

# Simultaneous $^{23}\text{Na}/^1\text{H}$ Imaging with Dual Excitation and Double Tuned Birdcage Coil

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## Introduction

The tissue concentration of sodium is sensitive to disease as an indicator of cellular and metabolic integrity [1]. Due to the low  $^{23}\text{Na}$  MR signal level, however, relatively long scan times are required. Furthermore, an additional  $^1\text{H}$  image is needed for an anatomic co-registration. In this context, a truly simultaneous acquisition of the  $^{23}\text{Na}$  and  $^1\text{H}$  signal would be helpful to reduce the scan duration and avoid misregistration between the sodium and proton image. Furthermore, dual-tuned coils eliminate the need for retuning the coils, or replacing coils during examination, which would require some sort of mechanical fixation of the subject [1]. In this study, an MR sequence with dual Nuclei excitation and simultaneous sampling on the  $^{23}\text{Na}$  and  $^1\text{H}$  frequency was implemented, and a dual-tuned transmit/receive coil was used to enable simultaneous  $^{23}\text{Na}/^1\text{H}$  imaging. First *in vivo* examples were obtained in a human knee to demonstrate the basic feasibility of true simultaneous  $^1\text{H}/^{23}\text{Na}$  imaging.

## Methods

Sodium and proton images were acquired simultaneously on a clinical 3T scanner (Philips Healthcare, Best, The Netherlands) equipped with a modified acquisition software and a dual-tuned  $^{23}\text{Na}/^1\text{H}$  birdcage transmit/receive coil (Rapid Biomedical, Würzburg, Germany). A 3D Cartesian spoiled gradient echo sequence (FFE,  $\text{TR}/\text{TE}=8\text{ms}/2.25\text{ms}$ ,  $\alpha=15^\circ$ , matrix size  $256 \times 256$ , 10 slices, 24 averages, total scan time 11 minutes) was used, where a dual RF excitation and sampling on the  $^{23}\text{Na}$  and  $^1\text{H}$  frequencies was performed. A schematic plot of the employed MR sequence is shown in Fig. 1. Due to the simultaneous acquisition of two nuclei within a single readout, the individual FOV and resolution are scaled with the respective gyromagnetic ratios ( $\gamma_{^{23}\text{Na}} = 17.25 \text{ MHz/T}$ ,  $\gamma_{^1\text{H}} = 42.58 \text{ MHz/T}$ ). The resulting spatial resolution was  $0.8 \times 0.8 \times 10\text{mm}$  for the proton image, and  $2 \times 2 \times 10\text{mm}$  for the sodium image. First *in vivo* images of the knee were acquired in 3 healthy adults. Written informed consent was obtained from all participants. The images were re-scaled retrospectively to a uniform FOV using the known gyromagnetic ratios of  $^1\text{H}$  and  $^{23}\text{Na}$ .

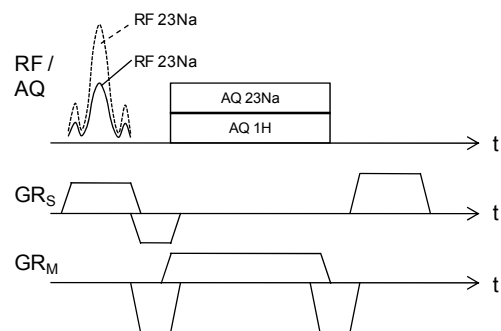
## Results and discussion

All experiments were completed successfully, and selected *in vivo* results, where  $^1\text{H}$  and  $^{23}\text{Na}$  images were simultaneously obtained, are shown in Fig. 2[a] and [b], respectively. A fusion image of the proton image and the color-coded  $^{23}\text{Na}$  image is shown in Fig. 2[c]. The elevated  $^{23}\text{Na}$  levels in cartilage were clearly visualized.

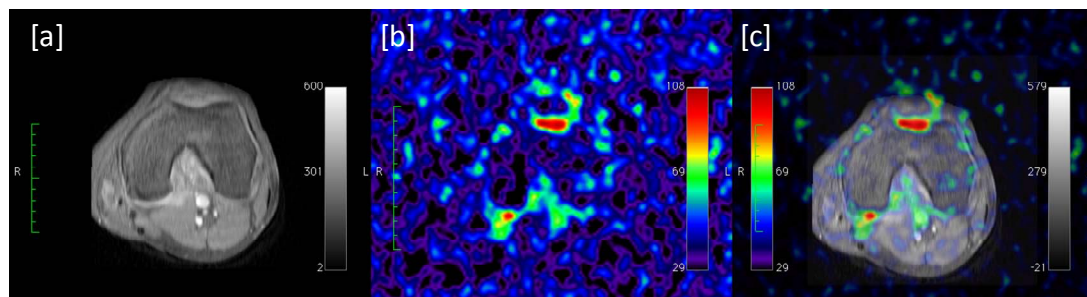
## Conclusion

So far, simultaneous dual-frequency sequences have been used for spectroscopy (proton decoupling), or Overhauser imaging, or recently for the simultaneous acquisition of  $^{19}\text{F}$  and  $^1\text{H}$  [2]. In this study, first

results for true simultaneous  $^1\text{H}/^{23}\text{Na}$  imaging using a dual-tuned coil are shown. The simultaneous technique overcomes the need for an additional  $^1\text{H}$  scan and eliminates the risk of misregistration of the sodium and proton image. The basic sequence implementation used in the present study offers a large potential for further optimization. Non-Cartesian FID sampling strategies should be employed to reduce the echo time (TE) and allow to assess fast decaying sodium components [3]. Furthermore, non-Cartesian sampling may be favorable with respect to potential backfolding artifacts in the proton image with inherently smaller FOV. Alternatively, multi-element  $^1\text{H}$  coils in concert with parallel imaging could be employed to unfold the proton image.



**Fig. 1** Schematic plot of simultaneous  $^1\text{H}/^{23}\text{Na}$  sequence. The RF pulses are played simultaneously on the respective resonance frequencies. Sampling is performed simultaneously on separate receive channels.



**Fig. 2** Simultaneously acquired proton image [a], color-coded  $^{23}\text{Na}$  image [b], and overlay of anatomy and  $^{23}\text{Na}$  level [c]. The elevated  $^{23}\text{Na}$  level in cartilage is clearly visualized in the overlay image.

## References:

- [1] Ouwerkerk R et al, Radiology 2003; 227(2):529-37
- [2] Keupp J et al, Proc ISMRM 14, p. 102 (2006)
- [3] Rahmer J et al, Magn Reson Med. 2006; 55(5):1075-82