

# In vitro and In vivo Studies of <sup>17</sup>O NMR Sensitivity at 9.4 and 16.4 Tesla

M. Lu<sup>1,2</sup>, X. Wang<sup>1,2</sup>, R. Taylor<sup>1,2</sup>, Y. Zhang<sup>1,2</sup>, K. Ugurbil<sup>1,2</sup>, W. Chen<sup>1,2</sup>, and X-H. Zhu<sup>1,2</sup>

<sup>1</sup>Center for Magnetic Resonance Research, University of Minnesota Medical School, Minneapolis, Minnesota, United States, <sup>2</sup>Department of Radiology, University of Minnesota Medical School, Minneapolis, Minnesota, United States

## Introduction

The lack of non-destructive and robust *in vivo* imaging approaches for investigating cellular oxidative metabolism has limited our understanding of the mechanism underlying metabolic alteration between normal and diseased tissues. Direct observing the dynamics of metabolic H<sub>2</sub><sup>17</sup>O production from the reduction of <sup>17</sup>O-labeled oxygen gas provides an opportunity to quantify and image the cerebral rate of oxygen consumption (CMRO<sub>2</sub>) *in vivo*. However, the efforts of direct monitoring the accumulation rate of H<sub>2</sub><sup>17</sup>O have been suffered from the low NMR detection sensitivity due to the very low gyromagnetic ratio of the <sup>17</sup>O spin and low H<sub>2</sub><sup>17</sup>O content. It is known that the optimal signal-to-noise ratio (SNR) for detecting NMR signals depends on field strength (B<sub>0</sub>), T<sub>1</sub>, T<sub>2</sub>\* and the RF coil quality factor (Q) according to the following relationship:

$$SNR \propto B_0^\beta \sqrt{\frac{QT_2^*}{T_1}}$$

Two previous studies have compared the *in vitro* and *in vivo* <sup>17</sup>O NMR sensitivity between 4.7T and 9.4T, and between 4.7T and 11T, respectively (1,2), suggesting great advantages of high field. The unique properties of <sup>17</sup>O, i.e., the independence of <sup>17</sup>O relaxation times (T<sub>1</sub> and T<sub>2</sub>) on the field strength (1,2) and extremely short T<sub>1</sub>, also contribute to a large gain of <sup>17</sup>O NMR sensitivity at high/ultrahigh field. In this study, <sup>17</sup>O NMR sensitivity was measured and compared using the natural abundance H<sub>2</sub><sup>17</sup>O signal in phantom solution and rat brain at 9.4T and 16.4T to quantify the possible SNR gain for *in vivo* <sup>17</sup>O NMR application using the newly developed large-bore animal scanner with ultrahigh (highest) field of 16.4T.

## Methods

All NMR measurements were performed on either a 9.4T/31cm or a 16.4T/26cm bore magnet (MagneX Scientific) interfaced to VNMRJ consoles (Varian, CA). For both *in vitro* and *in vivo* studies, a <sup>17</sup>O radiofrequency (RF) probe consisting of a two-turn, oval (18mm×13mm) shaped surface-coil was designed and constructed. Its resonance frequency can be tuned to either 54.25 MHz for 9.4T or 94.65 MHz for 16.4T application. A 6mm-diameter glass sphere filled with natural abundance <sup>17</sup>O water was fixed on the RF probe for all phantom studies at both fields. A male Sprague Dawley rat was anesthetized and imaged for measuring and quantifying SNR of natural abundance brain H<sub>2</sub><sup>17</sup>O at 9.4T and 16.4T using the same surface-coil, which was placed over the cortical regions in the rat brain to obtain optimum *in vivo* sensitivity. The single-pulse-acquire sequence was applied to obtain the optimal <sup>17</sup>O SNR with a nominal 90° RF excitation pulse and following acquisition parameters: 20 kHz spectral width, 512 number of points for each FID, 7 s temporal resolution with 128 signal averages for phantom measurements and 512 (28 s temporal resolution) or 128 averages for *in vivo* studies. The raw NMR signal was processed by exponential filtering with a line broadening of 100 Hz to enhance SNR, followed by Fourier transformation. The <sup>17</sup>O NMR sensitivity was evaluated using the SNR of H<sub>2</sub><sup>17</sup>O resonance peak calculated by dividing peak intensity by the standard deviation of the noise. Another relevant question is whether the <sup>17</sup>O signal is stable among repeated measurements; thus, the stability of the <sup>17</sup>O signal was also assessed by computing the standard deviation of H<sub>2</sub><sup>17</sup>O signals from 10 repetitions of data acquisition.

