^{23}NaT imaging and hypointense signals in ^{23}NaR imaging (Fig. 1b). The pattern of signal changes in ^{23}NaT and ^{23}NaR was consistent for all WHO grade I–III brain tumors with elevated ^{23}NaT and decreased ^{23}NaR signals of tumor tissue. In all five glioblastomas the ^{23}NaR signal was higher than the maximal ^{23}NaR signal of WHO grade I–III tumors (Fig. 1a). Exemplarily images of a glioblastoma are shown in Fig. 2. Regression analysis revealed a positive correlation between normalized ^{23}NaR signal of tumors and Mib-1 proliferation rate ($R^2 = 0.74$, $p_{corr} < 0.00$) (Fig. 3a), whereas no correlation was found between ^{23}NaT signal and Mib-1 proliferation rate (Fig. 3b). Also, no correlations were found between normalized ^{23}Na signal and other histopathological markers such as mitotic activity, cell density and vascularization.

Discussion

An increased signal in both ^{23}NaT and ^{23}NaR imaging suggests tissue with an elevated concentration of sodium ions with short relaxation times. This signal increase might be due to an increase of the intracellular ^{23}Na concentration indicating a breakdown of the Na⁺ / K⁺ - ATPase and / or the Na⁺ co-transporter, e.g. in tumors with high proliferation rates as indicated by the positive correlation of ^{23}NaR signal and Mib-1 proliferation rate (Fig. 3a). Results from published animal studies also suggest an intracellular weighting of the $^{23}\text{NaR}_{IR}$ signal [4]. An elevated signal in ^{23}NaT imaging along with a decreased signal in ^{23}NaR imaging might be compatible with an increased extracellular volume fraction (e.g. due to edema, c.f. Fig. 1b). It should be noted, that a pathologically altered density of the intra- or extracellular matrix might evoke changes in ^{23}Na signal intensities as well. Although this study is not suited for describing the physiological processes behind the ^{23}NaR signal, our results allowed for a correct separation of all gliomas into WHO grade I–III and WHO grade IV tumors. This indicates that ^{23}NaR imaging reveals valuable physiological tissue characteristics different from ^{23}NaT imaging and might provide significant information for a functional *in vivo* tissue characterization.

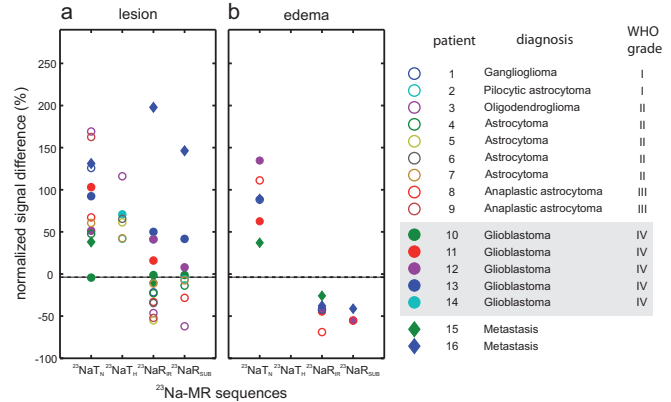


Fig. 1. Relative ^{23}NaT and ^{23}NaR signal intensities of the lesion (a) and perifocal edema (b). All glioblastomas exhibited ^{23}NaR signals higher than the WHO grade I–III tumors (a). Perifocal edema (b) showed hyperintense signals in ^{23}NaT and hypointense signals in ^{23}NaR imaging.

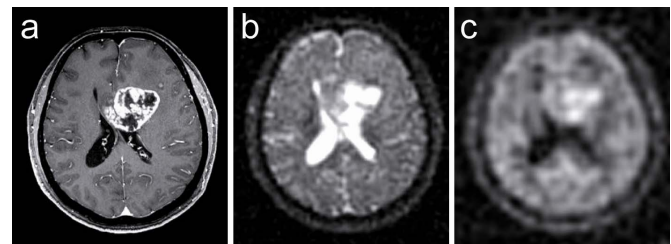


Fig. 2. Glioblastoma (WHO grade IV). (a) T1w imaging revealed rim enhancement upon contrast media administration. (b) $^{23}\text{NaT}_H$ imaging demonstrated an increased signal of tumor tissue. (c) $^{23}\text{NaR}_{IR}$ imaging yielded elevated signals mainly of the central tumor portion.

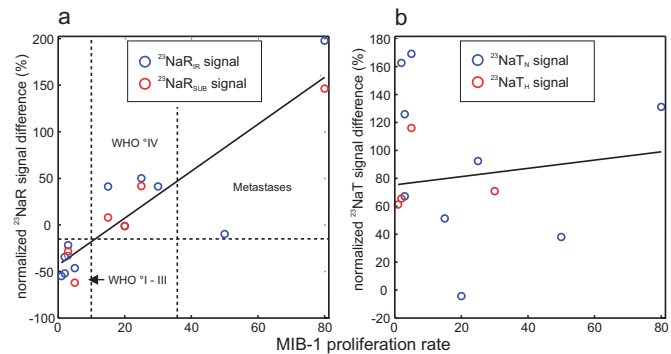


Fig. 3. Linear regression analysis demonstrated a positive association between ^{23}NaR signal and Mib-1 proliferation rate (a). There was no association between ^{23}NaT signal and Mib-1 proliferation rate (b).

References

- Boada FE, et al. Curr Top Dev Biol (2005) 70: p. 77.
- Nagel AM, et al. In Proc. ISMRM 2010, p. 727.
- Nagel AM, et al. Magn Reson Med (2009) 62: p. 1565.
- Kline RP, et al. Clin Cancer Res (2000) 6: p. 2146.

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