

# Hyperpolarized $^{13}\text{C}$ MRS in the Rat Brain: Spectral Improvements with $^1\text{H}$ Decoupling

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## Introduction

Most *in vivo* studies using the dynamic nuclear polarization (DNP) technique (1) to enhance sensitivity of  $^{13}\text{C}$  have been utilizing molecules with  $^{13}\text{C}$  labeled quaternary carbons. In the most often used  $[1-^{13}\text{C}]$ pyruvate,  $^{13}\text{C}$  labeled carbon does not have any  $^1\text{H}$  attached to it and experiences only small  $J$ -coupling with  $^1\text{H}$ 's three bonds away. In case of  $[2-^{13}\text{C}]$ pyruvate and  $[1-^{13}\text{C}]$ lactate,  $^{13}\text{C}$  labeled carbon also does not have any  $^1\text{H}$  attached to it, but it is  $J$ -coupled to  $^1\text{H}$ 's which are two bonds away. The  $J$ -coupling structure can be very useful for providing qualitative molecular structure information. However, for *in vivo* application, this splitting structure is undesirable since  $J$ -splittings distribute signal intensity over many smaller peaks and therefore reduce detection sensitivity. In this work, we investigate the effects of heteronuclear  $J$ -coupling on hyperpolarized  $[1-^{13}\text{C}]$ pyruvate and  $[2-^{13}\text{C}]$ pyruvate signals and their metabolic products.

## Methods

A mixture of  $[1-^{13}\text{C}]$ pyruvic acid and OX63 trityl radical and  $[2-^{13}\text{C}]$ pyruvic acid and OX63 trityl radical were hyperpolarized by DNP (Hypersense, UK) for 90 min in a field strength of 3.35 T at approximately 1.4 K (1). The sample was then dissolved in 40 mM TRIS buffer, 40 mM NaOH and 0.32 mM Na<sub>2</sub>EDTA solution to produce 4 mL of hyperpolarized solution at a concentration of ~35 mM. *In vivo* experiments were performed using a 9.4-T/31-cm bore magnet equipped with a Varian INOVA spectrometer. Fasted male Sprague-Dawley rats were injected intravenously with approximately 2.2 mL of hyperpolarized  $[1-^{13}\text{C}]$ pyruvate or  $[2-^{13}\text{C}]$ pyruvate under isoflurane anesthesia.

*In vivo*  $^{13}\text{C}$  NMR spectra were acquired using a coil assembly consisting of a  $^1\text{H}$  quadrature surface coil (two loops of 14 mm diameter) and an inner  $^{13}\text{C}$  linearly polarized surface coil (12 mm diameter). A small sphere filled with  $^{13}\text{C}$  labeled formic acid placed at the center of the coil served as external reference. Decoupled and undecoupled spectra were acquired one after another 10 s after injection of a hyperpolarized  $[1-^{13}\text{C}]$ pyruvate solution with LASER sequence (2) adapted for  $^{13}\text{C}$  spectroscopy and using a 45° BIR4 pulse for excitation. The  $^1\text{H}$  decoupling was performed using WALTZ-16.

## Results and Discussion

Figure 1 shows representative spectra obtained with  $^1\text{H}$  decoupling from 400  $\mu\text{L}$  voxel placed in the rat brain. Table 1 reports the effects of decoupling on linewidths. The linewidth of  $[1-^{13}\text{C}]$ pyruvate signal was narrower by  $1.2 \pm 0.3$  Hz with decoupling and  $[1-^{13}\text{C}]$ lactate signal by  $6.3 \pm 0.6$  Hz.

