

# CONTRAST AT ULTRA-HIGH FIELD: RELAXATION TIMES IN THE RAT BRAIN AT 16.4 T

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**Introduction:** Knowledge of the relaxation times is vital for adjusting sequence parameters for optimum SNR or contrast. For MR imaging at ultra-high fields, the relaxation times also play an important role in determining the advantage of the field strength, since the longer  $T_1$  and shorter  $T_2$  may partially compensate for the linear SNR gain in anatomical imaging, while causing additional gain in other applications, like perfusion or functional MRI. Here, we have performed highly accurate measurements of the relaxation times in the rat brain at a field strength of 16.4 T to predict SNR and contrast behavior at ultra-high field.

**Materials and Methods:** All experiments were performed with a 16.4 T magnet with a bore size of 26 cm, interfaced to a Bruker console. A quadrature surface coil with a homebuilt TR-switch and preamplifier was used for excitation and signal reception.  $T_1$ ,  $T_2$  and  $T_2^*$  were each measured in six rats with different ages under isoflurane anaesthesia. During the experiments, the animals were maintained at a constant temperature of 37°C controlled by a rectal sensor. Measurement techniques were selected for accuracy and insensitivity to  $B_1$  inhomogeneities caused by the transmit field of the surface coil. In all experiments, six 0.6 mm slices were scanned with a spatial resolution of 180  $\mu\text{m}^2$ . For the  $T_1$  measurements, an inversion-recovery sequence with a RARE readout was used. 17 images with different  $T_1$  between 400 ms and 8000 ms were acquired with a repetition time of 13 s.  $T_2$  was measured with a single spin echo sequence, using 11 echo times between 7.5 ms and 87 ms. To obtain  $T_2^*$  data, gradient echo images with 11 different echo times between 3 ms and 35 ms were acquired. The relaxation time values of different anatomical structures were calculated by positioning circular ROIs in the image, adding the signals from the selected voxels and fitting the exponential function corresponding to the relaxation time in question. For obtaining relaxation time maps, the SNR was boosted by applying a Hanning-filter to the raw data before reconstruction, thereby effectively decreasing the resolution by a factor of two, and then fitting the exponential function to every image point.

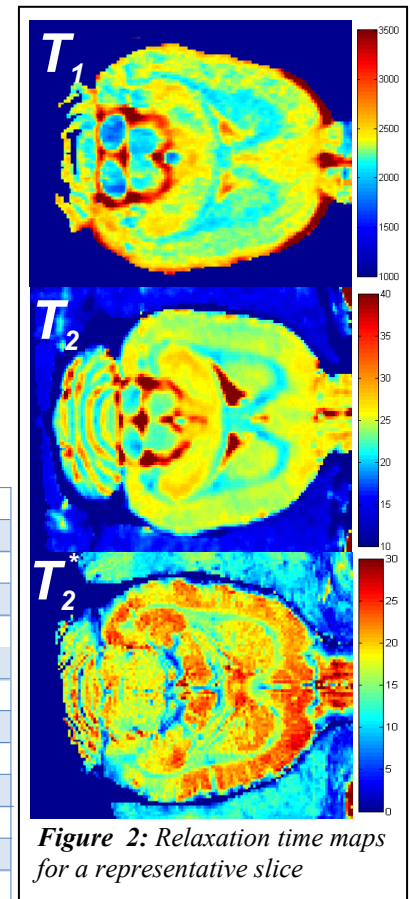
**Results:** Table 1 shows relaxation times of selected anatomical structures.  $T_1$  ranges from 1800 ms in the colliculus to above 2300 ms in cortical gray matter and hippocampus.  $T_2$  in the brain is between 20 ms (corpus callosum) and around 25 ms (cortex, hippocampus), while mean  $T_2^*$  values lie between 13 ms and 22 ms for the same structures, though the latter showing strong local variations. No differences were found between right and left hemispheres, while  $T_1$  showed a significant variation with age in almost all anatomical structures. The relaxation time maps, Fig. 1, allow clear distinction between the different structures.

	$T_1$	Stdev	$N_{ROIS}$	$T_2$	Stdev	$N_{ROIS}$	$T_2^*$	Stdev	$N_{ROIS}$
somatosensory cortex	2194.4	97.7	42	23.9	1.2	45	19.5	2.5	42
auditory cortex	2289.2	91.3	14	23.6	1.4	10	19.7	1.7	16
motor cortex	2313.9	77.9	12	25.1	1.1	10	20.6	4.1	14
caudate putamen	2193.7	88.5	48	24.0	1.2	44	19.8	2.0	55
corpus callosum	2072.6	97.1	22	19.6	1.2	24	13.6	1.5	29
thalamus	2141.4	144.6	32	23.5	1.6	34	20.0	2.1	40
hippocampus	2330.5	97.1	24	25.1	1.7	20	20.2	3.0	32
dentate gyrus	2370.8	71.0	48	25.9	1.3	40	17.6	3.2	40
colliculus	1840.4	74.1	22	20.7	1.2	23	14.8	2.2	28
cerebellum	2120.5	120.9	24	24.0	1.5	26	17.4	1.8	25
accumbens nucleus	2306.3	64.5	12	24.8	0.8	10	22.0	1.8	14
septal nucleus	2288.6	76.3	19	25.9	0.6	16	22.0	2.4	21
bulb	2311.7	84.3	40	25.8	1.2	28	21.4	2.4	24
muscle	2442.7	181.5	15	15.3	1.3	12	13.4	1.5	31

**Table 1:** Values (in ms) of the relaxation times for selected anatomical structures, with standard deviations and total number of ROIs used to obtain the values.

## Conclusion:

The relaxation times in the rat brain were measured with high accuracy. As expected from measurements at lower fields,  $T_1$  continues to increase with field strength, while  $T_2$  and  $T_2^*$  get lower. Both factors limit the growth in SNR with increasing field strength for many applications.



**Figure 2:** Relaxation time maps for a representative slice