

# Proton Diffusion Weighted and Sodium MRI of Growing Intrahepatic and Subcutaneous Hepatocellular Carcinoma

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## Introduction

Hepatocellular carcinoma (HCC) growth is associated with structural and metabolic transformations that can be monitored by non-invasive  $^{23}\text{Na}$  and  $^1\text{H}$  MRI. Changes in water apparent diffusion coefficient (ADC) and total tissue  $\text{Na}^+$  reflect mostly alterations in relative extracellular space (ECS) in tumor tissue, while changes in intracellular  $\text{Na}^+$  reflect physiologic and metabolic transformation in HCC cells. Water ADC measurement in the rat intrahepatic (IH) HCC model is challenging due to the effects of respiratory, cardiac, and other physiologic motion. To reduce motion artifact, the water ADC in rodent models has been usually studied using subcutaneous (SC) tumor models, and thus the absolute ADC values of IH HCC and their post-treatment changes remain unclear. In this study, in growing IH and SC HCC rat tumors and surrounding normal tissues, we examined the relationship between 1) water ADC measured by diffusion-weighted (DW)  $^1\text{H}$  MRI, 2) total tissue  $\text{Na}^+$  measured by single-quantum (SQ)  $^{23}\text{Na}$  MRI, and 3) intracellular  $\text{Na}^+$  measured by triple-quantum-filtered (TQF)  $^{23}\text{Na}$  MRI.

## Methods

For the IH HCC model, one million N1S1 cells were inoculated in the left lateral lobe of the liver; for the SC HCC model, ten million cells were inoculated under the skin on the thigh. MR images were acquired with a Varian 9.4-T, 31-cm horizontal bore system. Each animal was examined weekly for 4 weeks after tumor cell inoculation. Water ADC of the IH tumors and nearby liver tissue was measured with a 63-mm birdcage coil. A multi-slice DW  $^1\text{H}$  imaging sequence with the following imaging parameters was used: 1,100 ms repetition time (TR), 21 ms echo time (TE), 256 x 128 data points over a 80 x 80 field of view (FOV), 0.5 mm slice thickness, 1.5 mm slice gap, and  $b = 0, 256, 945$ , and  $1,679 \text{ s/mm}^2$ . Respiratory gating was used to minimize the motion effect on water ADC in IH HCC.  $^{23}\text{Na}$  images of IH HCC were obtained with a loop-gap volume resonator (inner diameter = 60 mm, depth = 25 mm) tuned to 105 MHz. A 3D gradient-echo  $^{23}\text{Na}$  imaging sequence with the following parameter was used:  $\sim 240 \mu\text{s}$  non-selective excitation RF pulse, 50 ms TR, 4.6 ms TE, 64 x 64 x 16 data points over a 60 x 60 x 36 mm FOV, and 10 min total data collection time. TQF  $^{23}\text{Na}$  MRI was performed using the same parameters as for SQ  $^{23}\text{Na}$  MRI, except a TR of 100 ms and a data size of 64 x 32 x 8 was used.  $^1\text{H}$  and  $^{23}\text{Na}$  MRI of SC tumors and nearby tissue were obtained with a 30 mm diameter dual-tuned loop-gap volume coil. DW  $^1\text{H}$ , and SQ and TQF  $^{23}\text{Na}$  images of SC tumor were acquired employing the same parameters as for IH tumors, except a 60 x 60 mm FOV was used. Total data collection time for a set of DW  $^1\text{H}$  MRI, SQ  $^{23}\text{Na}$  MRI, and TQF  $^{23}\text{Na}$  MRI was 15, 7, and 45 min, respectively.

## Results

The tumor doubling time was 3.9 days for IH HCC and 11.2 days for SC HCC (Fig. 1). Seven days after cell inoculation, the water ADC in IH HCC ( $1.4 \pm 0.1 \times 10^{-3} \text{ mm}^2/\text{s}$ ) was significantly higher compared to the adjacent normal liver ( $1.0 \pm 0.1 \times 10^{-3} \text{ mm}^2/\text{s}$ ,  $p \leq 0.05$ ). This difference was consistent despite a small decrease in the ADC of IH HCC from day 7 through day 28. The motion artifacts in DW MRI were only partially avoided by respiratory gating. Fig. 2 shows that  $^1\text{H}$  images of IH tumor can be moderately (A) or intensively (B) blurred by motion at non-zero  $b$ -values, in contrast to SC tumors (C). The water ADC of SC HCC increased from  $0.63 \pm 0.01 \times 10^{-3} \text{ mm}^2/\text{s}$  at day 14 to  $0.72 \pm 0.04 \times 10^{-3} \text{ mm}^2/\text{s}$  at day 21, and  $0.79 \pm 0.06 \times 10^{-3} \text{ mm}^2/\text{s}$  at day 28 ( $p < 0.05$  vs. 14 day value). The water ADC of SC HCC was lower ( $p < 0.01$ ) compared to the IH HCC by 53%, 37%, and 24% on days 14, 21, and 28, respectively. Growth of IH HCC was associated with increases in both SQ and TQF  $^{23}\text{Na}$  signal intensity (SI). At day 28, mean SQ  $^{23}\text{Na}$  SI from the IH HCC increased to  $2.5 \pm 0.6$  times the day 7 value ( $p < 0.05$ ), while the SI from the surrounding liver tissue remained unchanged. The changes in TQF  $^{23}\text{Na}$  were similar to SQ  $^{23}\text{Na}$  but more profound. On day 21, the mean TQF  $^{23}\text{Na}$  SI increased to  $2.1 \pm 0.5$  times the day 7 value ( $p < 0.05$ ), and on day 28 to  $2.7 \pm 0.5$  times the day 7 value ( $p < 0.05$ ). SC HCC tumors also showed similar changes in SQ and TQF  $^{23}\text{Na}$  MRI SI. On day 28, the mean SQ  $^{23}\text{Na}$  SI increased to  $1.5 \pm 0.1$  times the day 14 value (Fig. 3). On day 21, the mean TQF  $^{23}\text{Na}$  SI increased to  $1.7 \pm 0.4$  times the day 14 value ( $p < 0.05$ ) and on day 28 to  $1.8 \pm 0.4$  times the day 14 value ( $p < 0.05$ ).

