# Efficient B0-inhomogeneity insensitive TQF <sup>23</sup>Na Imaging.

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#### Introduction

It is desirable to differentiate the signal due to free sodium ions (e.g. extra-cellular sodium) from that due to sodium ions restricted in their mobility (e.g. intra-cellular) invivo. One such method of discrimination is triple-qunatum filtering (see for example, [1,2,3]). It is well known [2,3] that TQF signal is severely damaged by possible  $B_0$ -inhomogeneities. The method of Wimperis et. al. [2] solved this problem by dephasing two out of the four contributing pathways using a gradient pulse, while the technique of Tanase and Boada [3] extracted all four contributing signals and corrected for  $B_0$  in post processing. Unfortunately, these approaches lead to loss of SNR efficiency. Here, we propose a new method which combines the advantages of the two techniques. In our method, the signal is split into two pairs of two coherence transfer pathways and the corresponding  $B_0$  correction is applied to each pair separately. This increases the TQF SNR efficiency by a factor of  $\sqrt{2}$  compared to the references [2,3]. In addition, if the signal to noise ratio is relatively high (SNR>5), the method can produce accurate  $B_0$ -corrected TQF images even without additional  $B_0$ -map information. We present the theory and a phantom validation of the method.

## Theory

Consider the TQF sequence [3,4] which consists of three excitation pulses of the same flip angle  $\theta$  and corresponding phases  $\phi_{123}$  and separated by delays  $\tau_{1,2}$  (see Figure 1) followed by a readout. The received signal is (see for example [3,5]):

followed by a readout. The received signal is (see for example [3,5]): 
$$S_{\Omega}(\phi_{1}, \phi_{2}, \phi_{3}, t) = \sum_{p_{1}=1}^{1} \sum_{p_{2}=3}^{3} e^{-i(p_{1}\phi_{1}+(p_{2}-p_{1})\phi_{2}-(1+p_{2})\phi_{3})} B_{p_{1}p_{2}}$$
(1)
$$B_{p_{1}p_{2}} = e^{-i(p_{1}\tau_{1}+p_{2}\tau_{2})\Omega} e^{i\Omega t} A_{p_{1}p_{2}}$$
(2)

where  $\Omega$  is the B<sub>0</sub>-field inhomogeneity and  $A_{p1p2}$  is the amplitude of the specified coherence pathway. The TQF signal is:

$$S^{TQ} = A_{+1-3} - A_{-1-3} - A_{-1+3} + A_{+1+3}$$

$$\approx e^{-i\Omega t} \sum_{p_1=\pm 1} p_1 \Big[ B_{p_1-3} + B_{p_1+3} \Big] e^{+ip_1\Omega \tau_1}$$
(3)

Consequently, the acquisition of  $B_0$ -corrected TQF data would consist of a  $B_0$ -mapping acquisition followed by a 12-step phase cycle: 1. Acquire signals  $S_{1;k}$  with  $\phi_{1;k} = 2\pi k/6$ ,  $\phi_{2;k} = 2\pi k/6$ ,  $\phi_{3;k} = 0$  for k=0,1,...,5; 2. Acquire signals  $S_{2;k}$  with  $\phi_{1;k} = \pi/2 + 2\pi k/6$ ,  $\phi_{2;k} = 2\pi k/6$ ,  $\phi_{3;k} = 0$  for k=0,1,...,5. The  $B_0$ -corrected TQF signal can be restored according to equation (3) taking into account (4):

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$$B_{p_1+3} + B_{p_1-3} = \frac{1}{2} \sum_{k=0}^{5} (-1)^{k+1} \left( S_{1;k} + i p_1 S_{2;k} \right)$$
(4)

### Results and Conclusions.

To validate the method, phantom experiments were performed on a 3T whole-body MAGNETOM Trio, A Tim System (Siemens AG, Germany) with a dual-tuned TX/RX  $^1\text{H}/^{23}\text{Na}$  head coil (Stark Contrast, Germany) and a modified GRE sequence (see Figures 1-3). The RF excitation train was comprised of three non-selective pulses of 500  $\mu s$  duration each. Acquisition parameters for the TQF imaging were 240x240x240 mm³ FOV with 16x16x16 encoding matrix; TR=165ms, TE=6.6ms, FA=90 $^0$  and  $\tau_1$ =5.5ms  $\tau_2$ =150 $\mu s$ . The images were acquired both with a 24-step cycle [3] and with the 12-step phase cycle as described here. SNR efficiency improvement between the 12-step and the 24-step methods is 1.47+/-0.08 which is in an agreement with theoretically predicted value of  $\sqrt{2}\approx1.41$  (see Figure 3).

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**References. 1.** Jaccard, et. al. J Chem Phys 85:6282, 1986. **2.** Wimperis, et. al. J Magn Reson 98:628, 1992. **3.** Tanase, et. al. J Magn Reson 174:270, 2005. **4.** Hancu, et. al. Magn Reson Med 42:1146, 1999. **5.** Keeler, Understanding NMR Spectroscopy, Wiley&Sons, 2005.

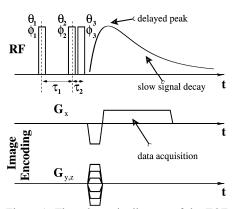


Figure 1: The schematic diagram of the TQF excitation block superposed with signal evolution and imaging readout.

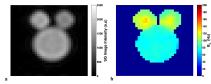


Figure 2: (a) A single-quantum sodium image of the phantom setup. Small bottles contain 4% agar gel with sodium, while large bottle contains saline. (b)  $B_0$ -map of the same slice. The field gradients cause minor intra-voxel dephasing on single-quantum images, but cause major signal dropout on the triple-quantum images (see Figure 3).

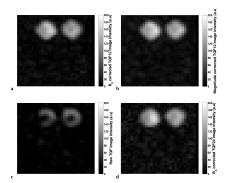


Figure 3: TQF image produced by the 12-step cycle after  $B_0$  correction (a) and after magnitude  $B_0$  correction (b).  $B_0$ -uncorrected TQF image (c) reveals signal dropouts in the areas of magnetic field offsets. For comparison, the TQF image produced with a 24-step cycle is presented in panel (d). SNR efficiency improvement between the 12-step and the 24-step methods is 1.47+/-0.08 which is in an agreement with theoretically predicted value of  $\sqrt{2} \approx 1.41$ .