## Results

Figure 1 shows typical <sup>17</sup>O NMR spectra of natural abundance H<sub>2</sub><sup>17</sup>O acquired from the sphere phantom and *in vivo* rat brain at two field strengths with the same vertical display scale. The average <sup>17</sup>O SNR gain at 16.4T was 2.9 and 2.6-fold higher than that at 9.4T, for the phantom and rat brain studies, respectively, as summarized in Table 1. The <sup>17</sup>O signal stabilities at both field strengths are also shown in Table 1. The overall results clearly demonstrate excellent sensitivity and high stability at both fields for obtaining the <sup>17</sup>O signals of natural abundance H<sub>2</sub><sup>17</sup>O (lowest concentration in nature) from either phantom or brain. Nevertheless, the 16.4T scanner offers striking improvements in both sensitivity and reproducibility.

## Discussion and Conclusion

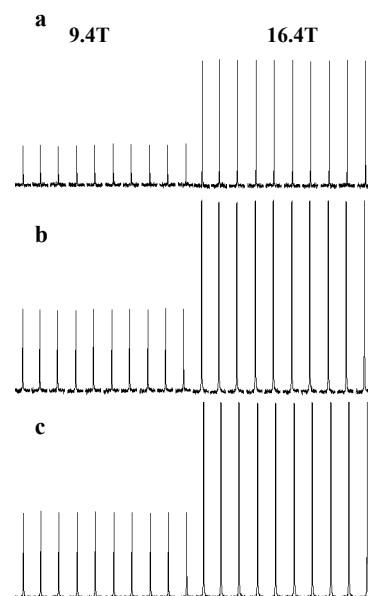
In the present study, we examined the *in vitro* and *in vivo* <sup>17</sup>O NMR sensitivity at two high field strengths. The results indicate an approximated 2.6–3-fold SNR gain at 16.4T compared with 9.4T. Also, an approximated square power (β=1.7~2) dependence of <sup>17</sup>O SNR on B<sub>0</sub> was indicated, and this value is consistent with previous reports (1,2) and the theoretical prediction of 7/4. The significant SNR improvements achieved at 16.4T should benefit 3D CMRO<sub>2</sub> imaging based on the <sup>17</sup>O MRS method, which should provide an opportunity to detect altered oxidative metabolism associated with brain function and neurological diseases with improved spatial and temporal resolutions.

## Acknowledgements

This work is supported in part by NIH grants NS41262, NS57560, P41 RR08079 and P30 NS057091, S10 RR025031; and the Keck foundation.

## References

1. Zhu, X. H., Merkle, H., Kwag, J. H., Ugurbil, K., and Chen, W. (2001) *Mag. Reson. Med.* **45**, 543-549.
2. Thelwall, P. E., Blackband, S. J., Chen, W. (2003) *Proc. Intl. Soc. Mag. Reson. Med.* p. 504.



**Figure 1.** <sup>17</sup>O spectra of the sphere (a) and *in vivo* rat brain (b) with 128 averages. *In vivo* rat brain <sup>17</sup>O spectra with 512 averages (c).

**Table 1.** <sup>17</sup>O SNR and signal stability comparisons between 9.4T and 16.4T

	Sphere (128 averages)	Rat Brain (128 averages)	Rat Brain (512 averages)
SNR <sub>9.4T</sub>	36.8± 3.5	69.9± 5.8	142.4± 15.8
SNR <sub>16.4T</sub>	108.4± 11.3	178.6± 8.1	349.6± 46.8
SNR <sub>16.4T</sub> /SNR <sub>9.4T</sub>	2.9	2.6	2.5
Stability at 9.4T	2.19%	0.84%	0.66%
Stability at 16.4T	0.53%	0.43%	0.27%