

Renormalization Group Method: Enhancement of Bassler-Sen Model of the Brain White Matter

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1. Introduction: Water diffusion in neurological tissues is known to exhibit multi-component diffusion behaviour. The random motion of water molecules is in accordance with the structure peculiarities and the physical properties of composite brain white matter. We simulate the complex behaviour of water molecules using the *Bassler-Sen* model [1] and the renormalization group (*RG*) method [2,3] (in this study we do not use the Maxwell-Garnett approximation adapted in [2,3]). In the context of the modelling framework, we explore a bridge between local and effective global diffusive transport properties and estimate the sensitive of the diffusion coefficient to the dominant set of micro-parameters: extracellular volume fraction, extracellular diffusion, myelin-sheath diffusion, axon diffusion, mean size of axon, mean size of myelin-sheath, extra-cellular proton density, myelin-sheath proton density, and axon proton density.

2. Methods: Brain white matter has a very complex, multi compartmental structure. In general it comprises myelinated axons immersed in extracellular matrix. Axons are distributed chaotically and, for convenience, they can be treated as ideal cylinders. Following the *Bassler-Sen* model, we characterize coated fibres by D_m (myelin-sheath diffusion), D_a (axon diffusion) and corresponding proton densities c_a, c_m , which have outer (R_m) and inner (R_a) radius. Such a fibre is immersed in an extra-cellular space, the Wigner-Seitz (WS) cell, with diffusion D_e , proton density c_e and linear size L (Fig.1). It is possible to calculate the diffusive properties of WS cell using the *Bassler-Sen* model for the case when WS is occupied with a fibre and the empty WS cell is assigned with extra-cellular properties. Two types of WS cells can be randomly distributed on the square lattice with probability p that WS cell is empty and $(1-p)$ that WS is occupied with fibre (Fig.2, a black WS cell indicates fibre occupation). Such an approach is the opposite of the ordered spatial distribution of fibres described in the *Bassler-Sen* model. On the square lattice with randomly occupied cells it is possible to outline 2×2 WS cell. All non-degenerative configurations of black and white WS cells on the scale 2×2 are presented in Fig.3. In Fig.4 the process of scale renormalization is depicted for the specific distribution of WS cells. Mathematically, such an *RG* process can be described by a system of nonlinear equations (Eq.1). In the Table1, equations for probability r_n^k and their degeneracy numbers for six classes of 2×2 cells (Fig.3) are presented. These equations comprise Eq.1a representing the *RG* process for an extra-cellular region. Eqs.(1c,d) were derived according to the rules given in the last column of Table1 and probability density (Eq.1b).

$$P_{n+1} = \sum_k g_k r_n^k \quad (1a)$$

$$P_{n+1} = (1-p_n)\delta(D_e - D_e^{L,n}) + p_n\delta(D_e - D_e^{U,n}) \quad (1b)$$

$$D_e^{U,n+1} = \langle D_e^{U,n} \rangle \quad (1c)$$

$$D_e^{L,n+1} = \langle D_e^{L,n} \rangle \quad (1d)$$

$$ADC_{eff} = (2D_e^{n \rightarrow \infty} + D_e)/3 \quad (2)$$

$$S = |\partial \log(ADC_{eff}) / \partial \log(X)| \quad (3)$$

Table 1

Class	Probability, r_n^k	Degeneracy, g_k	Effective diffusivity, $D_e^{U,L,n+1}$
I	$(1-p_n)^4$	1	$D_e^{L,n}$
II	$p_n^4(1-p_n)^3$	4	$(2D_e^{L,n}D_e^{U,n} + D_e^{L,n}(D_e^{L,n} + D_e^{U,n}))/2(D_e^{L,n} + D_e^{U,n})$
III	$p_n^2(1-p_n)^4$	4	$(2D_e^{L,n}D_e^{U,n})/(D_e^{L,n} + D_e^{U,n})$
IV	$p_n^2(1-p_n)^4$	2	$(D_e^{L,n} + D_e^{U,n})/2$
V	$p_n^4(1-p_n)^4$	4	$(2D_e^{L,n}D_e^{U,n} + D_e^{U,n}(D_e^{L,n} + D_e^{U,n}))/2(D_e^{L,n} + D_e^{U,n})$
VI	p_n^4	1	$D_e^{U,n}$

Table 2

Parameter X	Input value
D_e	$2 \cdot 10^{-9} \text{ m}^2 / \text{s}$
D_m	$.75 \cdot 10^{-9} \text{ m}^2 / \text{s}$
D_a	$.3 \cdot 10^{-9} \text{ m}^2 / \text{s}$
c_e	.95
c_a	.88
c_m	.5
R_m	$6.57 \cdot 10^{-6} \text{ m}$
R_a	$4 \cdot 10^{-6} \text{ m}$
p	[0,1]