**Table 1.** Effects of decoupling on linewidths reported in Hz (4 animals, 10 dissolutions).

Undecoupled linewidths		Decoupled linewidths		Difference in linewidths	
$[1-^{13}\text{C}]$ pyr	$[1-^{13}\text{C}]$ lac	$[1-^{13}\text{C}]$ pyr	$[1-^{13}\text{C}]$ lac	$[1-^{13}\text{C}]$ pyr	$[1-^{13}\text{C}]$ lac
$7 \pm 1$	$12.8 \pm 0.9$	$6 \pm 1$	$6.4 \pm 0.6$	$1.2 \pm 0.3$	$6.3 \pm 0.6$

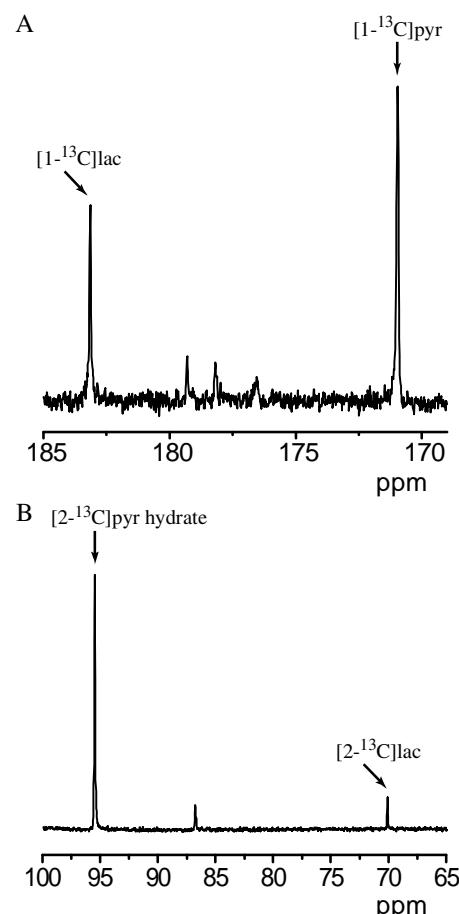
The effect of decoupling on SNR was difficult to determine *in vivo* due to the loss of magnetization caused by a 45° BIR4 excitation pulse. Therefore, to obtain information about effects of decoupling on SNR simulations were performed using values of long-range  $J$ -couplings and assuming a linewidth of 6 Hz, consistent with *in vivo* data. The effects of decoupling on SNR are reported in Table 2. There was almost no improvement in SNR for  $[1-^{13}\text{C}]$ pyruvate signal. Decoupling improved SNR for  $[1-^{13}\text{C}]$ lactate signal by 50%. The improvement in SNR was even greater for  $[2-^{13}\text{C}]$ pyruvate and  $[2-^{13}\text{C}]$ lactate signals. The larger improvement for  $[2-^{13}\text{C}]$ lactate signal was expected due to the large value of one bond  $J$ -coupling. The improvement in the linewidth in the simulations was consistent with experimental data (Table 1).

## Conclusions

$^1\text{H}$  decoupling significantly improved the linewidth and signal-to-noise ratio of  $[1-^{13}\text{C}]$ lactate,  $[2-^{13}\text{C}]$ pyruvate and  $[2-^{13}\text{C}]$ lactate. Negligible improvement was observed for  $[1-^{13}\text{C}]$ pyruvate, consistent with very small three bond  $J$ -coupling.

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**References:** 1. Abragam and Goldman, *Rep Prog Phys* 1978. 2. Garwood *et al.*, *J Magn Reson* 2001.



**Figure 1.** Representative localized spectra obtained after injection of hyperpolarized (a)  $[1-^{13}\text{C}]$ pyruvate and (b)  $[2-^{13}\text{C}]$ pyruvate solutions with  $^1\text{H}$  decoupling from 400  $\mu\text{L}$  brain voxel (LASER,  $T_R = 0.75$  s,  $T_E = 27$  ms,  $lb = 1$  Hz).

**Table 2.** Effects of decoupling on SNR reported as ratio of decoupled to undecoupled SNR.

$[1-^{13}\text{C}]$ pyr	$[1-^{13}\text{C}]$ lac	$[2-^{13}\text{C}]$ pyr	$[2-^{13}\text{C}]$ lac
1.01	1.51	1.85	2.61