

## Dixon bSSFP in the Presence of $B_0$ Inhomogeneities

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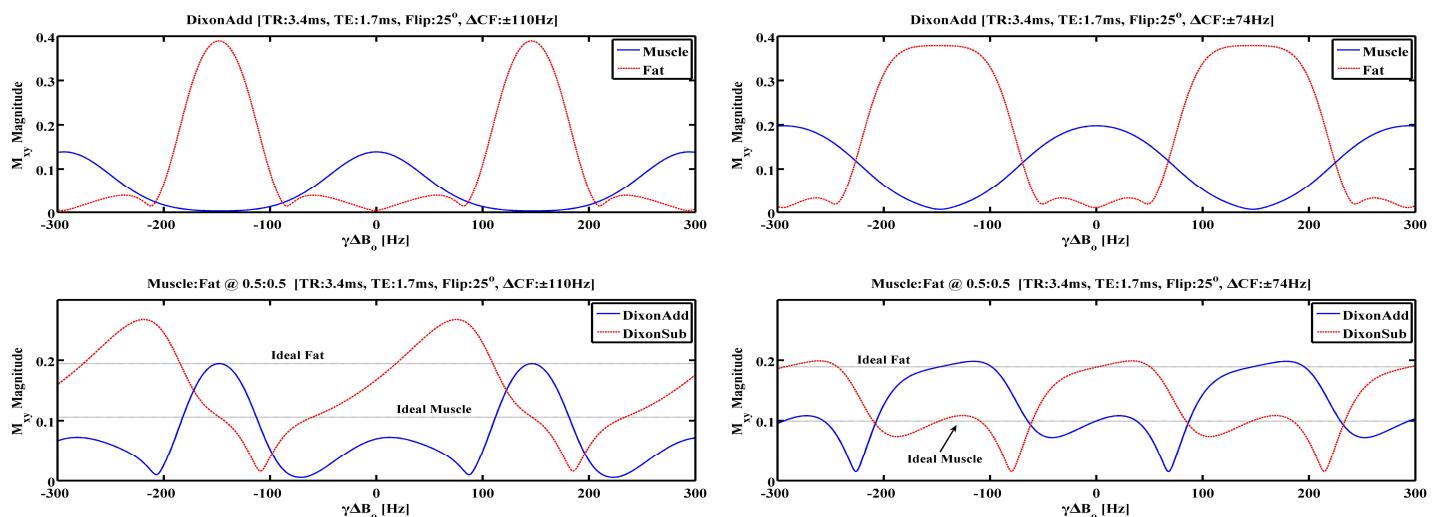
**Introduction:** The two-point, fat/water-separation Dixon method for balanced steady-state free precession (bSSFP) introduced by Huang *et al.*<sup>1</sup> shows great promise for non contrast-enhanced MR angiography<sup>2</sup>. Here, we investigate its limitations in the presence of  $B_0$  inhomogeneities (*i.e.*, from magnet non-uniformity, susceptibility, *etc.*), and for pixels containing a mixture of fat and water. From the analysis, we propose acquiring/using a  $B_0$  inhomogeneity map to better suppress fat and produce more robust water-only images.

**Methods:** All simulations were done in Matlab (version 7.4; The MathWorks, Natick, MA), with the theoretical, noise-free signals synthesized using the general SSFP equations from Haacke *et al.*<sup>3</sup> We used typical 3.0 tesla values for the tissue parameters  $M_0$ ,  $T_1$ ,  $T_2$ , and chemical shift (CS) of fat and water, namely  $M_0$ : 0.9/1.0,  $T_1$ : 300/1100 ms,  $T_2$ : 60/50 ms, and CS: -440/0 Hz, respectively. The cycle time,  $\tau_{cyc}$ , of fat with respect to water is  $\sim 2.27$  ms. The Huang-Dixon method requires (i) TR to be an odd half-multiple of  $\tau_{cyc}$ , (ii) TE =  $\frac{1}{2}$ TR, and (iii) two acquisitions with different centre frequency (CF) offsets. The water-only signal is calculated from the complex addition of the two scans. Simulations shown here used TR/TE: 3.4/1.7 ms, a 25° flip angle, and  $\gamma\Delta B_0$  within  $\pm 300$  Hz.