3. Results: We input the microscopic parameters, X , taken from Table2 into the *Bassler-Sen* model to estimate lower (L superscript in notation, black square in Fig.2) and upper (U superscript in notation, white square in Fig.2) bounds of transverse diffusivity (t subscript in notation). Then we were solving Eq.1 for different values of p . During the *RG* process, effective diffusion approaches the stable point $D_e^{U,n \rightarrow \infty} = D_e^{L,n \rightarrow \infty} = D_e^{n \rightarrow \infty}$ which depends on the extra-cellular volume fraction p (Fig.5). The number of n -steps in the *RG* trajectory is a function of p (Fig.6, changes of the effective diffusion are colour coded). In Fig.7 the dependence of longitudinal, D_e , transverse effective diffusion, $D_e^{n \rightarrow \infty}$, as well as ADC_{eff} (Eq.2) are presented. For comparison, we present the *classical Bassler-Sen* results. We estimated the absolute value of the sensitivity, S , of ADC_{eff} to the various X micro-parameters changes (Eq.3) and plot pie chart with corresponding weights (Fig.8).

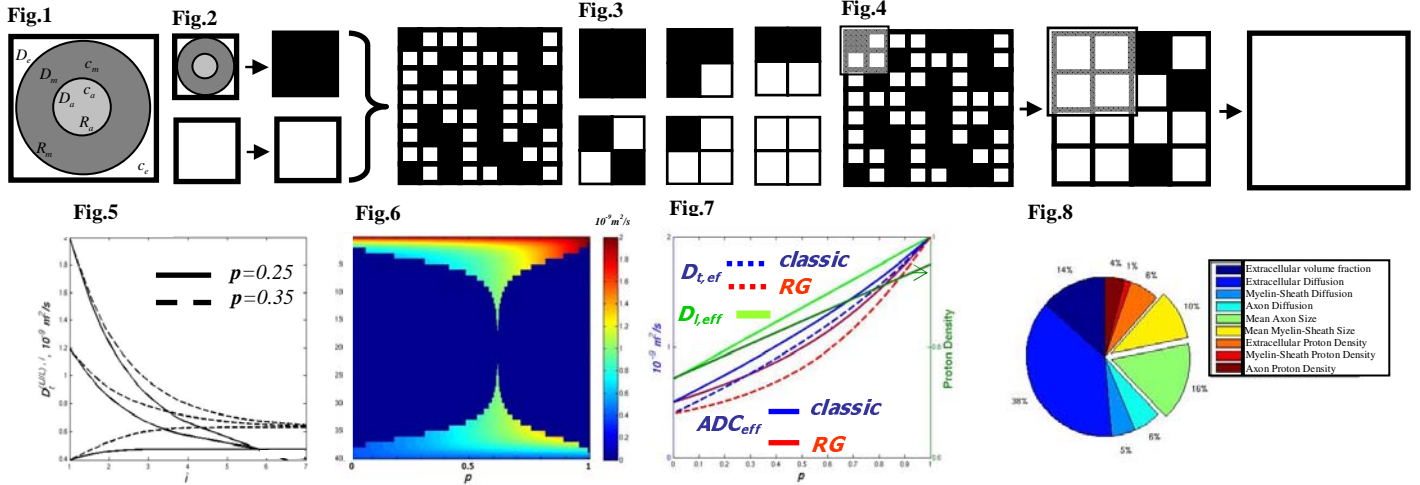


Fig.1. WS square cell occupied by myelinated fibre. The geometrical and physical parameters are labelled. **Fig.2.** Occupied and unoccupied WS cells imply upper (white) and lower (black) bounds of diffusivity. The WS cells are randomly distributed. **Fig.3.** Six basic configurations of WS cells with the scale 2×2 . **Fig.4.** The *RG* procedure for cell 2×2 . **Fig.5.** Approach of stable effective diffusivity after i *RG*-steps. **Fig.6.** Dependence of the number *RG* steps versus extra-cellular volume fraction. Evolution of diffusivity during the *RG*-process is colour-coded. **Fig.7.** Dependence of ADC_{eff} , $D_e^{L,eff}$, $D_e^{U,eff}$ versus p . Every point in these curves is a result of the *RG* process. For comparison, the *Bassler-Sen* results are shown. **Fig.8.** Pie chart of absolute values of the sensitivity, S , of ADC_{eff} near the physiologically relevant point ($p \sim 0.2$).

4. Discussion: Using the *RG* method we have calculated the sensitivity of the ADC_{eff} to the different microparameters variations. We found that the ADC_{eff} exhibits its the strongest sensitivity to the extra-cellular volume fraction and diffusivity. These findings suggest a possible mechanism to explain ADC_{eff} changes during neurodegenerative disease progression. The ADC_{eff} demonstrates more nonlinear behaviour vs p changes due to blocking effects which are absent in ordered model of the brain white matter.

References: [1] Sen P, Bassler P, *Biophys. J.*, **89** (2005) 2927. [2] Posnansky O., Shah N.J., *ISMRM2008*. [3] Posnansky O., Shah N.J., *J. Biol. Phys.*, in press.