

# Efficiency of Single-loop and Quadrature Surface RF Coils in the Human Brain at 9.4 Tesla

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## Introduction

NMR spectroscopy, especially in a single-voxel, is commonly performed with surface coils such as single-loop and “quadrature” coils since only a limited field of view is required and higher signal-to-noise ratio is achievable in comparison to single channel volume coils. However at high magnetic field transmit and receive  $B_1$  profiles are significantly distorted as demonstrated previously at 7 T [1]. Here we investigate the impact of these  $B_1$  field distortions in the human brain at 9.4 T when using single-loop and quadrature RF coils.

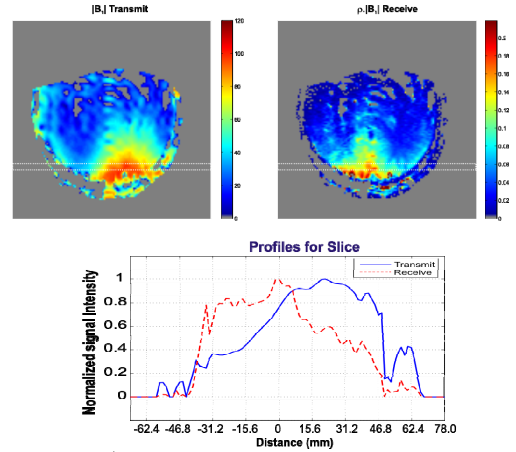
## Methods

Home-built single-loop (10cm in diameter) and quadrature (two overlapping loops, each 7cm in diameter) RF coils were used to image the occipital lobe in humans. Healthy human subjects were studied in a 9.4 Tesla/65cm bore magnet [2] interfaced to a DirectDrive 8-Transmit Channel Varian console.  $|B_1^+|$  maps were obtained with the two flip-angle technique [3]. To estimate the receive  $|B_1^-|$  profiles, the product  $\rho \cdot |B_1^-|$  was also derived ( $\rho$  being proton density). The two loops of the quadrature RF coil were driven by two independent channels, rather than with a classic hybrid (transmit-splitter/receive-combiner), thereby enabling the use of any phase shift between the two loops instead of the fixed  $90^\circ$  phase with a hybrid. RF efficiency maps were obtained for the quadrature RF coil by dividing the actual  $|B_1^+|$  by the sum of  $|B_1^+|$  of each loop (range: 0→1). Data processing was carried out in Matlab.

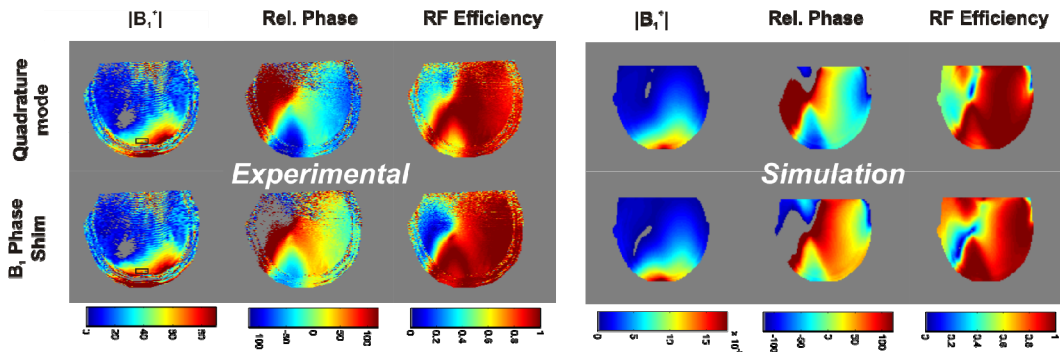
## Results and Discussion

**Single loop.**  $|B_1|$  maps in the human brain at 9.4 T with a single-loop RF coil clearly show two distinct patterns for  $B_1^+$  and  $B_1^-$  with opposite rotational direction (Fig. 1). Here we use  $\rho \cdot |B_1^-|$  to approximate the overall  $|B_1^-|$  profile. (Note that this lack of overlap between  $B_1$  profiles is not observed in small animals where the sample size is smaller than the  $^1\text{H}$  RF wavelength). Because transmit and receive profiles reach their maximum in different locations, a single voxel used in localized spectroscopy cannot be positioned optimally for both transmission and reception. In principle, higher RF power could be used to obtain higher peak  $B_1^+$  in a voxel located where  $B_1^-$  is maximal. However, power deposition (SAR) becomes a limiting factor at very high field and increasing transmit power is not a favorable option. A classical approach to enhance RF efficiency is to use a 2-loop quadrature coil. However, it has been shown that at high field  $B_1^+$  destructive interferences [4] can reduce RF efficiency between neighboring coils, thereby requiring proper adjustment of their relative phases [5,6].

**Two loops (“quadrature coil”).** Results show that when the two-loop coil was driven in classic quadrature mode, i.e. with a  $90^\circ$  phase between the loops, the transmit efficiency in a region-of-interest (ROI) located in the occipital lobe (black box in Fig. 2 left) was about 86% (Fig. 2, top). In contrast, when the transmit phase between these loops was locally adjusted using local  $B_1$  phase shim [5,6], the transmit efficiency in the same ROI was increased to 98% (Fig. 2, bottom). As a result, the peak RF power was reduced by  $\sim 30\%$  for a given excitation flip angle. Experimental measurements in a human head (Fig. 2, left) were highly consistent with simulated data obtained using similar RF coils design and a human head model (Remcom software) (Fig. 2 right). The phase shift calculated for local  $B_1$  phase shim was  $67^\circ$  in experiments and  $60^\circ$  in simulations.



**Fig. 1:**  $|B_1^+|$  and  $\rho \cdot |B_1^-|$  maps obtained with a single-loop coil in the human brain at 9.4 T with the mean profiles within the defined slice.



**Fig. 2:**  $|B_1^+|$ , relative phase difference between the loops and RF efficiency when using two loops in quadrature mode and with determined transmit phase. Experimentally measured maps in the human brain at 9.4 T (left) closely matched the simulated maps (right). RF efficiency is given by the ratio of actual  $B_1^+$  to available  $B_1^+$  [6].

## Conclusion

Single-loop RF coils do not appear optimal for NMR spectroscopy in human brain at 9.4 T because of limited overlap between transmit and receive  $B_1$  profiles. However, “quadrature” surface RF coils may be used as long as the relative phase between the two loops is optimized for a given ROI to maximize  $B_1$  transmit efficiency, thereby reducing SAR.

## References

[1] Collins MRM 2002 [2] Vaughan et al. MRM 2006; [3] Insko and Bolinger JMR 1993; [4] Van de Moortele et al. MRM 2005; [5] Van de Moortele et al. Int. Symp Biomed MRI, Germany 2006; [6] Metzger et al. MRM 2008.

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