**Results:** SSFP techniques are known to exhibit periodicity with respect to off-resonance frequency, whereby the signal “bandwidth”  $BW_{ssfp}$  is  $1/TR$  (*i.e.*,  $\sim 294$  Hz herein). Consequently, water that is off-resonant by  $\pm \frac{1}{2}BW_{ssfp}$  yields little signal and produces the familiar dark bands. By applying a centre frequency offset of say  $\delta f$ ,  $BW_{ssfp}$  is unchanged but the dark bands shift commensurately (*e.g.*, to  $\delta f \pm \frac{1}{2}BW_{ssfp}$  for water). Below are two Huang-Dixon outcomes (with CF offsets of  $\pm 110$  and  $\pm 74$  Hz, top row) for pixels containing only water or only fat. At first glance, the  $\pm 110$  Hz results seem more desirable, but the water signal is noticeably apodized. By comparison, the  $\pm 74$  Hz (*i.e.*,  $\pm \frac{1}{4}BW_{ssfp}$ ) offsets show a more symmetric/periodic behavior, and the complex subtraction (not shown) is its complement. Now, for an equal muscle-to-fat mixture, admittedly the worst-case scenario, the outcomes (bottom row) are striking: periodicity is still evident, the complementary nature of the complex add/subtract signals is seen only for the  $\pm 74$  Hz centre frequency offsets ( $\pm \frac{1}{4}BW_{ssfp}$ ), and the desired water signal is more severely modulated as compared to the no-mixture results.

**Conclusion:** Increasing the  $B_0$  uniformity is clearly of paramount importance for the Huang-Dixon method. However, the diagrams below show that by using CF offsets of  $\pm \frac{1}{4}BW_{ssfp}$ , the complex add/subtract results are complementary. This suggests that if one acquires a  $B_0$  inhomogeneity map (which may be of lower resolution), and applies (i) complex *summation* for pixels within the frequency ranges  $\gamma\Delta B_0 = \{ (n+\frac{1}{4})BW_{ssfp} \text{ to } (n-\frac{1}{4})BW_{ssfp} \}$ , with  $n$  an integer, and (ii) complex *subtraction* otherwise, one should ideally obtain an improved, fat-suppressed, mostly-water bSSFP image. More specifically, (a) for mostly-water pixels (upwards of  $\sim 80\%$ ), the banding artifacts would be significantly reduced, (b) mostly-fat pixels would be suppressed in the water-only image, regardless of  $B_0$  inhomogeneity, and (c) pixels that contain comparable amounts of fat and water *might* show band artifacts, but only for those pixels that are off-resonant near odd multiples of  $\pm \frac{1}{4}BW_{ssfp}$ .

**References:** <sup>1</sup>TY Huang, *et al.* Magn Reson Med 2004, 51:243. <sup>2</sup>R Stafford, *et al.* Magn Reson Med 2008, 59:430. <sup>3</sup>EM Haacke, *et al.* “Magnetic resonance imaging: Physical principles and sequence design”, John Wiley and Sons, New York, 1999, Chapter 18.



**Figure:** The upper row shows the Huang-Dixon complex addition results for pixels that contain only water or only fat. The left column is for CF offsets of  $\pm 110$  Hz, while the right column is for CF offsets of  $\pm 74$  Hz ( $\pm \frac{1}{4}BW_{ssfp}$ ). The lower row depicts both the complex addition and subtraction results for a pixel that contains 50% water and 50% fat. The ‘Ideal Fat’ and ‘Ideal Muscle’ horizontal lines represent the maximum signals for that tissue at their respective  $\pm$ CF offsets.