

# Accelerated Mapping of T1 Relaxation Times using TAPIR

K. Möllenhoff<sup>1</sup>, N. J. Shah<sup>1,2</sup>, E. D. Pracht<sup>1</sup>, and T. Stöcker<sup>1</sup>

<sup>1</sup>Institute of Neuroscience and Medicine – 4, Medical Imaging Physics, Forschungszentrum Juelich GmbH, Juelich, Germany, <sup>2</sup>Faculty of Medicine, Department of Neurology, RWTH Aachen University, JARA, Aachen, Germany

## Introduction

Fast and accurate T<sub>1</sub> mapping of the human brain provides many opportunities for diagnostic use. For example, it has been shown that T<sub>1</sub> values differ in the globus pallidus, the caudate nucleus, and the posterior limb of the internal capsule of patients suffering from hepatic encephalopathy, a liver disease with neuropsychiatric consequences [1]. The TAPIR sequence [2-5] is a distortion free and accurate method to acquire high resolution T<sub>1</sub> maps with an in-plane resolution of 1mm but without any acceleration it is too slow for clinical use for whole brain coverage. It has been shown that the accuracy of T<sub>1</sub> measurements using a Look-Locker sequence can be increased through the use of an adiabatic fast passage (AFP) inversion pulse [6].

TAPIR is an extremely flexible Look-Locker sequence that allows choices to be made regarding coverage and number of time points acquired on the recovery curve. We have implemented and investigated a more accurate and faster version of the TAPIR sequence using adiabatic fast passage inversion pulses, parallel imaging and a segmented EPI readout which is an integral feature of TAPIR.

## Methods

All experiments were performed on a 3 Tesla Siemens Tim-Trio System using a body coil for transmission and a 12 channel head-array for reception of the signal (Siemens Medical, Erlangen, Germany). The inversion pulse is a hyperbolic secant and its amplitude and phase are modulated with  $amp = \text{sech}(\beta u)$  and  $phase = \mu \log(amp)$  with  $\beta = 4.5$  and  $\mu = 5$ . Further, parallel imaging was implemented with external acquisition of GRAPPA reference lines prior to the TAPIR sequence. GRAPPA reconstruction was performed using the standard software provided by the MR scanner. An inversion efficiency (IE) measurement, as needed when using rectangular inversion pulses, is not necessary when using the AFP pulse because it results in a very good inversion. [6]

The total acquisition time without acceleration for a T<sub>1</sub> map with volume coverage of 4 slices with a slice thickness of 4 mm is about 17 minutes (TR=12ms and 40 time points (TP), FA=25°, BW=720Hz/Px) and additional 4 minutes for an inversion efficiency measurement using an EPI factor of 5 (4 slices, TR=12ms, FA=25° BW=720Hz/Px). Using parallel imaging with an acceleration factor of 2 and an EPI-factor of 5 the total acquisition time can be reduced to 2 minutes. This results in an effective total acquisition time of 30 seconds per slice.

Increasing the number of slices to 7 and decreasing the number of time points to 25 results in nearly the same total acquisition time while the results do not suffer much from the lower number of time points [7]. This results in an effective total acquisition time of 17 seconds per slice.

The influence of adiabatic inversion as well as the acceleration of the acquisition (EPI and/or parallel imaging) was experimentally investigated. T<sub>1</sub> mapping was performed on a healthy volunteer and a so-called “revolver phantom” comprising 6 tubes filled with distilled water that was doped with different concentrations of GdCl<sub>3</sub>. For the phantom measurements, TAPIR results were compared to the gold standard spectroscopic inversion recovery measurements.

## In Vitro Results

As can be seen in Table 1, the T<sub>1</sub> values measured with an adiabatic fast passage inversion pulse are more accurate than the T<sub>1</sub> values measured with a rectangular inversion pulse. The parameters used were: single slice with a thickness of 4 mm, TR=12ms, 128 time points, BW=720Hz/Px, FA=25°.

SPECT T1 [ms]	T <sub>1</sub> using rect. inversion [ms]	T <sub>1</sub> using AFP [ms]	T <sub>1</sub> using AFP and EPI5 iPAT 2 [ms]
1349	1499 ± 87	1365 ± 55	1365 ± 59
838	828 ± 24	827 ± 16	824 ± 21
631	594 ± 12	601 ± 9	617 ± 13
490	489 ± 11	490 ± 7	493 ± 8
400	402 ± 9	405 ± 6	408 ± 7
339	329 ± 7	338 ± 4	340 ± 5

Table 1: Phantom results: spectroscopic T<sub>1</sub> measurements versus the different TAPIR results in six differently doped tubes

		Slice 1 T <sub>1</sub> [ms]	Slice 4 T <sub>1</sub> [ms]
rectangular	WM	824 ± 42	817 ± 41
	GM	1089 ± 113	1082 ± 117
AFP	WM	828 ± 37	815 ± 37
	GM	1095 ± 111	1081 ± 116
EPI5 iPAT2	WM	820 ± 34	815 ± 34
	GM	1093 ± 112	1083 ± 116

Table 2: In vivo results: T<sub>1</sub> values and the standard deviations of GM and WM of the human brain in different slices measured with the TAPIR sequence with a rectangular inversion pulse and an IE measurement compared with T<sub>1</sub> values measured with AFP and with accelerated methods in ms.

## In Vivo Results

The measured T<sub>1</sub> values for WM and GM of the human brain are listed in Table 2. In general, the segmented EPI readout and parallel imaging have little influence on the accuracy.

## Discussion and Conclusions

For a given set of parameters, it is possible to acquire high resolution T<sub>1</sub> maps with volume coverage of 4 slices in about 2 minutes instead of 21 minutes (17 minutes plus additional 4 minutes for the IE measurement) using an EPI readout and parallel imaging without a noticeable degradation of the T<sub>1</sub> results. We have demonstrated that the accuracy of the T<sub>1</sub> mapping procedure is increased when using an adiabatic fast passage inversion pulse instead of a rectangular pulse, even if we use an EPI factor of 5 and parallel imaging with an acceleration factor of 2. The standard deviations are between 1% and 5% which is in the same range as the ones for other methods described in the literature [6]. This technique offers the possibility to acquire accurate and distortion-free T<sub>1</sub> maps of the human brain in a short acquisition time.

## References

- [1] Shah et al., Hepatology. 2003 Nov;38(5):1219-26.; [2] Shah et al., German Patent Number: 10028171; [3] Shah et al., US Patent 6803762; [4] Steinhoff et al., Magn Reson Med. 2001 Jul;46(1):131-40.; [5] Shah et al., NeuroImage Vol. 14, Issue 5, Nov 2001, 1175-1185; [6] Deichmann et al., Magn Reson Med. 2005 Jul;54(1):20-27.; [7] Zaitsev et al., Magn Reson Med 2003 49:1121-1132;

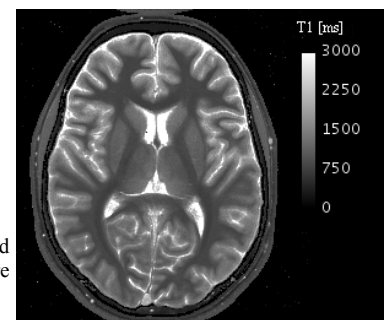


Figure 1: Representative T<sub>1</sub> map of a human brain in ms