

Rapid and Direct Quantification of Longitudinal Relaxation Time (T₁) in Look-Locker Sequences Using an Adaptive Neural Network

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Introduction:

Fast and accurate measurement of the longitudinal relaxation time T₁, has become increasingly important to quantitatively estimate tissue physiological parameters such as perfusion, capillary permeability, and the volume of extravascular-extracellular space using R₁ (R₁=1/T₁) maps in dynamic contrast-enhanced MRI (DCE-MRI) [1-5]. In the past, we have used an imaging variant of the Look-Locker sequence, the T One by Multiple Readout Pulses (TOMROP) sequence, for estimates of the temporal variation of contrast agent concentration in tissue and blood [6]. The Look-Locker (LL) sequence provides accurate T₁ estimates, with the advantages of shorter acquisition time, and a wide range of sampling times post-inversion [7]. In the Look-Locker experiment, the relationship between T₁ and the acquired signal in the Bloch equation is fairly complex. Finding the T₁ value for the LL is generally accomplished by some form of multi-dimensional curve fitting used to estimate a set of unknown parameters (T₁, tip-angle, M₀, etc) in the LL signal [7]. However, these fitting methods are sensitive to initial guesses and a biased estimation of one parameter will bias estimates of the other parameters. In this study, an Adaptive Neural Network (ANN) is trained and employed as an unbiased estimator of T₁. The presented estimator was tested by simulating the LL signal at different levels of SNR and results of its application to the DCE experimental data were compared with the T₁ maps estimated by conventional methods (Simplex-least square fitting) and the values of T₁ reported by literature.

Materials and Methods: We hypothesized that, given a signal generated by a LL model, an ANN could be trained to directly estimate T₁. The analytical equation of the Look-Locker signal (Gelman *et al* [7] was considered as the gold standard of training and a set of LL signals for a wide range of T₁'s were generated. For each T₁ value LL signal inputs were generated by varying the other independent parameters in the synthetic model of signal (T₂*, M₀ etc). A range of Gaussian noise (SNRs of 10, 15, 20, 30, 50, and 100) was added to all simulated signals; simulated signals were input to the ANN and their T₁ value was used as the ANN training output. To characterize the generalization error the ANN was trained and validated by the K-Folding Cross Validation (KFCV) method [8-9]. The average error, calculated by the Area Under Receiver Operator Characteristic (AUROCC) of the ANN validated on the K omitted subsets then served as the estimate of the generalization error. In this study, to assure a very reliable estimate of the generalization error, K was set to 20 for ~900,000 samples (45000 in each fold). The ANN thus constructed had a single output, an estimate of T₁ value. To illustrate and test the ANN's accuracy for analysis of the experimental LL data, it was also applied to the LL sequences acquired from 19 Crl:NIH nude rats implanted with U251 cells (2x10⁵ cells/0.1 ml) intracerebrally. All rats with 2-week old tumors, were scanned using a 7T magnet, Bruker Avance console, and Bruker-supplied RF coils. A T-One by Multiple Read-Out Pulses (TOMROP) sequence acquired at baseline and every 145 s following injection of a contrast agent, Gadomer (Schering AG). Figure 1 illustrates an example of pre and post contrast T₁ maps estimated by the model-trained ANN, and a map of ΔR_1 . To check the accuracy of the ANN in temporal estimation, the ΔR_1 maps for each slice were constructed and the lesion time signature, normal area and sagittal sinus were plotted and compared. Results demonstrated that the model-trained ANN was capable of estimating a reliable map of T₁.

Results and discussion: This study proposes an ANN trained by an analytical input to demonstrate the flexibility of ANNs, and the multiple paths that these instruments offer in the assessment of nonlinear input-response systems. This pilot study imply possibility that generation of an ANN based on the Shutter Speed Model, with a wide range of model conditions (transfer constants, compartmental water exchange rates and sizes, etc.) as model training sets. In this study an accurate estimator for direct and rapid quantification of longitudinal T₁ relaxation time is proposed. Beside simulation, to illustrate and test the method's accuracy for analysis of the experimental LL data, it was also applied to the LL sequences acquired from 19 animals (3 slices each with U251 tumor (An example is shown in figure 2). Experimental results of the proposed method for all 19 animals were also compared to the results of the conventional method (Simplex method with least square fitting). Results imply that the proposed and conventional methods are highly correlated (r=0.83, p<0.0001). Therefore the proposed method has a very good potential to be used as a fast and accurate T₁ map or delta R₁ map estimator from LL data in DCE studies which play an important role in quantification of physiological parameters.

References:

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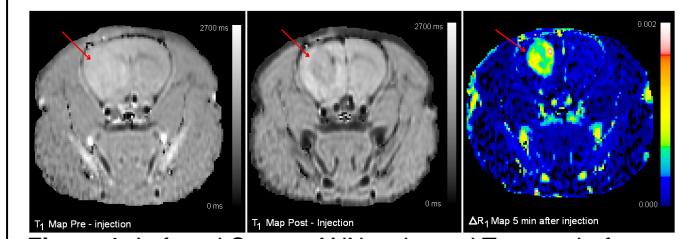


Figure 1: Left and Center: ANN estimated T₁ maps before (Left) and after injection of Gadomer in a U251 model of cerebral tumor. Right: ΔR_1 . These maps were constructed using an ANN trained by an analytical model.