## Discussion

Our previous data show that the increase in SQ and TQF  $^{23}\text{Na}$  MR SI of SC-implanted RIF-1 and 9L tumors are caused by increases in ECS and intracellular  $\text{Na}^+$  concentration, and not by changes in  $^{23}\text{Na}$  relaxation times [1, 2]. Histological analysis of IH HCC showed that its growth is associated with increased inflammation and necrosis, which leads to increases in ECS and SQ  $^{23}\text{Na}$  SI. The observed increase in TQF  $^{23}\text{Na}$  SI may result from progressive hypoxia with tumor growth. Hypoxia shifts the tumor metabolism from oxidative phosphorylation to glycolysis, which may reduce ATP production. The decrease in energy status may decrease the activity of  $\text{Na}^+/\text{K}^+$ -ATPase and increase intracellular  $\text{Na}^+$  concentration. Thus, the observed increase in SQ  $^{23}\text{Na}$  in growing HCC reflects an increase in ECS, and the increase in TQF  $^{23}\text{Na}$  represents an increase in intracellular  $\text{Na}^+$  concentration.

## Conclusion

Water ADC of HCC depends on tumor location and is greatly affected by physiological motion. SQ and TQF  $^{23}\text{Na}$  MRI are not affected by motion, and show increases in total and intracellular  $\text{Na}^+$  with untreated tumor growth in both IH and SC tumors. SQ and TQF  $^{23}\text{Na}$  MRI techniques are more reliable compared to water ADC measurements for hepatic tumor studies because of their insensitivity to motion.

## References

- 1) Winter et al. *Cancer Res* 2001; 61: 2002-2007.
- 2) Babsky et al. *Neoplasia* 2005; 7: 7658-7666.

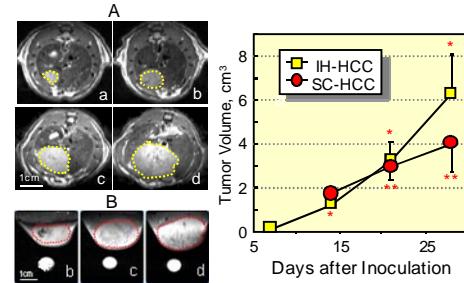


Fig.1. The HCC volumes on 7 (a), 14 (b), 21 (c) and 28 (d) days after N1S1 cell inoculation. On the left side DWI of IH (A) and SC (B) tumors are marked by dotted lines; on the right side the means of tumor volume are presented: \*  $p < 0.05$  (vs. Day 7), \*\*  $p < 0.05$  (vs. Day 14),  $N=5$ .

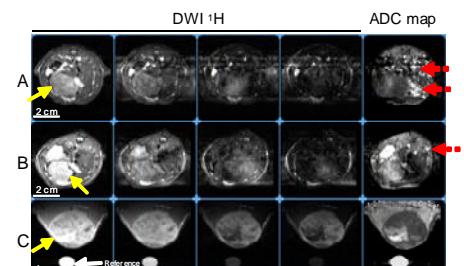


Fig.2. DWI and ADC maps of IH (A, B) and SC (C) HCCs at different  $b$ -factors (in  $\text{s/mm}^2$ ): a - 0, b - 256, c - 945, d - 1679. HCC is marked by yellow arrows and the motion artifact is marked by the dotted red arrows on the ADC maps.

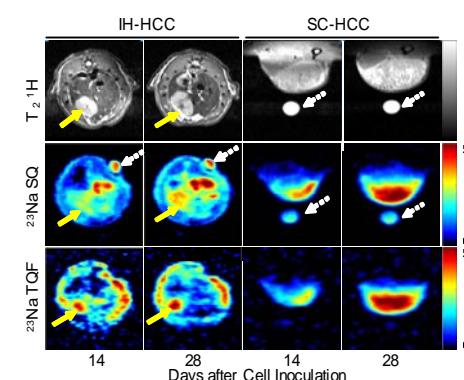


Fig.3. DWI  $^1\text{H}$ , SQ and TQF  $^{23}\text{Na}$  MRIs of IH and SC HCCs 14 and 28 days after N1S1 cell inoculation. IH-HCCs are marked by yellow arrows and the references are marked by the dotted white arrows.